

# **TUBULIN IN VITRO, IN VIVO AND IN SILICO**

A Dissertation

by

ANDREAS MERSHIN

Submitted to the Office of Graduate Studies of  
Texas A&M University  
in partial fulfillment of the requirements for the degree of

DOCTOR OF PHILOSOPHY

December 2003

Major Subject: Physics

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## ABSTRACT

Tubulin in Vitro, in Vivo and in Silico. (December 2003)

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Tubulin, microtubules and associated proteins were studied theoretically, computationally and experimentally in vitro and in vivo in order to elucidate the possible role these play in cellular information processing and storage. Use of the electric dipole moment of tubulin as the basis for binary switches (biobits) in nanofabricated circuits was explored with surface plasmon resonance, refractometry and dielectric spectroscopy. The effects of burdening the microtubular cytoskeleton of olfactory associative memory neurons with excess microtubule associated protein TAU in *Drosophila* fruitflies were determined. To investigate whether tubulin may be used as the substrate for quantum computation as a bioqubit, suggestions for experimental detection of quantum coherence and entanglement among tubulin electric dipole moment states were developed.

## **DEDICATION**

In memory of Petros Antaios, thinker, writer, poet and grandfather.

## ACKNOWLEDGEMENTS

I wish to express sincere appreciation to the chair of my committee Prof. Dimitri Nanopoulos for his guidance and supervision throughout my graduate school years. I am indebted to Prof. Hans Schuessler, Prof. Efthimios Skoulakis and Dr. Alex Kolomenski for their advice, guidance and help during this Ph.D. project.

Ms Rita Williamson provided essential help at critical points in the production of this manuscript. The Williamson, Sekaquaptewa and Hilliard families have given me much support and have been instrumental in enriching my Texas experience. I also wish to thank the financial sponsors of this project: the National Science Foundation, The Texas Informatics Task Force, the Dean of Science of Texas A&M University and the S.A. Onassis Public Benefit Foundation. In particular, Dr. Mita Desai's help and encouragement were invaluable.

Finally, none of this work would have been possible without the decades-long constant efforts, support and love by Lina and Slava and Loula and Stavros.

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## CHAPTER I

### INTRODUCTION

#### 1.1 Overview

This thesis reports on my efforts to address in several different ways the hypotheses concerning the existence and function of subcellular, protein-based information-processing elements.

The system of interest is the neural cytoskeleton and specifically the tubulin polymers known as microtubules (MTs). This work was originally motivated by quantum physics-based scenaria of brain function and consciousness that implicated these structures [1,2,3]. It was however found that the vast majority of such proposals were purely speculative, with no experimental evidence mentioned or sought. As a result, the first step in this Ph.D. was to show that at least some of the predictions of the more realistic scenaria proposed, such as for instance the models put forth by D.V. Nanopoulos et al., are in fact experimentally testable. Initially, this research concentrated on testing one prediction that was common to many of these exotic theories: that microtubules had a global role in neural function and were not merely the structural scaffolding of cells occasionally assisting in mobility and intracellular transport. To test this prediction, it was decided to investigate what effects a minimal disruption of the microtubular network of neural cells has on memory. Memory was selected because the more interesting models such as for instance the Guitar String Model (GSM) of the

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This dissertation follows the style of *Biopolymers*.

engram -see Chapter II) suggested an intracellular memory encoding and storage mechanism highly dependent on the precise stoichiometry of microtubules and microtubule associated proteins (MAPs) such as TAU (Chapter II).

This stoichiometry could be manipulated in genetically altered organisms whose memory could then be tested to reveal any effects. Thus it was ascertained that *Drosophila* olfactory associative memory does indeed suffer when the equilibrium of MAPs and MTs is disturbed (Chapter III) thus suggesting that the neural cytoskeleton plays a role in memory encoding and retrieval beyond those that were traditionally reported.

The next step was to further investigate the properties of tubulin and MTs since once experimentally implicated in information manipulation, it was not unreasonable to ask whether these protein structures do indeed work as biological and perhaps quantum binary digits (biobits or bioqubits). The dielectric constant and electric dipole moment of tubulin were chosen for closer study since these featured prominently in information manipulation schemes by naturally occurring or fabricated MT networks. Supercomputer-based molecular dynamics simulations were undertaken and the dipole moment was determined (Chapter IV).

In order to check the validity of the computer simulations, an experimental determination of the dielectric constant of tubulin and MTs was needed. This was undertaken in the high frequency (optical) region (using refractometry and surface plasmon resonance) and low frequency region (using dielectric spectroscopy) and it was found that the rather high dipole moment suggested by simulation is reasonable (Chapter V).

As a result of these efforts, novel experimental techniques and theoretical models have been developed that point the way to several directions of further experimental research from molecular electronics and proteomics to actually at least one way of *directly* testing for quantum coherence and entanglement in biological matter (Chapter VI).

Chapter VII brings together the different approaches and unifies the knowledge gained.



## **1.2 Tubulin and Microtubules**

Proteins are the ubiquitous living machines inside all cells performing everything from signal and energy transduction to movement, force generation, catalysis of reactions and -it has been suggested, information manipulation and storage in the case of tubulin, microtubules and associated proteins.

### **1.2.1 Tubulin Biochemistry**

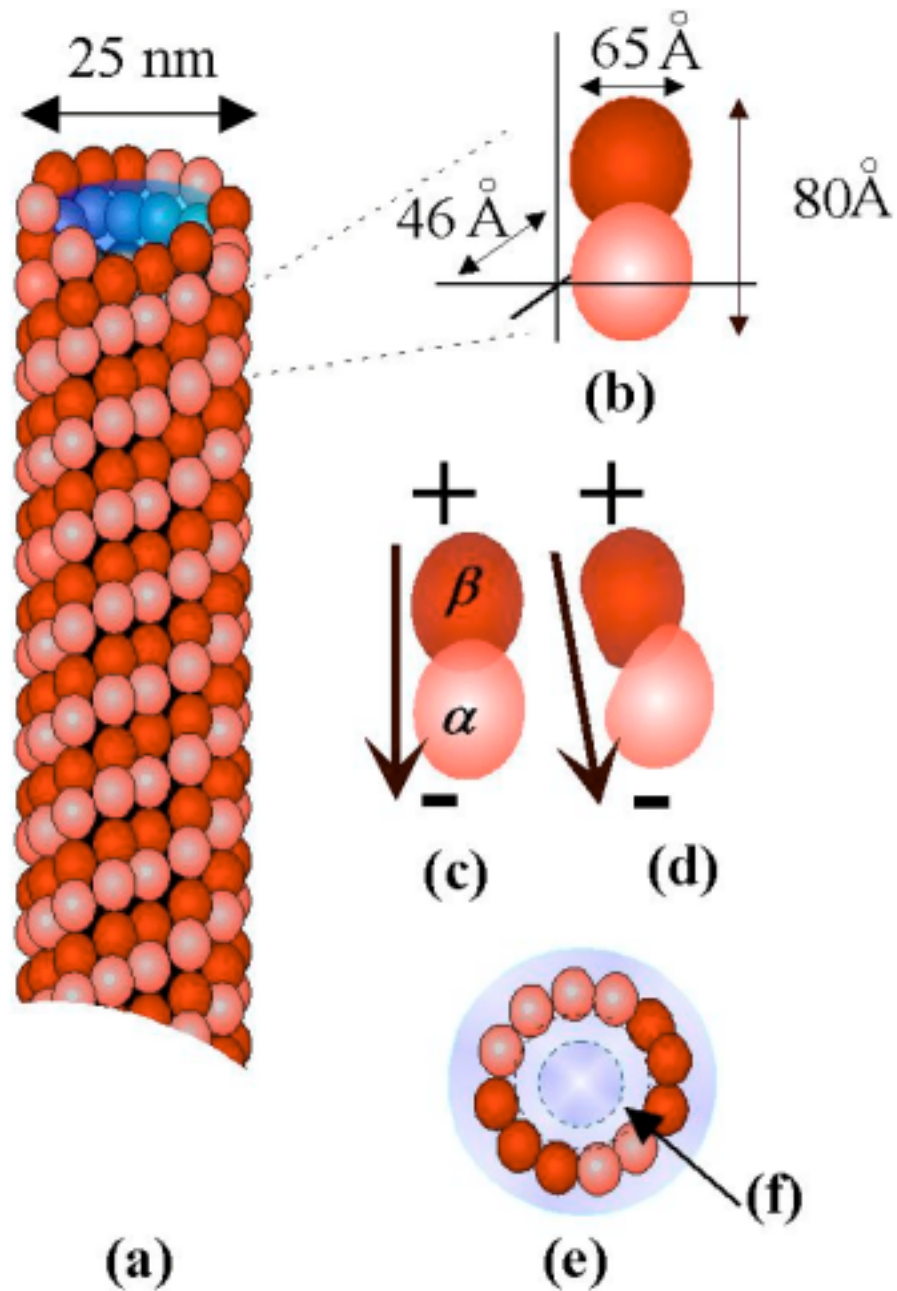
Tubulin is a common polar protein found mainly in the cytoskeleton of eukariotic cells and especially enriched in brain tissue. Many of its properties have been studied both experimentally and theoretically because of its importance in mitosis, its role as the building block of microtubules and its relevance to the pathology of several neurodegenerative diseases including cancer and Alzheimer's.

Although the structure of tubulin has been solved to better than 3.7Å, by electron crystallography [4, 5], the dipole moment has only been calculated via computer simulations presented in this thesis (see Chapter IV) and elsewhere [6].

MTs are hollow (25nm-outer diameter, 14nm inner diameter), [Fig. 1 (a)] tubes forming the main component of the cytoskeleton and apart from giving shape and support to the cell, they also play a major role in cellular transport and have been hypothesized to be central in cellular information processing. The structure of MTs has been the subject of comprehensive study using electron and optical microscopy and it transpires that MTs come in a variety of arrangements the predominant of which is a 5-start, period-13 helical tube of dimers which resembles a corn ear [Fig.1 (a)] made out of

13 offset protofilaments. Recent measurements [4] have confirmed earlier data suggesting that the tubulin heterodimer has dimensions 46 X 80 X 65 Å [Fig. 1 (b)]. Under normal physiological conditions, tubulin is found as a heterodimer, consisting of two nearly identical monomers called the  $\alpha$ - and  $\beta$ - tubulin each of molecular weight of about 55kDalton [5]. GDP-GTP exchange (hydrolysis) releases approximately 0.42eV per molecule and can be modeled by a conformational change resulting in a 27°42' angle [6] between the original line connecting the centers of the  $\alpha$  and  $\beta$  monomers and the new center-to-center line as shown in Fig. 1 (d). Note that for free tubulin, the energy needed for this conformational change is roughly 200 times lower than a conventional silicon-based binary switch and about 30 times more than thermal noise at room temperature. Therefore, at least energy-wise these two conformations can act as the basis for a naturally occurring or fabricated biobit.

There exists a large number of studies dealing with microtubule (MT) dynamics, and various scenaria have been proposed for explaining the dynamic behavior of MTs. At this point however, there is controversy even as to the correct mechanism of polymerization with the “GTP cap” theory [38] facing alternatives such as those described in [7].



**Fig. 1 Microtubules and Tubulin.** MTs are hollow (25nm-outer diameter, 14nm inner diameter) tubes forming the main component of the cytoskeleton **(a)** Typical microtubule made of 13 tubulin protofilaments. **(b)** dimensions of the  $\alpha\beta$ -heterodimer. **(c)** GTP-tubulin. **(d)** GDP-tubulin **(e)** a cross-section of the MT showing water environment **(f)** thin isolated region that has been theoretically shown to be equivalent to a quantum optical (QED) cavity[8].

Unless otherwise specified, ‘tubulin’ refers to the  $\alpha\beta$ -dimer. Tubulin can bind guanosine 5’ triphosphate (GTP) in which case it exists in an energy-rich form that favors polymerization, or it can bind guanosine 5’ diphosphate (GDP-tubulin) thus being in an energy-poor form (GDP-tubulin) that favors dissociation. Above 0° C, free tubulin can self-assemble into MTs in vitro provided the buffer contains sufficient GTP and the concentration is above critical (about 1mg/mL) so that sufficient nucleation sites exist. The size of the minimum nucleus required to start polymerization is not exactly understood. Counterintuitively, MTs depolymerize at or below 0° C and polymerization is facilitated by higher temperatures peaking at 37° C.

Certain interesting phenomena arise during the (de-) polymerization of tubulin such as length oscillations, treadmilling etc. generally referred to as ‘dynamic instability’ and these have been studied extensively [9, 10] but are not directly relevant to our analysis at this stage as such phenomena can be avoided in vitro by choosing appropriate environments.

### **1.2.2 Tubulin Biophysics**

A measurement of the tubulin electric dipole moment will be useful in simulations of MTs that aim at understanding the polymerization mechanism, as it can be incorporated in the various models as an experimentally determined parameter. For similar reasons, studies involving the computer simulation of MT networks as cellular automata will also benefit from such a measurement. Furthermore, drug interactions with tubulin are currently under investigation and it has been theorized that electric

dipole moment 'flips' are responsible for London forces during interaction of tubulin with other molecules possessing dipole moments such as general anesthetic molecules [11].

A simplistic estimate of the tubulin dipole moment  $\mathbf{p}$  based on a mobile charge of 18 electrons multiplied by a separation of 4nm gives a magnitude of  $\mathbf{p} = 4 \times 10^{-27} \text{ C m}$  (or 1200 Debye) while using a more sophisticated molecular simulation,  $\mathbf{p}$  has been quoted at 1714 Debye [6]. At physiological pH (=7.2) MTs are negatively charged [12,13,14] due to the presence of a 15-residue carboxyl terminus 'tail' and there have been suggestions that this C-terminus is important in polymerization, protein interactions and perhaps charge conduction [14]. This has not been included in the electron crystallography data of Nogales and Downing [4,5] so all values concerning the dipole moment are quoted with the understanding that  $\mathbf{p}$  has been calculated ignoring the effect of the C-terminus. It is also known that at pH 5.6 MTs become neutral. Finally, there have been some preliminary experiments aimed at measuring the electric field around MTs [15,16,17] indicating that MTs could be ferroelectric.

Apart from the above observations, there exists little experimental evidence concerning tubulin's and MTs' electrical properties. On the other hand, there has been a large number of publications of theoretical work describing various electrical and optical properties that tubulin and MTs are expected to have based on their structure and function. Ferroelectricity (the property related to the spontaneous abrupt orientation of dipoles for an above-threshold externally applied electric field) has been thoroughly explored and so far supported by the analysis in [18]. The MTs' paracrystalline

geometrical structure has been implicated in error-correcting codes [19]. Energy loss-free transport along MTs has also been theoretically shown in [8] and the presence of “kink like excitations” or solitons has also been suggested as an energy-transfer mechanism in MTs [20]. Many models exist regarding the exact nature of these excitations and waves but they all depend on the dipole moment of tubulin and its ability to flip while in the polymerized state so we will collectively call them “flip waves”. Depending on the model and the parameters assumed, the speed of such waves has been estimated to be  $10^{2\pm1}$  m/s. Note that although biochemically it seems MTs are made predominantly of GDP-tubulin, this does not mean that the dipole flips are ‘frozen-out’ since intramolecular electron motion can still occur in the hydrophobic pockets of the tubulin heterodimer. Detection of such waves would be a major step towards understanding the function of MTs and also towards using them as nanowires for bioelectronic circuits.

## 1.3 Motivation

### 1.3.1 Tubulin and Classical Molecular Electronics

Recent efforts have concentrated on identifying various chemical substances with appropriate characteristics to act as binary switches and logic gates needed for computation. While at present the size of the smallest conventional silicon-based devices is 180nm, molecular devices promise a one or two order of magnitude reduction in this minimum. For instance, rotaxanes have been considered as switches and/or fuses [21] and carbon nanotubes as active channels in field effect transistors [22]. Many of these are not suitable for placement on traditional chips [23] or for forming ordered networks while virtually all of these attempt to hybridize some kind of electrical wires to chemical substrates in order to obtain current flows. This requirement adds a level of complexity to the task because of the need for appropriate nanomanufactured wires and connections. The work presented here is suggestive of a different approach. The role of the binary states can be played not by the presence or bulk movement of electrons but by naturally occurring conformational states of protein (tubulin) molecules. The external interaction with these states may be performed by coupling laser light to specific spots of the MT network. Signal propagation can be achieved by travelling electric dipole moment flip waves along protofilaments and MTs while modulation can be achieved by MAP binding that creates “nodes” in the MT network. In this proposed scheme for information manipulation, there is no bulk transfer of charge or mass involved. Permanent information encoding can be achieved by creating geometrical arrangements via placing

the MTs on chips spotted with appropriate chemicals (e.g. taxol, zinc, colchicine) to force specific features such as centers, sheets, spirals or elongated structures to emerge from the MT self-assembly.

The end products of tubulin polymerization can be controlled by temperature and application of chemicals and MAPs to yield closely or widely spaced MTs, centers, sheets, rings and other structures [24,25] thus facilitating fabrication of nanowires, nodes and networks. Charge conduction by peptides/natural switches has been under investigation using femtosecond laser pulses and the results show that electron transfer exists in peptides even at low energies [26]. Femtosecond processes are taking place as charges jump across peptide backbones in certain favorable conformations that provide extreme transduction efficiency, or charges are stopped by those same peptides assuming a non-conducting conformation [27]. These general properties of peptides make proteins even more attractive as molecular switch candidates. Finally, these assemblies of protein are ideal for implementing fault-tolerant operation, as massive redundancy is possible due to the relative ease of obtaining large amounts of protein polymerized to specifications, e.g. etched on chips.

### **1.3.2 Quantum Computing and Quantum Brain Hypotheses**

All of the microtubule-based “quantum brain” models that abound today have at their core the assumption that the tubulin electric dipole moment is capable of flips while in the polymerized state and starting from that assumption, predictions have been developed such as long-lived superposed and entangled states among tubulin dimers [28]



and long-range non-neurotransmitter based communication among neurons [11]. Interaction between water molecule dipoles and the tubulin dipole plays a central role in the models predicting ferroelectricity along MT protofilaments, emission of coherent photons, intracellular quantum teleportation of dipole quanta states [28] and other controversial yet fascinating features. As explained in Chapter VI, a minimally modified design of the SPR apparatus built and used for this project, coupled to a entangled photon source and a correlation device might be capable of detecting the often conjectured mesoscopic (of order micrometers) bulk coherence and partial quantum entanglement of dipole moment states, existence of which will cast biomolecules as appropriate candidates for the implementation of bioqubits.

## CHAPTER II

### MODELS OF TUBULIN AND IMPLICATIONS

#### 2.1 Introduction

##### 2.1.1 Background

Observable quantum effects in biological matter such as proteins are naively expected to be strongly suppressed, mainly due to the macroscopic nature of most biological entities as well as the fact that such systems live at near room temperature. These conditions normally result in a very fast collapse of the pertinent wave functions to one of the allowed classical states. However, it is suggested here that under certain circumstances it is in principle possible to obtain the necessary isolation against thermal losses and other environmental interactions, so that meso- and macroscopic quantum-mechanical coherence, and conceivably entanglement extending over scales that are considerably larger than the atomic scale, may be achieved and maintained for times comparable to the characteristic times for biomolecular and cellular processes.

In particular, it has been shown [8] how microtubules (MTs) [29] can be treated as quantum-mechanically isolated (QED) cavities, exhibiting properties analogous to those of electromagnetic cavities routinely used in quantum optics [30,31,32,33]. Recently, this speculative model has been supported by some indirect experimental evidence. It has been experimentally shown [34], that it is possible to maintain partial entanglement of the bulk spin of a macroscopic quantity of Caesium (Cs) atoms

( $N=10^{12}$ ), at room temperature, for a relatively long time (0.5ms). Note that in this experiment, the large quantity of atoms was of paramount importance in creating and maintaining the entanglement, and even though the gas samples were in constant contact with the environmental heat bath, by using a careful experimental arrangement, Julsgaard et.al. managed to detect the existence of entanglement for a much longer time than one would intuitively expect. Here, the main features of the Nanopoulos et al. QED model of the quantum mechanical properties of MTs (described in detail in [8,28]), and we exhibit its relevance of the Julsgaard et al. experiment. A direct consequence of this model for MTs as QED cavities is that virtually every experimentally known QED-cavity-based observation may have an analogue in living MTs and we show this analytically with the specific case of intra- and inter-cellular dissipation-less energy transfer and quantum teleportation of coherent quantum states.

### **2.1.2 Intracellular Energy Transfer**

Energy transfer across cells, without dissipation, had been first speculated to occur in biological matter by Fröhlich [35]. The phenomenon conjectured by Fröhlich was based on a one-dimensional superconductivity model: a one dimensional electron system with holes, where the formation of solitonic structures due to electron-hole pairing results in the transfer of electric current without dissipation. Fröhlich suggested that, if appropriate solitonic configurations are formed inside cells, energy in biological matter could also be transferred without any dissipation (superefficiently). This idea has

lead theorists to construct various models for cellular energy transfer, based on the formation of kink classical solutions [36].

In these early works, no specific microscopic models had been considered [36]. In 1993 Sataric et al. constructed a classical physics model for microtubule dynamics [37], in which solitons transfer energy across MTs without dissipation. In the past, quantum aspects of this one-dimensional model have been analyzed, and a framework for the consistent quantization of the soliton solutions was developed [8]. That work suggested that such semiclassical solutions may emerge as a result of 'decoherence' due to environmental interactions, in agreement with ideas in [38].

The basic assumption used in creating the model of ref. [8] was that the building blocks of MTs, the tubulin molecule dimers, can be treated as elements of Ising spin chains (one-space-dimensional structures). The interaction of each tubulin chain (protofilament) with the neighboring chains and the surrounding water environment has been accounted for by suitable potential terms in the one-dimensional Hamiltonian. The model describing the dynamics of such one-dimensional sub-structures was the ferroelectric distortive spin chain model of [37].

Ferroelectricity is an essential ingredient of the quantum-mechanical mechanism of energy transfer that we propose. It has been speculated [39] that the ferroelectric nature of MTs will be that of hydrated ferroelectrics, i.e. the ordering of the electric dipole moment of the tubulin molecules will be due to the interaction of the tubulin dimers' electric dipoles with the ordered-water molecules in the interior and possibly exterior of the microtubular cavities. Ferroelectricity induces a dynamical dielectric

'constant'  $\epsilon(\omega)$  which is dependent on the frequency  $\omega$  of the excitations in the medium. Below a certain frequency, such materials are characterized by almost vanishing dynamical dielectric 'constants', which in turn implies that electrostatic interactions inversely proportional to  $\epsilon$  will be enhanced, and thus become dominant against thermal losses. In the case of microtubules, the pertinent interactions are of the electric dipole type, scaling with the distance  $r$  as  $1/(\epsilon r^3)$ . For ordinary water media, the dielectric constant is of order 80. In the ferroelectric regime however, this  $\epsilon$  is diminished significantly. As a result, the electric dipole-dipole interactions may overcome the thermal losses proportional to  $k_B T$  at room temperature inside the interior cylindrical region of MT bounded by the dimer walls of thickness of order of a few Å [8] see Fig. 1.

### 2.1.3 Cavities

It is known experimentally [40], that in a thin exterior neighborhood of MTs there are areas of atomic thickness, consisting of charged ions, which isolate the MT from thermal losses. This means that the electrostatic interactions overcome thermal agitations. It seems theoretically plausible, albeit yet unverified, that such thermally isolated exterior areas can also operate as cavity regions, in a manner similar to the areas interior to MTs. At this point, it is unclear whether there exist the necessary coherent dipole quanta in the ionic areas. Further experimental and theoretical (simulation) work needs to be done regarding this issue and this is in progress.

Once such an isolation is provided, one can treat the thin interior regions as electromagnetic cavities in a way similar to that of QED cavities. Note that the role of

MT as waveguides has been proposed by S. Hameroff already some time ago [41]. In this scenario on the other hand, we are interested in isolated regions inside the MT that play the role of QED cavities.

QED cavities are well known for their capacity to sustain in their interior coherent modes of electromagnetic radiation. Similarly, one expects that such coherent cavity modes will occur in the thin interior regions of MTs bounded by the protein dimer walls. Indeed, as was discussed in [8], these modes are provided by the interaction of the electric dipole moments of the ordered-water molecules in the interior of MT with the quantized electromagnetic radiation [42,43]. Such coherent modes are termed dipole quanta. It is the interaction of such cavity modes with the electric dipole excitations of the dimers that leads to the formation of coherent (dipole) states on the tubulin dimer walls of MTs. A review of how this can happen, and what purely quantum effects can emerge from the QED nature of MTs, will be the main topic of this Chapter.

A concise exposé of the mechanism described in [8] is presented that justifies the application of quantum physics to the treatment of certain aspects of MT dynamics. An analogy of this mechanism to the experimental setup used by Julsgaard et al. [44] is drawn. A straight forward calculation of how quantum teleportation of states can occur in MTs, in direct analogy to the suggested experimental quantum teleportation in optical cavities that has been observed recently [45,46] is performed. A parallel between certain geometrical features of MTs such as their ordered structure which obeys a potentially information-encoding code is illustrated and suggestions to exploit for this for (quantum) error-correction and dense coding are put forth.

## 2.2 Quantum Coherence in Biological Matter?

### 2.2.1 Tubulin, Microtubules and Coherent States

Tubulin was described in detail in Chapter I. The interior of the MT, seems to contain ordered water molecules [8] , which implies the existence of an electric dipole moment and an electric field. We stress that the intracellular ordered water which is full of proteins and other molecules is different from ordinary water in various respects e.g. as is implied in [47]. Free tubulin can self-assemble into MTs both in vivo and in vitro where the most common arrangement of the tubulin dimers is such that, if one treats them as points, they resemble triangular lattices on the MT surface. It has been put forward that each dimer has two hydrophobic protein pockets, containing  $2 \times 18$  unpaired electrons [29] that have at least two possible configurations associated with the GTP and GDP states of tubulin, which we will call  $\uparrow$  and  $\downarrow$  electron (or equivalently electric dipole moment) conformations respectively.

Using the fact that a typical 'distance' for the transition between the  $\uparrow$  and  $\downarrow$  conformations is of order of the distance between the two hydrophobic dimer pockets,  $\sim 4$  nm, a simplistic estimate of the free tubulin electric dipole moment  $d$  can be obtained based on a mobile charge of  $\sim 10$  electrons multiplied by this separation of  $\sim 4$  nm giving a magnitude of  $|\mathbf{p}| \sim 6 \times 10^{-27} \text{ C} \cdot \text{m}$ , or  $\sim 2 \times 10^3$  Debye (D) where  $1\text{D} = 3.338 \times 10^{-30} \text{ C} \cdot \text{m}$ . In Chapter IV a sophisticated molecular dynamics simulation, gives a value of 1714 Debye. It is evident that an experimentally determined electric dipole moment for the tubulin molecule and its dynamics are important areas of study for this field. If we

account for the effect of the water environment that screens the electric charge of the dimers by the relative dielectric constant of the water, which is will be denoted by  $\kappa = \epsilon / \epsilon_0 = 80$ , we arrive at a value

$$p_{(\text{dimer})} = 3 \times 10^{-28} \text{C} \times \text{m} \quad (1)$$

Note that under physiological conditions, the unpaired electric charges in the dimer may lead to even further suppression of  $p_{(\text{dimer})}$ .

At physiological pH ( $\approx 7.2$ ) MTs are negatively charged [13] due to the presence of a 15-residue carboxyl-terminus 'tail' and there have been suggestions that this C-terminus is important in polymerization, protein interactions and perhaps charge conduction [40]. This terminus has not been included in the electron crystallography data of Nogales and Downing [4,5] so all values concerning the dipole moment are quoted with the understanding that  $p$  has been calculated ignoring the effect of the C-terminus. It is also known that at pH 5.6 MTs become neutral. Finally, there have been some preliminary experiments aimed at measuring the electric field around MTs [15,16,17] indicating that MTs could be ferroelectric, as has been suggested in the models of [8] and [39]. Note that although the 'caps' of the MT contain both GTP and GDP tubulin, it is well known experimentally [12] that the tubulin comprising the 'trunk' of the MT is GDP-tubulin incapable of acquiring a phosphate and becoming GTP tubulin. However, this does not preclude electric-dipole moment flip wave propagation down the MT, as a flip at the cap can be propagated without phosphorylation or



hydrolysis but rather via the mechanism suggested below. In view of this, the value of the yet undetermined electric dipole moment direction flip angle  $\theta_{\text{flip}}$  is much smaller than the  $27^{\circ}42'$  value for free tubulin. The  $\uparrow$  and  $\downarrow$  states still exist, but are hard to observe experimentally as they are not associated with a large-scale geometrical mass shift. Note that virtually all of the MT-based "quantum brain" hypotheses today fail to take this into account and instead wrongly suggest that  $\theta_{\text{flip}}$  is of the order of  $27^{\circ}$  and that such large distortions occur in the trunk of the polymerized MT.

In standard models for the simulation of MT dynamics [37], the physical degree of freedom which is relevant for the description of energy transfer is the projection of the electric dipole moment on the longitudinal symmetry axis (x-axis) of the MT cylinder. The  $\theta_{\text{flip}}$  distortion of the  $\downarrow$ -conformation leads to a displacement  $u_n$  along the x-axis. This way, the effective system is one-dimensional (spatial), and one has the possibility of being quantum integrable [8].

It has been suggested for quite some time that information processing via interactions among the MT protofilament chains can be sustained on such a system, if the system is considered as a series of interacting Ising chains on a triangular lattice. For such schemes to work, one must first show that the electromagnetic interactions among the tubulin dimers are strong enough to overcome thermal noise. It is due to this problem that such models for intra-neuronal information processing have been criticized as unphysical [49]. Classically, the various dimers can only be in the  $\uparrow$  and  $\downarrow$  conformations. Each dimer is influenced by the neighboring dimers resulting in the

possibility of a transition. This is the basis for classical information processing, which constitutes the picture of a (classical) cellular automaton.

If we assume (and there is theoretical basis for such an assumption [8]) that each dimer can find itself in a superposition of  $\uparrow$  and  $\downarrow$  states, a quantum nature results. Tubulin can then be viewed as a typical two-state quantum mechanical system, where the dimers couple to conformational changes with  $10^{-9}$ - $10^{-11}$  sec transitions, corresponding to an angular frequency  $\omega \sim 10^{10}$ - $10^{12}$  Hz. In this approximation, the upper bound of this frequency range is assumed to represent (in order of magnitude) the characteristic frequency of the dimers, viewed as a two-state quantum-mechanical system:

$$\omega_0 \sim (10^{12}) \text{ Hz} \quad (2)$$

Let  $u_n$  be the displacement field of the  $n$ -th dimer in a MT chain. The continuous approximation proves sufficient for the study of phenomena associated with energy transfer in biological cells, and this implies that one can make the replacement

$$u_n \rightarrow u(x,t) \quad (3)$$

with  $x$  a spatial coordinate along the longitudinal symmetry axis of the MT. There is a time variable  $t$  due to fluctuations of the displacements  $u(x)$  as a result of the dipole oscillations in the dimers.

The effects of the neighboring dimers (including neighboring chains) can be phenomenologically accounted for by an effective potential  $V(u)$ . In the model of ref. [37] a double-well potential was used, leading to a classical kink solution for the  $u(x,t)$  field. More complicated interactions are allowed in the picture of ref. [8], where we have considered more generic polynomial potentials.

The effects of the surrounding water molecules can be accounted for by a viscous force term that damps out the dimer oscillations,

$$F = -\gamma \partial_t u \quad (4)$$

with  $\gamma$  determined phenomenologically at this stage. This friction should be viewed as an environmental effect, which however does not lead to energy dissipation, as a result of the non-trivial solitonic structure of the ground state and the non-zero constant force due to the electric field. This is a well-known result, directly relevant to energy transfer in biological systems [36].

The effective equation of motion for the relevant field degree of freedom  $u(x,t)$  reads:

$$u''(\xi) + \rho u'(\xi) = P(u) \quad (5)$$

where  $\xi = x - vt$ ,  $v$  is the velocity of the soliton,  $\rho$  is proportional to  $\gamma$  [37], and  $P(u)$  is a polynomial in  $u$ , of a certain degree, stemming from the variations of the potential  $V(u)$

describing interactions among the MT chains [8]. In the mathematical literature [50] there has been a classification of solutions of equations of this form. For certain forms of the potential [8] the solutions include kink solitons that may be responsible for dissipation-free energy transfer in biological cells [36]:

$$u(x,t) \sim c_1(\tanh[c_2(x-vt)] + c_3) \quad (6)$$

where  $c_1, c_2, c_3$  are constants depending on the parameters of the dimer lattice model. For the form of the potential assumed in the model of [37], there are solitons of the form

$$u(x,t) = c'_1 + \frac{c'_2 - c'_1}{1 + e^{c'_3(c'_2 - c'_1)(x-vt)}}, \text{ where again } c'_i \text{ where } i=1,2,3 \text{ are appropriate constants.}$$

A semiclassical quantization of such solitonic states has been considered in [8]. The result of such a quantization yields a modified soliton equation for the (quantum corrected) field  $u_q(x,t)$  [51]

$$\partial_t^2 u_q(x,t) - \partial_x^2 u_q(x,t) + M^{(1)}[u_q(x,t)] = 0 \quad (7)$$

with the notation  $M^{(n)} = e^{\frac{1}{2}(G(x,x,t) - G_0(x,x))} \frac{\partial^2}{\partial z^2} U^{(n)}(z) \Big|_{z=u_q(x,t)}$  and  $U^n \equiv d^n U / dz^n$  where the quantity  $U$  denotes the potential of the original soliton Hamiltonian, and  $G(x,y,t)$  is a bilocal field that describes quantum corrections due to the modified boson field around the soliton. The quantities  $M^{(n)}$  carry information about the quantum corrections. For the

kink soliton (eq. 6) the quantum corrections (7) have been calculated explicitly in ref. [51], thereby providing us with a concrete example of a large-scale quantum coherent state.

A typical propagation velocity of the kink solitons (e.g. in the model of ref. [37]) is  $v \sim 2$  m/sec, although, models with  $v \sim 20$  m/sec have also been considered [52]. This implies that, for moderately long microtubules of length  $L \sim 10^{-6}$  m, such kinks transport energy without dissipation in

$$t \sim 5 \times 10^{-7} \text{ sec} \quad (8)$$

Energy will be transferred super-efficiently via this mechanism only if the decoherence time is of the order of, or longer than, this time. We shall see in fact that indeed such time scales are comparable to, or smaller in magnitude than, the decoherence time scale of the coherent (solitonic) states  $u_q(x,t)$ . This then implies that fundamental quantum mechanical phenomena may be responsible for frictionless, dissipationless super-efficient energy (and signal) transfer and/or transduction across microtubular networks in the cell.

### 2.2.2 Microtubules as Cavities

In ref. [8] a microscopic analysis of the physics underlying the interaction of the water molecules with the dimers of the MT was presented. This interaction is

responsible for providing the friction term (4) in the effective (continuum) description. Below this scenario is briefly reviewed.

As a result of the ordered structure of the water environment in the interior of MTs, there appear collective coherent modes, the so-called dipole quanta [42]. These arise from the interaction of the electric dipole moment of the water molecule with the quantized radiation of the electromagnetic field [43], which may be self-generated in the case of MT arrangements [8,52]. Such coherent modes play the role of 'cavity modes' in the quantum optics terminology. These in turn interact with the dimer structures, mainly through the unpaired electrons of the dimers, leading to the formation of a quantum coherent solitonic state that may extend even over the entire MT network. As mentioned above, such states may be identified [8] with semi-classical solutions of the friction equations (5). These coherent, almost classical, states should be viewed as the result of decoherence of the dimer system due to its interaction/coupling with the water environment [38].

Such a dimer/water coupling can lead to a situation analogous to that of atoms interacting with coherent modes of the electromagnetic radiation in quantum optical cavities, namely to the so-called Vacuum-Field Rabi Splitting (VFRS) effect [32]. VFRS appears in both the emission and absorption spectra of atoms [30] in interaction with a coherent mode of electromagnetic radiation in a cavity. For our purposes below, we shall review the phenomenon by restricting ourselves for definiteness to the absorption spectra case.

Consider a collection of  $N$  atoms of characteristic frequency  $\omega_0$  inside an electromagnetic cavity. Injecting a pulse of frequency  $\Omega$  into the cavity causes a doublet structure (splitting) in the absorption spectrum of the atom-cavity system with peaks at:

$$\Omega = \omega_0 - \Delta/2 \pm (1/2)(\Delta^2 + 4N\lambda^2)^{1/2} \quad (9)$$

where  $\Delta = \omega_c - \omega_0$  is the detuning of the cavity mode, of frequency  $\omega_c$ , compared to the atomic frequency. For resonant cavities the splitting occurs with equal weights

$$\Omega = \omega_0 \pm \lambda\sqrt{N} \quad (10)$$

Notice here the *enhancement* of the effect for multi-atom systems  $N \gg 1$ . The quantity  $2\lambda\sqrt{N}$  is called the 'Rabi frequency' [32]. From the emission-spectrum analysis an estimate of  $\lambda$  can be inferred which involves the matrix element,  $\underline{d}$ , of atomic electric dipole between the energy states of the two-level atom [32]:

$$\lambda = \frac{E_c \underline{d} \cdot \underline{p}}{\hbar} \quad (11)$$

where  $\underline{p}$  is the cavity (radiation) mode polarization, and

$$E_c \sim \left( \frac{2\pi\hbar\omega_c}{\epsilon V} \right) \quad (12)$$

is the r.m.s. vacuum (electric) field amplitude at the center of a cavity of volume  $V$ , and of frequency  $\omega_c$ , with  $\epsilon$  being the dielectric constant of the medium inside the volume  $V$ . In atomic physics the VFRS effect has been confirmed by experiments involving beams of Rydberg atoms resonantly coupled to superconducting cavities [33].

In the analogy between the thin cavity regions near the dimer walls of MTs with electromagnetic cavities, the role of atoms is played by the unpaired two-state electrons of the tubulin dimers [8] oscillating with a frequency (2). To estimate the Rabi coupling between cavity modes and dimer oscillations, one should use (11) for the MT case.

We have used some simplified models for the ordered-water molecules, which yield a frequency of the coherent dipole quanta ('cavity' modes) of order [8]:

$$\omega_c \sim 6 \times 10^{12} \text{ Hz} \quad (13)$$

Notably this is of the same order of magnitude as the characteristic frequency of the dimers (2), implying that the dominant cavity mode and the dimer system are almost in resonance in the model of [8]. Note that this is a feature shared by atomic physics systems in cavities, and thus we can apply the pertinent formalism to our system. Assuming a relative dielectric constant of water w.r.t to that of vacuum  $\epsilon_0$ ,  $\epsilon / \epsilon_0 \sim 80$ , one obtains from (12) for the case of MT cavities:

$$E_c \sim 10^4 \text{ V/m} \quad (14)$$



Electric fields of such a magnitude can be provided by the electromagnetic interactions of the MT dimer chains, the latter viewed as giant electric dipoles [37]. This suggests that the coherent modes  $\omega_c$ , which in our scenario interact with the unpaired electric charges of the dimers and produce the kink solitons along the chains, owe their existence to the (quantized) electromagnetic interactions of the dimers themselves.

The Rabi coupling for the MT case then is estimated from ([dipolerabi](#)) to be of order:

$$\begin{aligned} \text{Rabi coupling for MT} &\equiv \lambda_{\text{MT}} \\ &= \sqrt{N} \lambda_0 \sim 3 \times 10^{11} \text{ Hz} \end{aligned} \tag{15}$$

which is, on average, an order of magnitude smaller than the characteristic frequency of the dimers (2).

In the above analysis, we have assumed that the system of tubulin dimers interacts with a *single* dipole-quantum coherent mode of the ordered water and hence we ignored dimer-dimer interactions. More complicated cases, involving interactions either among the dimers or of the dimers with more than one radiation quantum, which undoubtedly occur in vivo, may affect the above estimate.

The presence of such a coupling between water molecules and dimers leads to quantum coherent solitonic states of the electric dipole quanta on the tubulin dimer walls. To estimate the decoherence time we remark that the main source of dissipation

(environmental entanglement) comes from the imperfect walls of the cavities, which allow leakage of coherent modes and energy. The time scale,  $T_r$ , over which a cavity-MT dissipates its energy, can be identified in our model with the average life-time  $t_L$  of a coherent-dipole quantum state, which has been found to be [8]:  $T_r \sim t_L \sim 10^{-4}$  sec. This leads to a first-order-approximation estimate of the quality factor for the MT cavities,  $Q_{MT} \sim \omega_c T_r \sim 10^8$ . We note, for comparison, that high-quality cavities encountered in Rydberg atom experiments dissipate energy in time scales of  $10^{-3}$ - $10^{-4}$  sec, and thus have  $Q$ 's which are comparable to  $Q_{MT}$  above. The analysis of [8] yields the following estimate for the collapse time of the kink coherent state of the MT dimers due to dissipation:

$$t_{\text{collapse}} \sim 10^{-7} - 10^{-6} \text{ sec} \quad (16)$$

This is larger than the time scale (8) required for energy transport across the MT by an average kink soliton in the models of [8,52]. The result (16), then, implies that quantum physics may be relevant as far as dissipationless energy transfer across the MT is concerned.

Therefore, this specific model is in stark disagreement with the conclusions of Tegmark in [49], i.e. that only classical physics is relevant to the energy and signal transfer in biological matter. Tegmark's conclusions did not take proper account of the possible isolation against environmental interactions, which seems to occur inside certain regions of MTs with appropriate geometry.

We would now like to discuss the feasibility of the above, admittedly speculative, ideas by making a brief report on recent progress made by experimentally demonstrating macroscopic quantum entanglement at room temperature in atomic physics.

### 2.2.3 Ordered Water in Biological Systems

The above scenaria are consistent with independent studies of water in biological matter, which is summarized below.

Recent experimental spectroscopic studies of resonant intermolecular transfer of vibrational energy in liquid water [53] have established that energy is transferred extremely rapidly and along many water molecules before it dissipates. This energy is in the form of OH-stretch excitations and is thought to be mediated by dipole-dipole interactions in addition to a yet unknown mechanism which speeds up the transfer beyond that predicted by the so-called Förster expression for the energy transfer rate between two OH oscillators,  $k$ .

$$k = T_1^{-1} \left( \frac{r_o}{r} \right)^6 \quad (17)$$

where  $T_1$  is the lifetime of the excited state,  $r$  the distance between the oscillators and  $r_o$  the Förster radius. The Förster radius, which is a parameter experimentally determined for each material, characterizes the intermolecular energy transfer and has been

determined by Woutersen et al. [53] to be  $r_0 = 2.1 \pm 0.05 \text{ \AA}$  while the typical intermolecular distance (at room temperature) for water is  $\sim 2.8 \text{ \AA}$ . It is evident from these data that the energy transfer in pure water will be fast (of order 100ps) and yet experimentally it is determined to be even faster than that by one or even two orders of magnitude. Woutersen et al. speculate that this extremely high rate of resonant energy transfer in liquid water may be a consequence of the proximity of the OH groups in liquid water which causes other, higher-order -uples to also exchange energy. Here, we propose another mechanism to explain the rapidity of the energy transfer, namely kink-soliton propagation. This proposition is based on the phenomenological realization that this is exactly the kind of energy transfer that one would expect to see experimentally as a result of the existence of kink-solitons. It is evident that such a mechanism, regardless of exact origin, is ideal for loss-free energy transfer between OH groups located on either different biomolecules or along extended biological structures such as MTs which would be covered (inside and out) with water. Note also that such a mechanism would predict that OH groups in hydrophobic environments would be able to remain in a vibrationally excited state longer than OH groups in hydrophilic environment lending credence to our working assumption that the electrons inside the hydrophobic pockets of the tubulin molecules are sufficiently isolated from thermal noise.

It must be stressed though, that such solitonic states in water may not be quantum in origin in the case of microtubules. The 25 nm diameter of the MT is too big a region to allow for quantum effects to be sustained throughout, as we discussed above. Such solitons may be nothing other than the ones conjectured in [54], which may be

responsible for the optical transparency of the water interior of MTs. Such classical solitons in the bulk of the water interior may co-exist with the quantum coherent states on the dimer walls [8].

#### **2.2.4 Error Correction and Quantum Entanglement of a Macroscopic System**

As we have seen above, under appropriate environmental isolation, it is possible to obtain quantum coherence of macroscopic populations of tubulin dimers in microtubule systems, which can be sustained for long enough times so that dissipationless energy and signal (information) transfer can occur in a cell.

In a recent article [34] Julsgaard et al. describe the macroscopic entanglement of two samples of Cs atoms at room temperature. The entangling mechanism (See Chapter VI for more on entanglement) is a pulsed laser beam and although the atoms are far from cold or isolated from the environment, partial entanglement of bulk spin is unambiguously demonstrated for  $10^{12}$  atoms for  $\sim 0.5$  ms. The system's resilience to decoherence is in fact *facilitated* by the existence of a large number of atoms as even though atoms lose the proper spin orientation continuously, the bulk entanglement is not immediately lost. Quantum Informatics, the science that deals with ways to encode, store and retrieve information written in qubits has to offer an alternative way of interpreting the surprising resilience of the Cs atoms by using the idea of "redundancy". Simply stated, information can be stored in such a way that the logical (qu)bits correspond to many physical (qu)bits and thus are resistant to corruption of content. Yet another way of looking at this is given in the work by Kielpinski et al. [55] where they have

experimentally demonstrated a decoherence-free quantum memory of one qubit by encoding the qubit into the "decoherence-free subspace" (DFS) of a pair of trapped Beryllium  $^9\text{Be}^+$  ions. They achieved this by exploiting a "safe-from-noise-area" of the Hilbert space for a superposition of two basis states for the ions, thus encoding the qubit in the superposition rather than one of the basis states. By doing this they achieved decoherence times on average an order of magnitude longer. Both of the above works show that it is possible to use DFS, error correction and high redundancy to both store information and to keep superpositions and entanglements intact for biologically relevant times in macroscopic systems at high (room) temperature. Thus, it may not be entirely inappropriate to imagine that in biological *in vivo* regimes, one has, under certain circumstances such as specified above, entanglement of tubulin/MT arrangements.

### **2.3 Implications of Quantum Coherence for Cell Function**

The above raises the question of how such phenomena can affect the functioning of cells. In other words, would the existence of such coherent states and the emergence of quantum mechanical entanglement be somehow useful or beneficial to biological function? Is it then reasonable to propose that in certain cases, natural selection may have favored molecules and cellular structures that exhibited and sustained such phenomena? If we accept the notion that according to the laws of quantum physics certain macroscopic arrangements of atoms will exhibit such effects, is it not reasonable then to expect that biomolecules and (by extension) cellular structures and whole cells have 'found' a use for such phenomena and have evolved to incorporate them? We stress that at a given instant in time, the different microtubule coherent states participating in a specific bulk entanglement would be almost identical due to the fact that they are related/triggered by a specific "external agent" (e.g. the passing of a specific train of action potentials.) This is of importance since it increases the system's resilience to decoherence (by entangling a large number of nearly identical states), in addition to facilitating "sharp decision making" (i.e. rapid choice among a vast number of very similar states) as explained in [1] which is presumably a trait favored by natural selection. Here we digress to investigate one possible use of such effects by noting a straight-forward application of entanglement to teleportation of coherent quantum states across and between cells.

### 2.3.1 Biological Quantum Teleportation

We define teleportation as the complete transfer of the coherent state of an MT *without any direct transfer of mass or energy*. This means that the 'receiver' MT finds itself in an identical state to the 'sender' MT. We will demonstrate the way in which, given the possibility for entangled states, teleportation between microtubule A and microtubule C can happen. The use of pure state vectors,  $|\Psi\rangle$ , to describe the coherent states along a MT arrangement is justifiable since they do not obey the ordinary Schrödinger evolution equation. Instead, they obey the stochastic equations of open systems, of the form discussed in [56]. Nowhere in the proof of teleportation below are the precise forms of the evolution equations used. As argued in [56], by using appropriate stochastic (Langevin type) equations one may recover, for instance, the standard Lindblad form of evolution equations for the corresponding density matrices  $\rho = \text{Tr}_M |\Psi\rangle\langle\Psi|$ , where M is an appropriate subset of environmental degrees of freedom, non-accessible to the observer.

A coherent state in microtubule A (referred to as simply A and designated as  $|\Psi(A)\rangle$ ) of the (collective) dipole moment(s) being in either of the two classically allowable states with probability amplitude  $\omega_0$  and  $\omega_1$  can be written as:

$$|\Psi(A)\rangle = \omega_0|0\rangle + \omega_1|1\rangle \quad (18)$$

Step 1: The cell finds itself with microtubule B and microtubule C -which can be close together or collinear- in an entangled state written as:



$$|\Psi(B,C)\rangle = (1/\sqrt{2}) (|1_B, 0_C\rangle + |0_B, 1_C\rangle) \quad (19)$$

The combined state of A,B,C can be written as:

$$|\Psi(A,B,C)\rangle = |\Psi(A)\rangle \otimes |\Psi(B,C)\rangle \quad (20)$$

which upon expanding the outer product  $\otimes$  can be written as:

$$|\Psi(A,B,C)\rangle = \frac{1}{\sqrt{2}} \{ \omega_0 (|0_A, 1_B, 0_C\rangle + |0_A, 0_B, 1_C\rangle) + \omega_1 (|1_A, 1_B, 0_C\rangle + |1_A, 0_B, 1_C\rangle) \} \quad (21)$$

We can also express the combined state  $|\Psi(A,B,C)\rangle$  in a different basis, known as the "Bell basis". Instead of  $|0\rangle$  and  $|1\rangle$ , the basis vectors will now be,

$$|\Psi^\pm(A,B)\rangle = \frac{1}{\sqrt{2}} (|0_A, 1_B\rangle \pm |1_A, 0_B\rangle) \quad (22)$$

and

$$|\Phi^\pm(A,B)\rangle = \frac{1}{\sqrt{2}} (|0_A, 0_B\rangle \pm |1_A, 1_B\rangle) \quad (23)$$

In this new basis, our state of the three microtubules  $|\Psi(A,B,C)\rangle$  is written as:

$$\begin{aligned}
|\Psi(A, B, C)\rangle = & \frac{1}{2} \left( |\Psi^+(A, B)\rangle \otimes (\omega_0|0_C\rangle + \omega_1|1_C\rangle) + \right. \\
& |\Phi^+(A, B)\rangle \otimes (\omega_0|1_C\rangle + \omega_1|0_C\rangle) + |\Psi^-(A, B)\rangle \otimes (\omega_0|0_C\rangle + \omega_1|1_C\rangle) + \\
& \left. |\Phi^-(A, B)\rangle \otimes (\omega_0|1_C\rangle + \omega_1|0_C\rangle) \right)
\end{aligned} \tag{24}$$

This concludes the first step of teleporting the state of MT A to MT C.

Step 2: Notice that so far, MT A has not interacted with the environment or cell, i.e. the coherent state of A which we designated as  $|\Psi(A)\rangle = \omega_0|0_C\rangle + \omega_1|1_C\rangle$  has not been touched. Now the part of the cell containing A and B (the "sender part") makes a "measurement" -which in our case can be an electromagnetic interaction with a passing action potential or the binding of a MAP molecule. If this measurement or forced collapse is done in the Bell basis, on  $|\Psi^\pm(A, B)\rangle$  it will project the state in MT C (!) to:

$$|\Psi^\pm(C)\rangle = \langle \Psi^\pm(A, B) | \Psi(A, B, C) \rangle = \omega_0|0_C\rangle \pm \omega_1|1_C\rangle \tag{25}$$

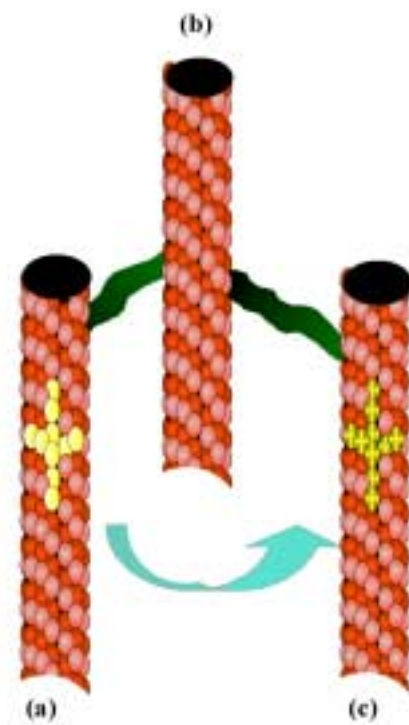
similarly

$$|\Phi^\pm(A, B)\rangle \rightarrow |\Phi^\pm(C)\rangle = \omega_0|1_C\rangle \pm \omega_1|0_C\rangle \tag{26}$$

This effectively concludes the teleportation of the state of MT A to MT C with one caveat. There is a probabilistic nature to this process, which means that MT C may receive the exact copy of the state of MT A i.e.  $|\Psi^+(C)\rangle$  or it may receive a state which is a unitary transformation away from the original  $|\Psi(A)\rangle$  (one of the other three possibilities:  $|\Psi^-\rangle$  or  $|\Phi^\pm\rangle$ . MT C can reproduce the state of MT A if there is a 'hardwired' condition so that when MT C receives  $|\Psi^+(C)\rangle$  it does nothing further, yet if

it receives one of the other three, it performs the correct unitary transformation to obtain the correct state from A. This 'hardwired' behavior can be implemented through the use of codes, not unlike the Koruga bioinformation [57] code that MTs follow. In principle, the exact state correspondence may not even have any significance and instead the information could be encoded in the frequency of transferred states, similar to information being encoded in the frequency of action potentials and not their shapes.

Teleportation is an entirely non-classical phenomenon and has been experimentally demonstrated in matter and light states and combinations of those (see Chapter VI). Currently, the scientific consensus is that teleportation is impossible without entanglement although this may change in the future. Biological teleportation as described above, can be imagined as the basis of intra- and inter- cellular correlation which leads to yoked function (e.g. intracellularly during translation and intercellularly during yoked neuron firing). Experiments to check for such teleportation of states can be designed based on the Surface Plasmon Resonance (SPR) principle [58] as applied to sheets of polymerized tubulin immobilized on a metal film (Chapters V and VI). A graphical representation of biological quantum teleportation of dipole moment states is presented in Fig. 2.

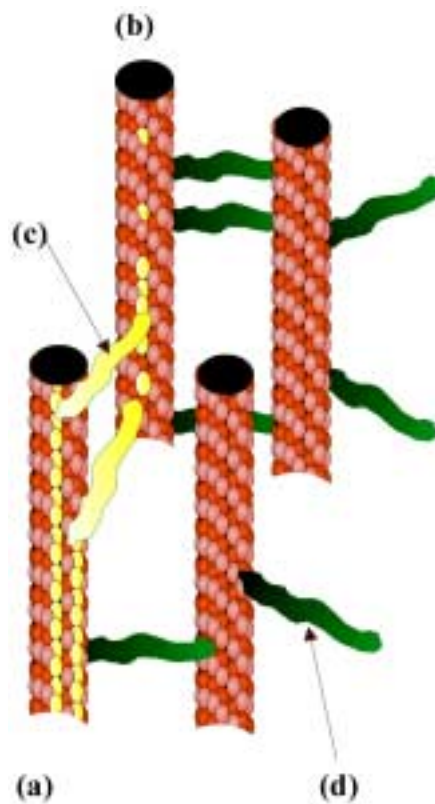


**Fig. 2. Schematic of Quantum Teleportation of Dipole States.** MT (a) sends its state (represented by the yellow cross) to MT (c) without any transfer of mass or energy. Both MT (a) and MT (c) are entangled with MT (b). Entanglement is represented by the presence of connecting MAPs (green).

### 2.3.2 Information Processing by Biopolymers and the Guitar String Model

In the quantum-mechanical scenario for MT dynamics discussed above, as suggested in [8], a quantum-hologram picture for information processing of MT networks emerges. Further, the existence of solitonic quantum-coherent states along the MT dimer walls implies a role for these biological entities as logic gates [59]. Consider, for instance, a node (junction) of three MTs connected by microtubule associated proteins (MAPs) see Fig. 3. The quantum nature of the coherent states makes the

junction interaction probabilistic. Therefore at tube junctions one is facing a Probabilistic Boolean Interaction. The probability for having a solitonic coherent state in a MT branch does depend on its geometric characteristics (such as length). By modulating the length of the tubes and the binding sites of the MAPs a bias can be introduced between bit states which can affect the probabilistic final outcomes. This has obvious implications for information processing by MT networks.



**Fig. 3. An XOR (Exclusive-OR) Logic Gate.** "0" ("1") is represented by absence (presence) of solitonic kink wave of dipole moment flips indicated in yellow. **(a)** Input MT, **(b)** Output MT, **(c)** A MAP transmitting a solitonic kink wave, **(d)** a 'quiet' MAP. MT (a) has two solitons travelling, encountering two MAPs that transmit both solitons to MT (b). In this hypothetical scenario, the solitons arrive out of phase at MT (b) and cancel each other out. The truth table for XOR reads:  $0,0 \rightarrow 0$ ;  $0,1 \rightarrow 1$ ;  $1,0 \rightarrow 1$ ;  $1,1 \rightarrow 0$  and can be realized by an MT arrangement if the Maps are arranged such that each can transmit a soliton independently ut if they both transmit the solitons cancel out, i.e. the two MAPs must be an odd number of dimers apart on MT(a).

Such a binary information system can then provide the basic substrate for quantum information processing inside a (not exclusively neural) cell. In a typical MT network, there may be about  $10^{12}$  tubulin dimers. Although such a number is macroscopic, as discussed earlier there may be subtle "shielding" mechanisms at play. The above scenario is not necessarily *quantum* in nature. An essentially identical argument can be made for information processing via waves of dipole flips or just momentum transfer as a result of propagating conformational changes.

This suggests an obvious model for encoding information in a network of MTs which we shall call the "Guitar String Model" to emphasize the analogy to the way six guitar strings (the MTs) can be pushed by four fingers (MAPs) at different nodes so generate hundreds of different chords (engrams). If propagating dipole moment flips are indeed carrying signals inside the cell then the nodes in the network can affect this propagation in a large variety of ways. A limited set of MTs with a limited set of MAP binding sites can have a very large set of engrams. This also suggests a way for new memories to form and old to be erased by simply changing the distribution of MAPs.

## 2.4 Conclusions

If it is experimentally confirmed that treating MTs as QED cavities is a fair approximation to their behavior, one can propose that nature has provided us with the necessary structures (microtubules) to operate as the basic substrate for quantum computation either in vivo, e.g. intracellularly, or in vitro, e.g. in fabricated bioqubit circuits. Such a development would pave the way to construct quantum computers by

using microtubules as building blocks, in much the same way as QED cavities in quantum optics are currently being used in successful attempts at implementing qubits and gates [46].

## CHAPTER III

### TAU ACCUMULATION IN *DROSOPHILA* MUSHROOM BODY NEURONS

#### RESULTS IN NEUROPLASTICITY IMPAIRMENT

##### 3.1 Introduction

In order to test some of the predictions of the models discussed in Chapters I and II, an in-vivo neurobiological behavioral study was undertaken. The goal was to experimentally investigate whether memory is affected by perturbations in the microtubular (MT) cytoskeleton. We tried disturbing the MTs as little as possible, avoiding perturbing the cytoskeleton by formation of such large protein aggregates as neurofibrillary tangles (NFTs) that could effectively 'strangle' the neuron disrupting or even stopping intracellular (axonal) transport. In addition, NFTs and/or amyloid or senile plaques (APs or SPs) have been unequivocally shown to contribute to neurodegeneration and eventual neuronal death and it is reasonable to expect a dying neuron to dysfunction, regardless of the state of its MTs. We also avoided causing any developmental problems by selecting drivers with appropriate temporal activity. Associative olfactory learning and memory were the types of memory accessible to us with the transgenic *Drosophila* behavior analysis system.

Since this is a dissertation addressed mostly to physicists an effort has been made to explain potentially unfamiliar biological terms and procedures. Following established standards in genetics, small case italics such as *tau* indicate the *gene* that codes for the protein TAU indicated in capitals. Strains or lines of transgenic animals (animals that



have been genetically manipulated and contain extra genes) are named somewhat arbitrarily so here we use *b*-, *h*-, or *d*-, indicating bovine- human- or *Drosophila*- (native) derived- genes while a few letters identifying the source (usually initials of the persons who obtained the strain) are included in an end identifying field such as in: *htauwtl* meaning flies containing the human *tau* gene (courtesy of Whatman et al.).

Microtubule associated protein (MAP) TAU has long being implicated in the encoding of human memory and it has been shown that mutations in the human NC-17 *tau* gene are one of the causes of Alzheimer's Disease [60,61,62]. For this reason, NFT and SP/AP formation have been the main focus of studies of tauopathies in animal models. For instance, transgenic mice with Fronto-Temporal Dementias with Parkinsonism (FTDP 17) mutations develop NFTs and neurodegeneration accompanied by motor deficits [63,64]. Expression of human wild type and FTDP-17-linked mutations in *Drosophila* results in age-dependent neurodegeneration without NFTs [65] except when wild-type TAU was phosphorylated by overexpressed *Drosophila* glycogen synthase kinase-3 [66]. Mice carrying mutated *tau*, *presenilin 1* and *alpha-beta Peptide Precursor (APP)* transgenes show synaptic dysfunction before the development of NFTs or amyloid plaques. From these and other studies it seems that tauopathy-caused deficits in memory appear even without NFTs or SPs/APs although frequently, at least NFTs do eventually appear in the late stages of the disease.

For NFTs to form there must be a situation of elevated TAU accumulation (in a non-filamentous or 'pre-tangle' state) in the affected neurons. Such a condition has been suggested as the underlying cause of pre-neurodegeneration cognitive symptoms such as

memory loss [63,67] and our research experimentally addresses the question of the effect of elevated pre-tangle state TAU in *Drosophila* mushroom bodies and we propose a connection of the observed effects with theoretical models of cytoskeletal function.

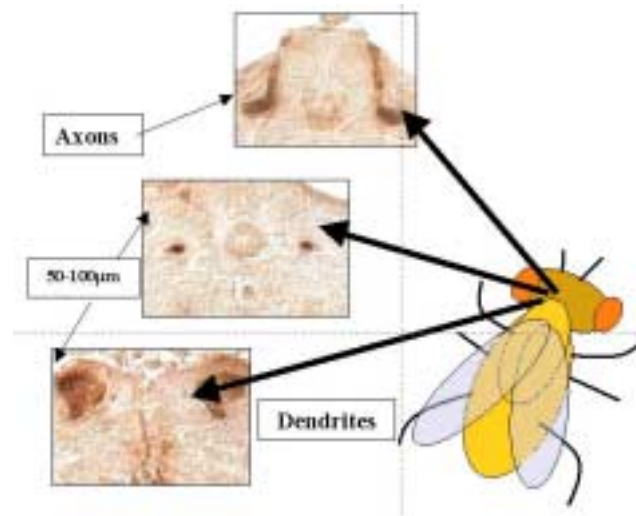
The work presented in this Chapter was carried out by the author and colleagues in the Department of Biology of Texas A&M University under the kind supervision of Prof. E.M.C. Skoulakis. During this two-year collaborative project, some results necessary for supporting the conclusions of this dissertation were obtained by student workers or Prof. Skoulakis himself. The most relevant of these are presented and are clearly acknowledged as work done by others.

### 3.2 *Drosophila*

The *Drosophila Melanogaster* fruit fly has long been a favorite of experimental behavioral neurobiologists for numerous reasons including its relatively simple genetic makeup and quick generation time, powerful classical and molecular genetics and the animal's ability to learn and remember a variety of tasks. All of our *Drosophila* lines were cultured in standard cornmeal sugar food supplemented with soy flour and  $\text{CaCl}_2$  at 20-22°C.

For historical purposes and to illustrate our approach and choice of *Drosophila* more fully, our initial experimental design will be briefly described here. *Drosophila* was suggested as the ideal system for investigating cytoskeletal involvement in learning and memory because we were to attempt to track an intraneuronal *redistribution* of

MAP-2 and/or MAP TAU as a result of conditioning. This is a prediction of the GSM described in Chapter II. In order to track a redistribution of MAPs *inside* neurons one must be able to differentiate between the various parts of the neuron such as the dendrites, axons, axonal projections and somata. In humans and other mammals, the neuronal organization is such that multiple neurons and neuronal types are involved in a given process forming an extensive complex network of axons and dendrites. As a result, it is particularly difficult to locate individual neurons' specific parts and stain selectively to track changes in distribution of a particular protein. In *Drosophila* on the other hand, the neuronal organization is such that differentiation of subneural parts is facilitated. For instance, neurons belonging to mushroom bodies (MBs are prominent structures in the *Drosophila* brain essential for olfactory learning and memory) represent a highly ordered, tightly and sequentially packed, neuronal system where axonal projections (i.e. synaptic fields), dendrites and somata are macroscopically (order  $\mu\text{m}$ ) separated in ordered fiber bundles, see Fig. 4.



**Fig. 4. Fly Mushroom bodies (MBs).** Fly mushroom bodies are shown in paraffin frontal sections  $\sim 5\mu\text{m}$  thick, stained for LEO, a MB specific protein.

This provides a strong advantage for analysis of the results of expression of microtubule associated proteins in specific neurons (e.g. those associated with a specific type of memory) but also *within* different parts of such neurons. For instance, a bulk redistribution of a certain MAP from the axons to the dendrites of the MB, presumably as a result of memory formation can, in principle, be tracked. This is in fact a prediction of the GSM for memory encoding since if the MAPs play the role of fingers on the guitar fretboard and the various chords correspond to encoded information, acquisition of new information and memory would result in a redistribution of MAPs. Unfortunately, our preliminary experiments utilizing directed expression of chicken MAP-2 in mushroom bodies showed that either the resolution offered by existent anti-MAP antibodies was insufficient to decipher appreciable MAP redistribution and/or no such redistribution took place as a result of learning. The latter would be inconsistent

with results obtained later by [68] in rodents that suggest a redistribution of MAP-2 resulting in accumulation in dendrites as a result of learning an auditory associative task.

We therefore shifted our approach to determining the impact of MAP TAU *overexpression* on the ability of the animals to learn and retain memories. Although this is not as direct a test of the GSM it does provide a solid link between the microtubular cytoskeleton and memory retrieval and stability as will be argued in this Chapter.

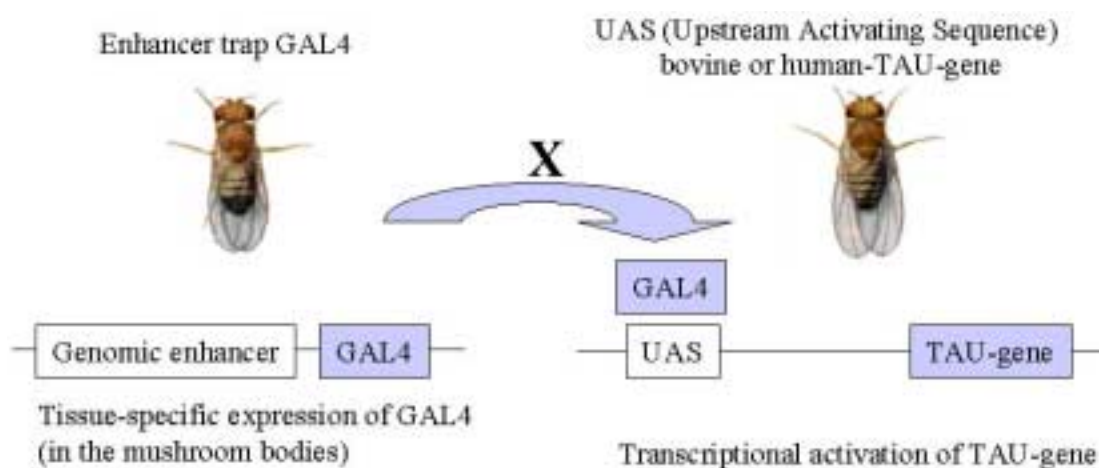
### 3.3 Genetic Engineering

We induced the expression of vertebrate (human and bovine) *tau* genes, producing TAU protein in *specific* tissues and at *specific times* in *Drosophila* using the method of directed gene expression.

#### 3.3.1 Directed Expression

Directed gene expression rests on the principle of obtaining two genetically manipulated (transgenic) lines, the first of which contains the gene to be expressed, fused to and under the direction of an *upstream activating sequence* (UAS). This UAS promoter is activated by the presence of its unique, selective and specific activator protein GAL4.

To generate transgenic lines expressing GAL4 in a cell or tissue specific pattern, the GAL4 gene is inserted randomly into the fly's genome, thus driven in its expression from various genomic enhancers. A GAL4 target gene (UAS-tau) will remain silent in the absence of GAL4. To activate the target gene, the flies carrying the UAS-tau are crossed to flies expressing GAL4 at specific tissues and at specific times in the animal's development (see Fig.5). To eliminate potential complications arising from expression of TAU in the embryonic and developing nervous system, we selected strains expressing GAL4 in late pupal and adult mushroom body neurons [69] only by utilizing the MB drivers c492 and c772.



**Fig. 5. Upstream Activating Sequence and Target Gene.**

### 3.3.2 Cryosections and LacZ

To be certain that the target gene is expressed at the appropriate tissues, we must test whether the genomic enhancer and enhancer trap GAL4 are working as advertised. To do this, we crossed flies that had the GAL4 gene with flies that had another gene whose activity could be readily monitored (reporter gene) by histological methods: the bacterial beta-galactosidase gene (LACZ). Flies having the UAS-LACZ gene were crossed to fly strains expressing GAL4 in their mushroom bodies. Flies that are the progeny of GAL4xLACZ will have beta-galactosidase activity in their mushroom bodies visualized as *blue pigment*. This provides us with a simple test of where the actual target gene is going to be expressed once activated in a GAL4xtau cross. Following the above procedure, the expression patterns were verified by crossing GAL4 strains to UAS-*lacZ* reporter-construct bearing animals [70] and monitoring reporter gene activity in head "cryosections" [71,72]. This sectioning procedure is different from the one described for all the immunohistochemical experiments described later as there was no need to stain.

Fly heads are cryosectioned (they are frozen to  $-20^{\circ}\text{C}$  in an embedding gel instead of being chemically fixed, and are then sectioned immediately) and staining is provided in the form of the naturally occurring blue pigment due to the expression of the lacZ gene. The results of this preliminary experiment showed that the mushroom bodies as well as certain other sections of the fly brain do indeed express LACZ indicated by the blue color in the sections. This is illustrated in (Fig. 6). Note that this is a low resolution method and we expected lacZ to be 'leaky' in its reporting of GAL4 presence. It was however sufficient to determine that we had the correct strains.

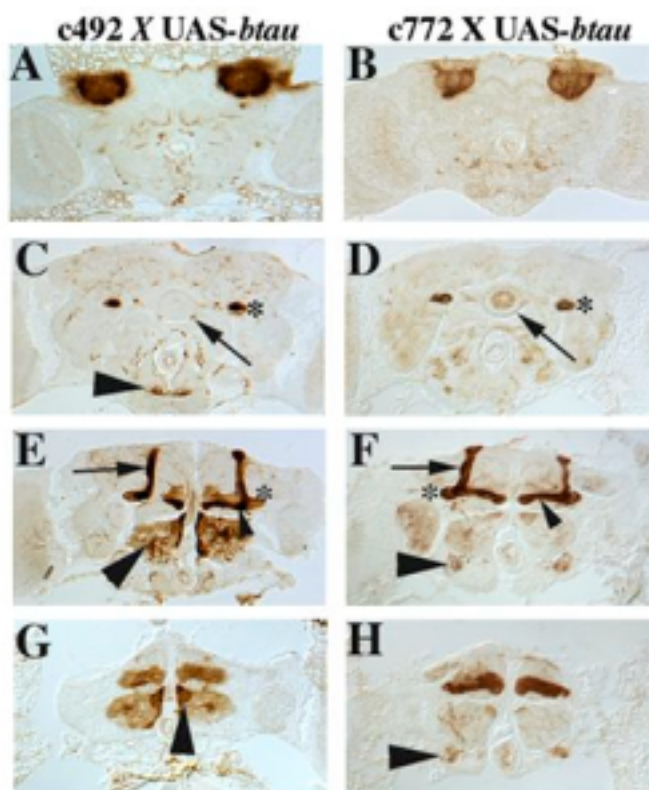


**Fig. 6.. Close-up of Frontal Cryosection.** A close-up of a frontal section of a fly brain expressing LACZ. Dark blue indicates directed expression of the lacZ gene. The stained structure is histologically identified as the left mushroom body ( $\gamma$  lobe) (dorsal is up).



### 3.3.3 Paraffin Sections and Immunohistochemistry

Of the three *tau* transgenes that we were interested in testing, only the bovine one was used to check the actual expression pattern of each of the two drivers. This was done because the anti-bTAU monoclonal antibody was commercially available and performed well on paraffin sections while at the time, antibodies for hTAU and dTAU were not available. Although we had no direct visualization of the expression patterns of htau and dtau transgenes, we are confident that since they were driven in their expression by the same MB drivers they were expressed in very similar, possibly identical patterns. The expression pattern of the c492 and c772 drivers is shown in Fig. 7. Both c492 and c772 GAL4 drivers directed bTAU distribution in the dendrites (Fig. 7 A, B), the fasciculated axons (Fig. 7C, D) and  $\alpha$  lobes (Fig. 7 E, F) of mushroom body neurons.



**Fig. 7. Expression of bTAU in Mushroom Body Neurons.**

Immunohistochemical detection of bovine TAU (bTAU) accumulation within adult *Drosophila* brain in 5 $\mu$ m frontal paraffin sections challenged with a monoclonal anti-TAU antibody. Dorsal is up in all photographs. Accumulation of bTAU is shown in c492; UAS-*btau* (A, C, E, G), and c772; UAS-*btau* (B, D, F, H) heterozygotes. (A and B). Accumulation of bTAU within the dendrites (calyxes) of mushroom body neurons in the posterior of the head. (C and D). bTAU accumulates within mushroom body pedunculi (asterisks) the ellipsoid body (arrow) of c772; UAS-*btau*, but not of c492; UAS-*btau* heterozygotes. In the latter, bTAU was found within distinct neurons of the sub-esophageal ganglion (arrowhead). (E and F). In the axonal projections of mushroom body neurons, bTAU was abundant in the  $\alpha$  (arrow) and  $\beta$  (arrowhead) lobes, but in lesser amounts in the  $\beta'$  lobe and “heel”(asterisks) in c492; UAS-*btau* animals. In addition, bTAU was found in intrinsic neurons of the antennal lobe (large arrowhead). However, in c772; UAS-*btau* the protein was found throughout the  $\alpha, \alpha'$  (arrow),  $\beta$  (arrowhead) lobes and “heel”(star) of the mushroom bodies and the antennal nerve (large arrowhead). (G and H). In contrast to the modest accumulation of bTAU in the  $\gamma$  lobes of c492; UAS-*btau*, the protein was abundant in the  $\gamma$  lobes of c772; UAS-*btau*. Large arrowheads indicate expression within antennal lobe neurons for c492; UAS-*btau* and the antennal nerve for c772; UAS-*btau*.

The c772 driver directed bTAU distribution throughout the mushroom body lobes and “heel” (Fig. 7 F, H), whereas under c492 lesser accumulation of the protein was observed in the  $\alpha'$ ,  $\beta'$   $\gamma$  lobes and “heel” (Fig. 7 E, G). An additional difference between these drivers was bTAU accumulation in the ellipsoid body ring neurons under c772 (Fig. 7 D) and accumulation of the protein in antennal lobe intrinsic neurons and sub-esophageal ganglion neurons under c492 (Fig. 7 C, G). The areas of overlapping TAU accumulation under the two MB drivers were the dendrites (calyces), pedunculi,  $\alpha$  and  $\beta$  lobes and to lesser degree the  $\gamma$  lobe. In addition, bTAU was observed in few other neurons of the adult brain that differ between the c492 and c772 drivers as shown in the figure.

From this histological analysis we can conclude that the c492 driver expresses late in development, is mostly restricted to mushroom body neurons and lightly in the antennal lobe intrinsic neurons and sub-esophageal ganglion neurons making it ideal for our purposes. In general, both c492 and c772 appear relatively restricted and specific both spatially and temporally.

### 3.3.4 Coimmunoprecipitation

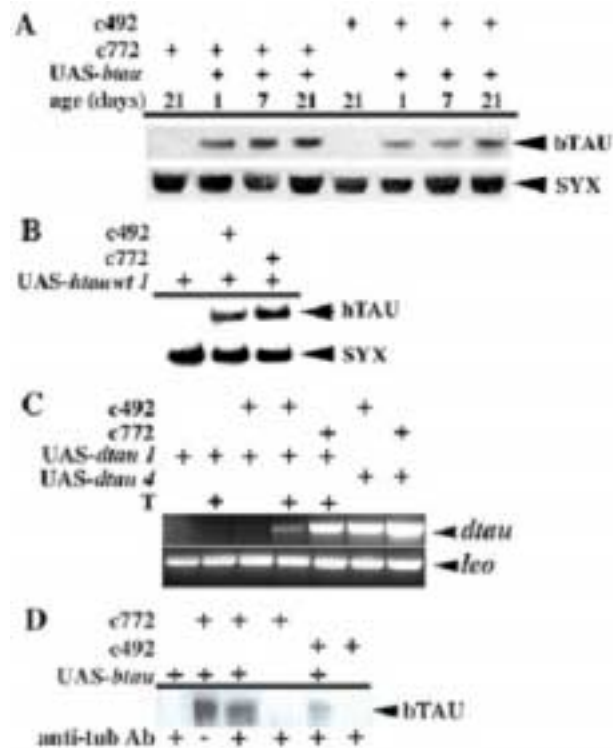
Note that past studies have shown that mere accumulation of non-*Drosophila* proteins such as  $\beta$ -galactosidase [71,72], and GAL4 (Fig. 5 and 6), or *Drosophila* proteins [73,74] that are not MT specific in MB neurons, do not cause any behavioral deficits. Therefore, once TAU is shown to bind to MB MTs, any effects of TAU accumulation in MBs can be taken as specific to TAU. Also note that mere presence of

two proteins in the same tissue does not necessarily mean they are bound together so although we expected h- and b- TAU to bind to MTs we performed a coimmunoprecipitation study. The *Drosophila* protein (dTAU), contains four putative tubulin binding repeat [75]. They exhibit 42% and 46% identity (62% and 66% similarity)\* with the respective sequence of bTAU and hTAU [75,76,77]. To determine whether this sequence conservation among vertebrate and *Drosophila* TAU signals also a functional conservation (i.e. if all types retain their MT binding sites intact), anti-tubulin antibodies were used in immunoprecipitation experiments from head lysates of *btau*-expressing animals and controls. We found that bTAU co-immunoprecipitates with *Drosophila* tubulin, indicating that the vertebrate protein is capable of binding *Drosophila* microtubules (Fig. 8D).

There is one obvious problem in assuming that we have just substituted 'more of the same' in the fly's mushroom bodies because dTAU lacks the amino-terminal extension of vertebrate TAU and this suggests that the conformation of vertebrate TAU will be somewhat different from the *Drosophila* protein despite its microtubule-binding ability. This however does not affect the conclusions of this study as will be illustrated later.

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\* Identity is defined as absolute conservation of the amino acid sequence between two proteins while similarity is conservation of type (e.g. exchanging one acidic amino acid for another acidic preserves similarity)



**Fig. 8 Coimmunoprecipitation (A)** A semi-quantitative Western blot of 15  $\mu$ g from adult head lysates obtained from animals aged 7-21 days as indicated. The genotypes of the animals used are indicated above for each lane. The blot represents one of a triplicate set that was used to quantify the amount of bovine TAU (bTAU) in the lysates densitometrically using the level of syntaxin (SYX) as a reference. There was no significant change in the level of bTAU over the period tested. **(B)** Expression of human TAU (hTAU) in adult *Drosophila* heads. 15  $\mu$ g head lysate from animals of the indicated genotypes aged 3-7 days were used. As with A, expression under the c492 mushroom-body driver was more pronounced. **(C)** Over-expression of *Drosophila tau* RNA (*dtau*) in adult heads. One of three independent experiments is shown. The genotype of the animals is indicated above each lane. T indicates incubation at 29 °C for 48-52 hours prior to tissue isolation. The *leo* RNA was used as quality control for the RT-PCR and serves as a semi-quantitative indicator of the relative levels of *dtau*. The level of *dtau1* under c772 at 23-24 °C was investigated in a different experimental set and not shown here, but it was found at the same or greater level than that of c492/+; *dtau1*/+ after 48-52 hour incubation at 29 °C. **(D)** bTAU co-immunoprecipitates with *Drosophila* tubulin, indicating that the vertebrate protein is capable of binding *Drosophila* microtubules (Fig. 8D)

Collectively, the ability to bind *Drosophila* tubulin in head lysates and its preferential accumulation within the mushroom bodies indicate that bTAU, and by virtue of its high degree of identity hTAU, which was not directly tested, bind to the microtubular cytoskeleton within these neurons. Therefore, in the mushroom body neurons of the three *tau* transgenics investigated, the microtubular cytoskeleton is likely burdened with excess TAU.

All strains were normalized to an isogenic (i.e. genetically identical)  $w^{1118}$  strain\*. To obtain flies for behavioral analyses, c772 and c492 homozygotes were crossed to UAS-*btau*, UAS-*htauwt1*, UAS-*dtau 4* and UAS-*dtau1* homozygotes (see separate section on *dtau* below) and the progeny was collected and tested 3-5 days after emergence. Similarly, the UAS-*btau*, UAS-*htauwt1*, UAS-*dtau 4* and UAS-*dtau1* homozygotes were crossed to  $w^{1118}$ , the line not containing any drivers (and thus one does not expect to see any extra tau expression) to obtain heterozygotes used as controls.

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\*Isogenic lines are strains of identical genetic background.  $w^{1118}$  was chosen to represent the wild type genotype. The transgene of interest was bound to red-eye phenotype and the transgenic flies were crossed to  $w^{1118}$  for seven generations (keeping only the red eyes) thus normalizing the genetic background and avoiding contamination.

To elevate expression from the UAS-*dtaul* transgene, flies raised at 23-24°C were subsequently placed at 29 °C for 48-52 hours prior to behavioral experiments, or tissue isolation for RT-PCR analysis. This was done because the UAS constructs were generated incorporating a part of a heat shock (hs) promoter (a gene that regulates expression as a function of temperature) which does not respond with the magnitude of a natural hs promoter, but does increase transcription of the transgene 2-3 times.

In addition to the pattern of expression of a gene, it is important to also quantify the amount of protein that is being created. To investigate the relative level of TAU accumulation within adult fly heads we performed semi-quantitative Western analyses (see method section below for details). We determined that bovine TAU was present in head lysates of animals that had the *tau* transgenes and the MB drivers, but not in parental strains (Fig. 8) as was expected. The level of bTAU protein did not appear to change significantly over a three-week period, indicated by densitometric quantification of results from three independent experiments such as that shown in Fig. 8A. Similarly, the level of hTAU appeared relatively constant (Fig. 8B and data not shown). In addition, the results in Fig. 8A and 8B indicate that transgenic protein accumulation was higher under MB driver *c772* rather than *c492*. Results from reverse-transcription polymerase chain reaction (RT-PCR) investigation of *dtau* RNA accumulation from the UAS-*dtau4* transgenic line were consistent with that observation (Fig. 8C). From all of the above we conclude that the bovine, human and *Drosophila* tau -expressing transgenic flies express a significantly higher level of TAU in their mushroom bodies.

Although it would be desirable to know exactly how much more TAU than normal is present, the techniques we used for quantifying the presence of b and h protein relied on mono- or polyclonal antibody binding and densitometry and thus are inherently difficult to normalize.

In principle, it would be possible to refine these findings with such elaborate methods as ion trapping and matrix-assisted laser directed ionization and time- of-flight spectroscopy we are confident that the transgenic animals did express a significantly higher level of TAU in their mushroom bodies and this is sufficient for the scope of the current study.



### 3.4 Conditioning

*Drosophila* fruit flies are naturally attracted or repulsed with a variety of affinities by different odors. We followed two standard negatively reinforced associative learning paradigms that essentially generalize the Pavlovian conditioning protocol by coupling aversive odors as conditioned stimuli (CS+ and CS-), and electric shock as the unconditioned stimulus (US). This way, olfactory cues are coupled with electric shock to condition the flies to avoid the odorant associated with the negative reinforcer. These conditioning protocols for *Drosophila* were initially developed by [78] and modified by E.M.C. Skoulakis et al. [71,79]. We used two aversive odorants: 3-Octanol (OCT) and Benzaldehyde (BNZ). The conditioning apparatus consists of a training chamber and a selection maze (see Fig. 9). The maze is normalized by adjusting the concentration of odorants. Once normalized, both wild type (control) and transgenic naïve (i.e. untrained) flies choose to enter one of two identical tubes smelling of OCT and BNZ respectively, with a probability of 50% as they avoid both odors equally. All "LONG TRAINING" was performed as described below by the author while the SHORT conditioning assay was performed by EMC Skoulakis as described in [80]. Because the earliest possible time that we can test the animals past the CS+ and US presentation is 180-200 seconds, our measurements cannot differentiate between "acquisition" and "3-minute memory". This earliest performance assessment will be referred to as "learning".

Conditioning of the flies in the LONG TRAINING protocol takes place as follows. A batch of wild type, naïve flies (numbering between 50 and 60) are collected under light anesthesia (using CO<sub>2</sub>) and 12-24 hours later are left in the dark for one to

two hours. The entire conditioning procedure takes place in a temperature- and humidity-controlled darkroom under red illumination as flies have been shown to react least to red light. This is done in order to isolate the effects of olfactory stimulation from visual stimulation. Once the flies have been acclimated to the darkroom, half are inserted into conditioning chamber A. The cylindrical wall of the chamber is covered by a grid of two interspersed conducting electrodes spaced such that at least two of the fly's six legs are likely to be in contact with two opposite electrodes. The diameter of the chamber is chosen such as to prevent flies from hovering midair. This way, the fly necessarily completes the circuit thus making it the path of least resistance. The electrodes are electrified by a signal generator set to 92.0V. The flies receive eleven electric shocks once every five seconds for about a minute. During this time, the chamber is filled with air containing OCT. The flies are given 30 seconds to rest while the air is being cleared of odorants and are then given the opposite (control) odorant (in this case BNZ) for another minute in the absence of electrical shocks. A rest period of 30 seconds follows after which the flies are tested for acquisition of memory by being inserted into the selection maze and given the choice of entering a chamber smelling of OCT or an identical one smelling of BNZ. For control and consistency purposes, the experiment is done simultaneously in an identical apparatus B with the shock-associated and control smells reversed. We define a conditioned or “trained” fly as one that has chosen to go into the chamber filled with the control odor after given the choice for 90 seconds.

It is observed that following training, a large percentage of wild type flies choose to avoid the smell that was present when they received the electric shocks. The percentage is calculated as a normalized *performance index* (PI) where

$$PI = \frac{(trained - untrained)}{total} \times 100\%$$

Typical PI values for wild type flies were between 75 and 90% giving us confidence that the flies have learned to associate the stimuli. The general procedure described above is a typical associative learning Pavlovian conditioning paradigm for behavioral experiments appropriate for a variety of animals and more details can be found in the literature [71, 79]. One improvement that was discovered (and increased wild type PI to about 90%) was that it was possible to collect the flies without subjecting them to CO<sub>2</sub> anesthesia after conditioning by simply tapping the chambers sharply so that the flies entered a test tube through a funnel by their own inertia. The mechanical ‘shock’ associated with such tapping was shown to have no effect on the flies’ PI while the (light) anesthesia immediately following conditioning as well as the presence of a naturally leaky CO<sub>2</sub> tank in the darkroom was known to compromise PI scores.

### 3.5 Controls

During physics experimentation, background measurements play a significant role in determining the signal. Similarly, a dominant theme in biological behavioral research of the type described here is that of a set of measurements collectively called "controls". When results such as, for instance, a decrement in learning and memory

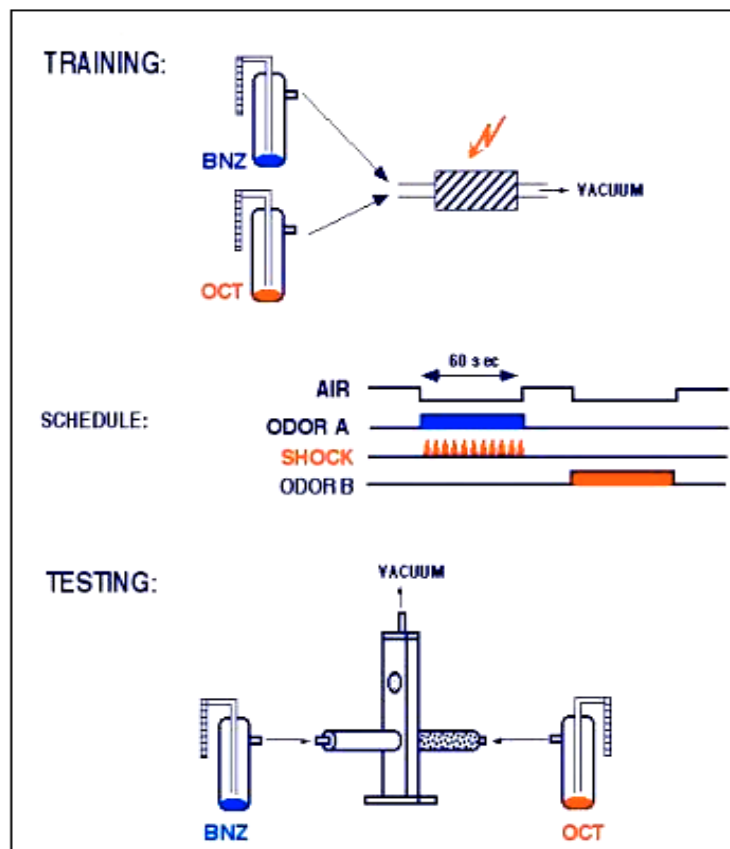
exhibited by transgenic animals are quoted, they are always quantified with respect to the equivalent in the control (non-transgenic or 'wild type' animal).

For our behavioral analyses to have any significance we had to first determine that the flies expressing foreign TAU or overexpressing native TAU were not affected in ways unrelated to learning and memory. Thus we had to assess the experimental flies' task-relevant sensory behaviors and olfactory acuity to an attractive odor in addition to testing their ability to feel and avoid electric shock and to detect and avoid aversive odorants. Experience-dependent non-associative behavior was also tested by examining the effects of *pre-exposure* to odorant plus shock since pre-exposure to electric shock and one odorant tends to decrease the animals' ability to perform well in associative learning tasks that depend on electric shock and another odorant.

We also had to determine that our flies were viable and no neurodegeneration took place as the result of expression of the transgenes. Note that in all these control experiments, the main principle is to always test the transgenic against the control, for instance, an absolute decrement in PI is not indicative of a TAU-mediated effect if it is mirrored identically in control flies also.

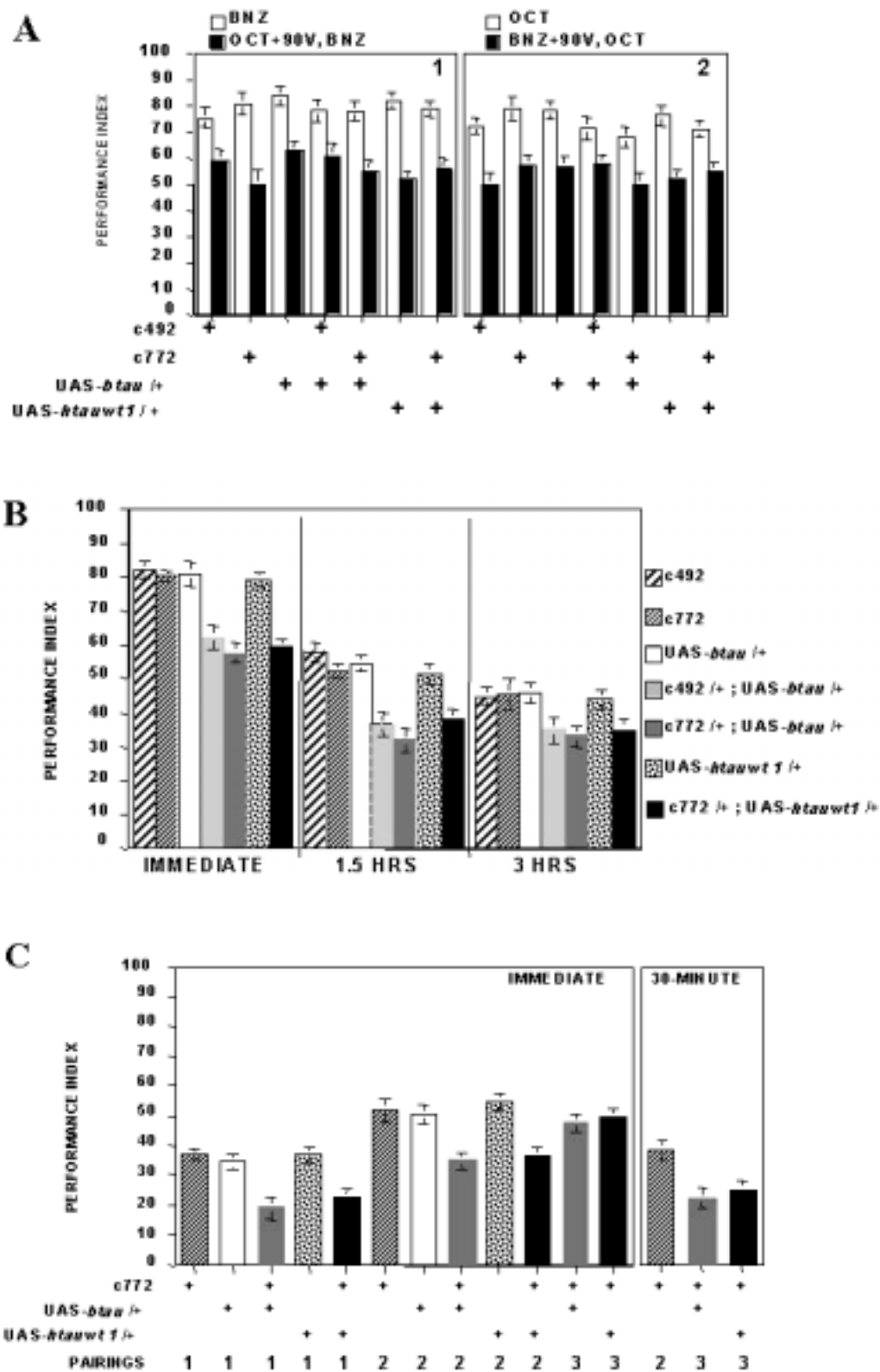
The results of these control experiments are shown in Fig. 10 and Tables 1 and 2. Attraction and navigation (column 8) data were obtained by O.Fitch. In addition to the controls described in detail below, we exposed flies to 29°C for 48-52 hours and did not observe any effect on their responses. This was done to check for possible leakage of any heat-shock genes that may have been present in or had contaminated the lines.

Finally, one must be certain that the observed effects are TAU specific, i.e. that other proteins that do not bind the microtubular cytoskeleton and are (over)expressed with the same drivers, result in no memory effects. This was done and was discussed in section 3.4 of this Chapter.



**Fig. 9. Conditioning apparatus and training schedule.**

**Fig. 10. Results (A)** Non-associative pre-exposure effect. 1. Avoidance of benzaldehyde after pre-exposure to full strength octanol and 90 V electric shock (filled bars) in comparison to avoidance without such pre-exposure (open bars) ( $n \geq 7$ ). ANOVA revealed significant effects of treatment ( $F_{(1, 78)} = 13.784$ ,  $p < 0.005$ , but not for genotype, both in pre-exposed and non pre-exposed animals. 2. Avoidance of octanol after pre-exposure to benzaldehyde and 90 V electric shock (filled bars) in comparison to octanol avoidance without pre-exposure (open bars) ( $n \geq 7$ ). ANOVA revealed significant effects of treatment ( $F_{(1, 84)} = 14.026$ ,  $p < 0.005$ , but not for genotype, both in pre-exposed and non pre-exposed animals. **(B)** Olfactory memory after LONG paradigm conditioning. The mean Performance Index  $\pm$  SEM of  $c492/+$ ,  $c772/+$ ,  $UAS-dtau4/+$  (open bars) and  $c492/+$ ;  $UAS-dtau4/+$  and  $c772/+$ ;  $UAS-dtau4/+$  (filled bars) are shown ( $n \geq 9$ ). Two way ANOVA revealed significant effects of genotype [ $F_{(4, 52)} = 14.687$ ,  $p < 0.005$ ] immediate (3-minute), and ( $F_{(4, 49)} = 9.327$ ,  $p < 0.005$ ) 1.5 hours]. Subsequent Dunnett's tests for each time interval did not reveal significant differences in performance among the  $c492/+$ ,  $c772/+$ ,  $UAS-dtau4/+$  control strains or between the  $c492/+$ ;  $UAS-dtau4/+$  and  $c772/+$ ;  $UAS-dtau4/+$  heterozygotes. However, the differences between  $c492/+$ ;  $UAS-dtau4/+$  and  $c772/+$ ;  $UAS-dtau4/+$  heterozygotes and the control strains were highly significant ( $p < 0.001$ ) for immediate memory and 1.5 hr memories. **(C)** Performance of  $c492/+$ ;  $UAS-dtau1/+$  and  $c772/+$ ;  $UAS-dtau1/+$  heterozygotes with or without induction at 29°C after LONG conditioning. The average performance (PI  $\pm$  SEM) of animals raised at 23-24°C for control strains ( $c492/+$ ,  $c772/+$ ,  $UAS-dtau1/+$ ) is indicated by open bars and  $c492/+$ ;  $UAS-dtau1/+$  and  $c772/+$ ;  $UAS-dtau1/+$  heterozygotes with gray filled bars. The performance of animals raised at 23-24°C and subsequently induced at 29 °C for 48-52 hours prior to behavioral experiments is indicated by the stippled bars for controls and the black-filled bars for  $c492/+$ ;  $UAS-dtau1/+$  and  $c772/+$ ;  $UAS-dtau1/+$  heterozygotes. Two way ANOVA indicated significant effects of genotype [ $F_{(4, 44)} = 8.287$ ,  $p < 0.005$ ] for 23-24°C animals and ( $F_{(4, 48)} = 10.016$ ,  $p < 0.005$ ) for animals induced at 29 °C]. Subsequent Dunnett's tests revealed significant differences between the performance of  $c772/+$ ;  $UAS-dtau1/+$  heterozygotes and all control strains, as well as  $c492/+$ ;  $UAS-dtau1/+$  when uninduced ( $p < 0.001$ ). In contrast, both  $c772/+$ ;  $UAS-dtau1/+$  and  $c492/+$ ;  $UAS-dtau1/+$  heterozygotes were different than controls when the animals were induced at 29°C.



### 3.5.1 Mechanosensory

Sensory control experiments to ascertain that the transgenic flies retained their mechanosensory abilities (to feel and avoid pain caused by electric shock) were performed as described in [71,79]. Avoidance of electrified grids kept at 92V (normal US stimulus), or 45V was not different between *tau*-expressing animals and controls (Table 2), indicating lack of mechanosensory deficits due to TAU accumulation. The two levels of voltage were used as a further refining mechanism to help find any mechanosensory effects that our transgene expression may have had (e.g. it may have made the flies less sensitive but still able to sense 92V).

### 3.5.2 Olfactory Acuity

#### 3.5.2.1 Pre-Exposure

For CS+/US pre-exposure experiments [81], flies were given 60 seconds of benzaldehyde, associated with 11, 90V electric shocks. Subsequently, their avoidance of octanol versus air was quantified. As for all our behavioral analyses, the complementary experiments with the odorants reversed (pre-exposing flies to octanol and 11, 90V electric shocks and evaluating benzaldehyde avoidance) were performed in parallel. During olfactory conditioning, normal perception of the control odor (CS-) following exposure to the CS+ and the electric shock is needed to show US-dependent establishment of a CS+ versus CS- differential response [82]. Since it has been established that *Drosophila* mutants are unable to perceive the CS- properly after CS+/US exposure [81] they exhibit performance decrements not because of impairment



in associative processes, but because of a differential decrease in CS- perception. This can be thought of as analogous to a person becoming less sensitive to any smell once exposed to a strong smell for some time. To establish whether TAU accumulation affected this task-relevant, experience-dependent yet *non-associative* response, we quantified the reduction in CS- perception following CS+/US pre-exposure. Although, as expected CS+/US pre-exposure significantly reduced subsequent avoidance of the complementary odor, *tau*-expressing animals and controls exhibited equal decrements (Fig. 10A). Therefore, TAU accumulation did not cause differential responses to odor-shock pre-exposure and we can conclude that TAU accumulation does not affect experience-dependent, non-associative tasks.

### 3.5.2.2 Attractive and Aversive Odors

Both control and transgenic *tau*-expressing animals avoided equally the aversive odors benzaldehyde and 3-octanol (CS) at two different odor concentrations given the choice of fresh air (Table 2). These results indicate that TAU accumulation in mushroom body and other central brain neurons described above, did not result in deficits in sensory abilities necessary for olfactory conditioning. In addition, we tested the response of *btau* and *htau*-expressing animals relative to controls to the attractive odor geraniol (GER) in olfactory trap assays [79]. Though this odor is not task relevant, it provided an independent measure of olfactory acuity towards a qualitatively different odor.

As shown in Table 1, the performance of *tau*-expressing animals was not significantly different from controls. Collectively, the results of these olfactory control experiments support the conclusion that despite the accumulation of TAU in antennal lobe neurons (that are used as olfactory sensors by the fly) (Fig. 7G, H), *btau* and *htau* expressing animals retained their normal olfactory responses to the odors tested.

Olfactory 'trap' assays with the attractive odorant geraniol were performed as described in Phillip *et al.* [79]. Briefly, 10 male flies were placed in a 100x15mm plastic Petri dish containing moistened Whatman paper and the olfactory trap made by cutting the bottoms of a 0.5ml and a 1.5ml Eppendorf tubes and attaching them via their cut bottoms. 200  $\mu$ l of 1% agarose containing 0.05% geraniol was placed in the lid of the 1.5ml Eppendorf tube which was subsequently tightly closed. Attraction to the odor was assessed at 23-24°C in the dark, see Table 1.

GENOTYPE	BNZ		OCT		SHOCK		GER
	1X	0.1X	1X	0.1X	90 V	45 V	
<b>c492</b>	73.24±2.31	61.59±4.18	78.91±4.54	59.86±5.07	76.31±3.61	56.41±6.44	68.05±4.75
<b>c772</b>	87.98±3.33	66.57±3.79	86.91±2.21	71.23±4.54	77.09±4.02	60.17±5.06	62.61±7.57
<b>UAS-<i>btau</i> /+</b>	80.13±2.39	59.22±2.43	83.96±2.33	59.04±4.55	69.05±5.09	58.51±4.01	78.94±4.48
<b>c492 /+; UAS-<i>btau</i> /+</b>	86.31±4.33	73.83±2.16	87.35±4.87	69.97±4.41	82.91±4.09	58.26±3.28	67.87±4.35
<b>c772 /+; UAS-<i>btau</i> /+</b>	76.03±5.26	67.55±2.73	82.64±2.78	74.09±6.73	70.24±5.29	49.11±8.41	70.19±4.13
<b>UAS-<i>htauwt1</i></b>	82.89±2.86	68.73±3.45	79.78±3.27	62.37±3.87	74.59±4.68	56.78±5.27	66.72±4.62
<b>c492 /+; UAS-<i>htauwt1</i> /+</b>	81.26±3.67	64.58±2.96	82.47±3.98	67.79±4.39	76.46±4.89	54.89±4.78	71.87±4.64
<b>c772 /+; UAS-<i>htauwt1</i> /+</b>	78.76±2.97	67.81±3.66	81.78±4.27	70.91±2.98	78.68±3.95	53.97±5.17	68.72±4.49
<b>UAS-<i>dtau 1</i> /+</b>	81.66±2.78	67.12±3.26	85.48±3.08	66.27±3.74	76.82±2.99	49.93±5.34	64.48±4.32
<b>UAS-<i>dtau 1</i> /+ 29°C</b>	80.03±3.10	63.93±2.93	86.69±3.34	61.94±3.92	73.27±3.46	52.78±4.97	68.72±4.49
<b>UAS-<i>dtau 4</i> /+</b>	82.14±2.37	63.48±3.57	80.96±2.87	64.36±4.28	74.08±4.29	56.82±4.39	67.24±5.27
<b>c492 /+; UAS-<i>dtau 1</i> /+</b>	77.73±3.76	65.28±2.84	80.46±3.24	66.15±3.94	79.12±4.53	51.32±4.88	69.47±4.78
<b>c492 /+; UAS-<i>dtau 1</i> /+ 29°C</b>	84.23±4.24	71.17±4.21	84.25±2.82	60.82±4.08	75.14±4.28	52.36±4.67	66.86±4.38
<b>c772 /+; UAS-<i>dtau 1</i> /+</b>	78.76±2.97	64.59±3.49	82.47±3.54	65.38±4.73	75.27±3.77	56.23±5.43	65.84±5.49
<b>c772 /+; UAS-<i>dtau 1</i> /+ 29°C</b>	81.57±3.17	69.22±3.62	86.18±3.21	68.17±4.46	71.89±4.95	55.62±4.71	67.48±4.72
<b>c492 /+; UAS-<i>dtau 4</i> /+</b>	84.76±2.72	70.88±4.04	83.85±2.73	63.36±3.92	76.36±4.16	52.88±4.64	63.87±4.97
<b>c772 /+; UAS-<i>dtau 4</i> /+</b>	80.69±3.18	66.47±3.29	82.94±2.58	67.11±4.24	74.83±3.78	57.74±4.89	65.47±4.28

**Table 1. Olfactory acuity to aversive and attractive odors.**

### 3.5.3 Viability of Transgenics

To assess the effects of extra TAU in MBs on the learning and memory capabilities of flies convincingly, we had to establish that our flies would be reasonably healthy during their conditioning and testing. We hypothesized that accumulation of TAU within the mushroom bodies would not affect survival because these neurons are dispensable for viability [83]. However, the effect on fly longevity of TAU accumulation in additional neurons where c772 and c492 drivers were determined to be active (Fig 7) was unknown. In addition, it has been recently shown that expression of human wild type and mutant TAU proteins in the entire *Drosophila* nervous system (pan-neural expression), or targeted expression in cholinergic neurons, results in neurodegeneration and premature death of adult flies [84]. In order to determine whether TAU expression in adult mushroom bodies and the other brain neurons described above affects the flies' viability, we evaluated the survival of *btau*, *htauwt1* and *dtau*-expressing flies over a period of 21 days post-eclosion\* (Table 2).

Because both male and female animals are used for our behavioral experiments, we used mixed sex populations to evaluate survival unlike previous studies [84,85]. To determine survival rates, groups of 40 animals of both sexes were collected within 2-4 days of emergence and were sequestered in food vials. The vials were changed weekly, and the percent of survivors was determined from duplicate vials and the results of at least two independent experimental sets were averaged. From Table 1 we can conclude that expression of vertebrate or *Drosophila tau* in adult mushroom body and other brain

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\* Eclosion refers to the adult fly emerging from the pupal case (cocoon)

neurons did not result in decreased survival (Table 1). No overt differences between control strains and transgenics were observed for a limited set of animals that were evaluated for viability for two additional weeks (data not shown). Furthermore, TAU accumulation did not appear to result in gross morphological differences, or decreased fecundity and vigor from control strains. These results indicate that TAU accumulation within the mushroom bodies and other neurons of the adult brain does not precipitate the neurodegeneration-dependent decrease in survival observed with pan-neural expression of human mutant TAU proteins throughout development [84].

### 3.5.4 Neuroanatomy and Histology

Although the mushroom bodies are not essential for viability, we expected that degeneration of these neurons would severely impair behavioral neuroplasticity [83]. To determine whether TAU accumulation in adult mushroom bodies causes their degeneration, we histologically investigated the brain neuroanatomy of animals that expressed the *tau* transgenes. Because in past studies the severity of neurodegeneration was observed to increase with age and accumulation of TAU [83], we focused on 21 day-old animals. The semi-quantitative western blot analysis on Fig. 7A demonstrated that bTAU levels remain relatively constant over the 21 days that they were evaluated. Therefore, it is unlikely that any degeneration in older flies is the result of progressively increasing amounts of TAU in mushroom body neurons. Note here that although as previously mentioned, densitometry and immunohistochemistry are by nature hard to normalize, they do give reasonably accurate relative results. Thus we were able to

determine that no more TAU was present in older flies even though we could not tell exactly how much overall TAU there was. Similarly, though the level of hTAU remained relatively constant, advanced age neurodegeneration was observed in flies expressing wild type and mutant protein [84]. Staining with various mushroom body antigenic markers [86] did not reveal detectable morphological anomalies in 21 day-old transgenic *tau*-expressing flies compared to similarly aged, or 2-3 day-old controls.

### 3.6 Results

The results of this study can be summarized as follows. Vertebrate (bovine and human) as well as native TAU accumulation in mushroom bodies of adult flies results in associative olfactory learning and memory deficits.

#### 3.6.1 Vertebrate TAU-Expressing Flies

We had determined that transgenic animals under the *c772* MB driver express higher levels of TAU so we used *c772/+; htauwt1/+* heterozygotes in the analysis presented below, and similar results were obtained for *c4922/+; htauwt1/+* heterozygotes in a limited set of experiments (data not shown).

To determine whether TAU accumulation in the mushroom bodies affected associative processes, we trained *btau*, *htau*- and *dtau* expressing animals and controls in the LONG version of a negatively reinforced, olfactory associative learning task as described above. *c492/+; UAS-btauI/+*, *c772/+; UAS-btauI/+* and *c772/+; UAS-*

*htauwt1/+* heterozygotes exhibited a highly significant 25-30% impairment in learning compared to controls (Fig. 10B, immediate). Similar results were obtained for *driver X dtau* and they are described in the literature [87]. These results demonstrated that TAU accumulation in the mushroom bodies strongly compromised behavioral neuroplasticity underlying associative olfactory learning and memory.

To more closely examine the learning and memory deficits of *btau*, *htau*- and *dtau* expressing animals, we utilized the SHORT variant of associative olfactory training [80] performed by E.M.C. Skoulakis. Because the LONG paradigm utilizes a 60-second CS+ presentation concurrent with 11, 92V electric shocks, the flies' performance represents learning from multiple rounds of what is referred to as 'massed' CS/US pairing. On the other hand, in the SHORT paradigm, a 10-second CS+ presentation is coupled to a single 1.25 second, 92V shock, allowing assessment after a single CS/US pairing [80,89]. Furthermore, performance in SHORT training improves upon multiple pairings with a 15-minute inter-trial interval [80,89]. This allows for a very fine-tuned experimental manipulation to produce equivalent learning in control and experimental animals, a necessary condition to investigate memory stability and retrieval properties.

The results in Fig. 10C demonstrate that a single CS/US pairing in *btau* and *htau*-expressing animals yielded losses in learning scores of the order of nearly 50% relative to controls. As with controls, the performance of *tau*-expressing animals improved upon multiple CS/US pairings indicating that the basic neuroplasticity mechanisms were at least operating in the right direction, but three CS/US pairings were necessary for *tau*-expressing animals to perform at the level reached by controls after only two pairings

(Fig. 10C). This suggests that TAU accumulation causes either an impairment in the learning resulting by each CS/US pairing, or a compromise of memory stability, retrieval, or a combination of the two.

To distinguish between these three possibilities, we trained *c772; UAS-*btau** and *c772; UAS-*htauwt1** heterozygotes to the same performance level as controls (3 pairings for *tau*-expressing animals and 2 for controls) and measured memory of the association after 30-minutes. The *tau*-expressing animals exhibited a significant decrease in 30-minute memory, despite performing equivalently to controls immediately after training. This indicates that memory retrieval and /or stability were compromised in TAU-expressing animals. This result implicates TAU within mushroom body neurons to mechanisms that are key to memory stability and/or retrieval. Since our coimmunoprecipitation experiments showed that all TAU tested bound to the MTs we can conclude that the behavioral deficits observed are the effect of burdening MTs with excessive TAU. This is in accord with what one would expect if the MTs were the first (or at least near the 'front lines') of intercellular information manipulation elements



### 3.6.2 d-TAU Overexpressing Animals

All work with the *dtau* transgene was performed by E.M.C. Skoulakis. A brief account of the results is given here. The methods are described in Materials and Methods later and are taken nearly verbatim from EMC Skoulakis' protocols. Accumulation of dTAU in the adult mushroom bodies did not result in decreased longevity irrespective of the degree of transgene expression (Table 2), or a reduction in responses to sensory stimuli (Table 1). In addition, the response to CS+/US pre-exposure of animals expressing *dtau* highly (*dtau4* transgenics) was not different from controls [87], suggesting that as with vertebrate TAU expressing animals, task relevant experience-dependent behaviors remain unaffected. Similar results were obtained with the low expressing *dtau1* transgenics (not shown). In contrast, accumulation of dTAU in mushroom bodies resulted in a 25-30% decrease in olfactory learning and 90 minute memory [87], similar to that observed in *btau* and *htauwt1* expressing animals.

GENOTYPE	% SURVIVAL				
	DAY 1	DAY 7	DAY 14	DAY 21	DAY 30
<b>c492/+</b>	100 ± 0	84.7 ± 1.5	77.9 ± 3.1	68.9 ± 4.2	64.4 ± 3.2
<b>c772/+</b>	100 ± 0	88.7 ± 3.9	76.2 ± 2.9	71.7 ± 3.6	66.1 ± 3.6
<b>UAS <i>btau</i> /+</b>	100 ± 0	86.9 ± 3.7	79.5 ± 4.1	68.8 ± 2.9	62.8 ± 4.3
<b>UAS <i>htauwt 1</i> /+</b>	100 ± 0	83.5 ± 3.6	78.6 ± 5.6	69.5 ± 3.6	66.7 ± 3.8
<b>UAS <i>dtau 1</i> /+</b>	100 ± 0	86.5 ± 3.2	81.9 ± 4.3	74.9 ± 6.1	63.7 ± 4.8
<b>UAS <i>dtau 1</i> /+ 29°C</b>	100 ± 0	80.7 ± 2.9	71.3 ± 3.8	66.7 ± 4.6	61.9 ± 5.3
<b>UAS <i>dtau 4</i> /+</b>	100 ± 0	83.4 ± 3.5	78.8 ± 2.7	70.3 ± 3.1	63.4 ± 3.7
<b>c492/+ ; UAS <i>btau</i> /+</b>	100 ± 0	87.8 ± 4.3	78.1 ± 3.1	71.2 ± 4.9	65.4 ± 4.2
<b>c492/+ ; UAS <i>htauwt 1</i> /+</b>	100 ± 0	84.6 ± 3.2	78.6 ± 4.3	72.5 ± 3.8	64.5 ± 3.9
<b>c492/+ ; UAS <i>dtau 1</i> /+</b>	100 ± 0	84.8 ± 3.4	77.6 ± 4.9	72.3 ± 4.3	66.2 ± 3.7
<b>c492/+ ; UAS <i>dtau 1</i> /+ 29°C</b>	100 ± 0	83.7 ± 4.2	73.7 ± 3.7	67.2 ± 3.9	59.5 ± 4.7
<b>c492/+ ; UAS <i>dtau 4</i> /+</b>	100 ± 0	86.2 ± 4.2	78.1 ± 3.1	73.6 ± 3.5	66.3 ± 2.4
<b>c772/+ ; UAS <i>btau</i> /+</b>	100 ± 0	87.1 ± 3.5	77.4 ± 3.3	69.7 ± 3.9	63.2 ± 3.3
<b>c772/+ ; UAS <i>htauwt 1</i> /+</b>	100 ± 0	83.9 ± 4.6	78.8 ± 3.7	72.7 ± 4.7	67.6 ± 5.1
<b>c772/+ ; UAS <i>dtau 1</i> /+</b>	100 ± 0	89.7 ± 3.9	83.6 ± 3.8	73.7 ± 2.8	64.8 ± 3.9
<b>c772/+ ; UAS <i>dtau 1</i> /+ 29°C</b>	100 ± 0	80.3 ± 3.6	72.8 ± 4.2	62.7 ± 4.6	58.6 ± 5.4
<b>c772/+ ; UAS <i>dtau 4</i> /+</b>	100 ± 0	87.6 ± 3.2	80.2 ± 2.9	76.9 ± 2.4	67.1 ± 4.4

**Table 2. Survival Data.** (Obtained by O. Fitch)

### 3.6.3 Integrating Results from h-, b-, dTAU Expressing Animals

Combining the above results we are led to the conclusion that the decrements in learning and memory observed in *btau* and *htau*-expressing animals were not caused by accumulation of a vertebrate protein, but rather by increasing the level of TAU in these

neurons. This conclusion was further supported by investigating learning in *dtau1* transgenics that express the transgene at detectable levels only after a 48-52 hour period at 29°C (Fig 8C). Low levels of *dtau* transcription did not affect the performance of *c492/+; UAS-dtau1/+* animals. However, elevation of *dtau* transcription precipitated learning deficits similar to those observed with vertebrate *tau* and *dtau4* transgenics [87]. Similar deficits were observed with *c772/+; UAS-dtau1/+* animals [87], except the effect of elevating transgene expression was not as pronounced since the *c772* MB driver appeared more active than *c492* at 23-24°C (Fig. 8C). These results strongly indicate that the associative learning and memory deficits in vertebrate *tau* and *dtau* expressing animals are the very likely the direct result of elevated TAU accumulation within mushroom body neurons and not because of the conformational differences between vertebrate and *Drosophila* proteins.

Finally, another -unlikely- scenario that fits the data is that since the native and overexpressed *dtau* genes were in different parts of the genome, some role was played by the directed expression on the conformation of the extra dTAU resulting in a perturbation that made dTAU behave like its b and h analogues. One way to rule this out would be to entirely knock out the native TAU gene replace it with *htau* or *btau* thus testing whether these will take up the role meant for *dtau* thus possibly refining the findings reported here and also determining whether the hypothesis behind the "fetal, 4R" TAU VS the "adult 3R" TAU in AD is correct.

### 3.7 Conclusions

Collectively, the results of the behavioral analyses suggest that the level of TAU within mushroom body neurons is essential for both olfactory learning elicited by each CS/US and memory retrieval or stability. The areas of significant homology between the vertebrate and *Drosophila* TAU are confined to the tubulin binding sites and the vertebrate protein appears to bind microtubules in a way similar to the way the fly protein does. Taken together, the results are consistent with excess TAU binding to the neuronal microtubular cytoskeleton and this causing mushroom body neuron dysfunction exhibited as learning and memory deficits. This also indicates that although excessive TAU may not result in neurodegeneration, it is sufficient to cause significant decrements in associative learning and memory that may underlie the cognitive deficits observed early in human tauopathies such as AD.

### 3.8 Discussion

The pre-tangle state of elevated tau has been the topic of limited study in the past (e.g. loss of TAU in axons and elevation in the somatodendritic compartment of neurons prior to tangle formation shown in humans and animal models [67,90] but the possible effect of this state neuroplasticity had not been explored. Similarly, splicing mutations that increase the level of 4R (fetal) TAU are the hallmark of many human tauopathies[91,92]. It has been argued that accumulation of unbound TAU and subsequent NFT formation in human tauopathies may be the result of conformational

changes [93]. However, the conformational differences between dTAU and its vertebrate homologs did not appear important in affecting learning and memory deficits in our study, at least at the level of resolution we could obtain. In contrast, the overall level of TAU within mushroom body neurons appeared to be of main importance.

An enhancement of the adverse effects of TAU elevation has been described in flies co-expressing the  $\beta$ -amyloid-like (APPL) protein in *Drosophila* [94] and more recently in mice [95]. A mild neurodegeneration within mushroom body neurons was apparent in 45-50 day-old flies (data not shown), but this is not a likely explanation for the learning and memory decrements described above for three reasons. First, the flies used for behavioral assays were not older than 7 days, a time over which neither viability decline, nor degeneration were detectable. Second, sensory and non-associative experience-dependent behaviors necessary for associative learning were normal in *tau*-expressing animals. This is especially important for neurons within the antennal lobe whose functions appear intact in two different experience-independent olfactory tasks (Table 1) and experience-dependent tasks (Fig. 10A). Lack of sensory deficits by TAU accumulation is consistent with genetic and pharmacological evidence indicating that disruption of mushroom body function does not effect the responses to odors or shock [83,96]. These results indicate that TAU elevation may affect associative processes differentially. Third, the mushroom body neurons of *tau*-expressing flies retain basic neuroplasticity properties indicated by improving their performance in the SHORT paradigm upon multiple CS/US pairings (Fig. 10C), a situation unlikely of degenerating and dying neurons.

TAU accumulation in mushroom body neurons caused robust associative learning and memory deficits. It is surprising that within the resolution limits of our techniques, the deficits appeared confined to associative learning and memory and not to other experience dependent olfactory processes. These results suggest that normal cytoskeletal-mediated processes, likely disrupted by excess TAU are necessary for mushroom body mediated neuroplasticity underlying associative functions. Interestingly, anterograde axonal transport was inhibited in *Drosophila* larval motor axons expressing bTAU [94]. Similarly, overexpression of TAU in cultured cell lines impaired kinesin-dependent transport of vesicles and organelles [97,98]. Moreover, microtubular dynamics and interactive capacity have been reported significantly reduced *in vitro*, in ratios of greater than one molecule of TAU to 15 molecules of tubulin [99]. Therefore, excessive TAU appears to bind the microtubular cytoskeleton, which not only impairs intracellular traffic, but interferes with the ability of other cellular proteins to interact with it as well. Similarly, inefficient vesicular traffic because of cytoskeletal function disruption may underlie the learning and memory deficits in animals expressing *tau* in their mushroom bodies. Interestingly memory retrieval, but not formation, was severely impaired by blocking neurotransmission from mushroom body neurons by abrogating dynamin-dependent neurotransmitter re-uptake [73,74]. However in contrast to this endocytotic blockade, TAU accumulation in the mushroom bodies affected both learning, and memory stability or retrieval. This suggests that TAU over-accumulation has broader effects on mushroom body physiology than blocking neurotransmission from these neurons. If TAU accumulation impairs neurotransmitter anterograde

transport limiting their availability, then the memory deficits of *tau*-expressing transgenics may underlie retrieval rather than memory stability deficits.

The alternative roles for neuronal microtubules and their dynamic interaction with the proper ratio of microtubule-binding proteins in learning and memory discussed in Chapter II and [68,100], or as neuronal computational elements have been proposed [28]. These data are consistent with specific predictions of these models, including the GSM model which proposes that perturbations in the ratio of microtubule-binding proteins will precipitate learning and memory dysfunction and also with the general approach behind the dipole-dipole logic suggestion where extra tau would alter the local dielectric constant by virtue of its increased density.

In summary, these results strongly suggest that the stoichiometry of TAU and microtubules within neurons is essential for behavioral neuroplasticity. Increasing the level of TAU within neurons precipitates deficits likely due to inhibition of microtubule-dependent intraneuronal traffic, microtubule stability or interactive capacity. The strong behavioral effects indicate that directed TAU-accumulation within neurons can be used as a tool to disrupt neuronal function in general.

### 3.9 Materials and Methods

#### 3.9.1 Fixation, Sectioning and Staining

Three protocols of different fixation strength were used [71]. Following fixation, flies were dehydrated through a series of ten ethanol baths (0-100%) and Methylbenzoate preparing them for embedding in Paraffin, decapitating and sectioning into 5µm frontal sections of heads. These were processed for immunohistochemistry or histology as described in [71,86]. To determine the expression pattern under the *c492* and *c772* drivers, an anti-bTAU monoclonal antibody (Sigma) was used at 1:1000 dilution after it was established by titration to be the optimal concentration. This antibody does not react with the native *Drosophila* protein demonstrated by the lack of staining in control *UAS-btau*, *c492* and *c772* animals. The anti-LEO, anti-FASII, anti-HRP and standard Hematoxylin-Eosin staining were used for neuroanatomical analyses as described previously [86]. Note that there is an important underlying assumption in this type of immunohistochemistry. We assume that the fixative solution preserves the tissue as it was at the instant of death so that all proteins including MAPs in the flies' neurons are permanently bound at their last location. It is further assumed that fixing and embedding in Paraffin will not affect the binding of MAPs to MTs or the structure and conformation of the MAPs. Affecting the conformation of proteins may mean changing them in such ways that they are either no longer identified by the antibody or antibodies now bind less specifically. Historically, such complications have been ignored mostly because fixation methods have been used for decades with good results despite the lack



of complete theoretical understanding as to the exact action of the fixatives. Use of monoclonal antibodies minimizes any side effects of the fixation process.

### **3.9.2 Western Blot Analysis and Immunoprecipitations.**

Heads from c772, c492, c772; UAS-*btau* and c492; UAS-*btau* animals were separated from bodies by vigorous shaking in liquid nitrogen and sieving. Heat stable protein extracts were prepared essentially as described in [75]. The lysates were quantified with Bradford (Biorad) assays, Laemmli buffer was added, run on standard SDS-PAGE and blotted. The anti-bTAU monoclonal antibody was used at 1:1,000. A polyclonal anti-TAU antibody (Dako) that identifies the human protein was used at 1:10,000. The results were visualized with enhanced chemiluminescence (Pierce). For immunoprecipitations, 10µg of each lysate were diluted 5-fold in immunoprecipitation buffer (25 mM Hepes/7.4, 100 mM NaCl, 5 mM MgCl<sub>2</sub>, 0.1mM EDTA, 0.1% Tween-20, 200 µg/ml BSA-Bovine Serum Albumin), and incubated at 4°C for 3 hrs with a monoclonal antibody against acetylated tubulin (Sigma). The immune complexes were blotted and probed with the monoclonal anti-TAU antibody and results were visualized with enhanced chemiluminescence.

### **3.9.3 Reverse-Transcriptase Polymerase Chain Reaction (RT-PCR)**

Forty heads were homogenized in 200µl of Trizol and RNA was prepared as suggested by the manufacturer (Gibco BRL). For Reverse Transcription (RT), 1µg of DNase I-treated total RNA was used per 50µl reaction along with twice the suggested

amount of ImProm-II<sup>TM</sup> Reverse Transcriptase (Promega) and the reaction proceeded at 42<sup>0</sup>C for 60 min. RT from transgene-derived transcripts was achieved with a reverse primer (200ng per reaction) specific for the unique SV40 derived sequence in pP[UAST] [70] present at the 3' of *dtau* transgenes (SV40A primer). 10% of each RT were subjected to 35 cycles PCR (94<sup>0</sup>C-1 minute, 58<sup>0</sup>C-45 seconds, 72<sup>0</sup>C-2 minutes), using the SV40A and dtauF1 (5'-GATCGAGACCCTGAAGATG-3') primers for *dtau* RT products. As a qualitative control of the RT, 200ng of leo6.2 reverse primer was used followed by PCR with *leo*-specific primers [79]. Specificity of the reactions was tested with DNase I-treated, not reverse transcribed RNA.

### 3.9.4 Statistical Analysis

Data were analyzed parametrically with JMP3.1 statistical software package (SAS Institute Inc., Cary, NC) as described in [71,72]. Following initial ANOVA, planned multiple comparisons, comparisons to a control strain (Dunnett's test) or Tukey–Kramer tests were performed as indicated in figure legends.

### 3.9.5 dTAU

To generate transgenic animals the entire *dtau* cDNA was cloned (EcoRI/XhoI) into the pP[UAST] vector and of the transgenic lines obtained, UAS-*dtau 4* was selected for further work because of the intense eye color of homozygotes suggesting strong expression of the transgene. Similarly, the UAS-*dtau1* line was selected because it exhibited the weakest eye color, suggesting low transgene expression. All other

transformant lines exhibited intermediate eye colors. We utilized two different *dtau* transgenic lines that yield quantitatively very different levels of transgenic products (Fig. 8C). Interestingly, the level of transgenic *dtau* RNA in line UAS-*dtau1* was undetectable when driven by c492 (Fig. 8C) and very low under c772 in heads of flies raised at 23-24°C. However, the amount of RNA increased significantly if the flies were incubated at 29°C for 48-52 hours prior to RNA isolation (Fig. 8C). This is most probably the result of low expression due to the chromosomal location of the transgene (position effects) in line *dtau1*. The apparent increase in *dtau* RNA upon temperature increase is a property of the (heat shock) UAS promoter and has been described previously [101]. Briefly, in wild type animals dTAU is distributed throughout the adult nervous system including the mushroom bodies (based on unpublished observations by E.M.C. Skoulakis and [75]).

## CHAPTER IV

### MOLECULAR DYNAMICS COMPUTER SIMULATION OF TUBULIN

#### 4.1 Background

A naïve estimate of the tubulin dipole moment  $\mathbf{p}$  in vacuum based on a charge of 10 electrons multiplied by a separation of 4nm (roughly the distance between the monomers) yields an  $|\mathbf{p}|$  of 1920D. Similarly, a rough volume estimate is  $V = 2V_{\text{glob}}$  where  $V_{\text{glob}}$  refers to the approximately spherical volume of each globular monomer of radius  $R \approx 26 \text{ \AA}$  so that  $V_{\text{glob}} = \frac{4}{3}\pi R^3$  and  $V \approx 73,600 \text{ \AA}^3$ .

The TINKER V3.9 (2001) molecular modeling[102,103] was applied and the CHARMM set of force-field parameters [104] to the 1TUB pdb data consisting of some 17,000 atomic coordinates and calculated  $|\mathbf{p}|$  to be 1740D for the tubulin dimer in close agreement with previous molecular simulation calculations[104].

## 4.2 Results

### 4.2.1 $\alpha\beta$ -Tubulin Dimer Properties

Total Electric Charge	:	-10
Electric Dipole Moment Magnitude	:	1739.093 Debyes
Electric Dipole Moment Direction	:	$\theta = 83.02^\circ$ $\phi(\text{azimuthal}) = 82.97^\circ$ (polar angles with MT aligned along y-axis)
Quadrupole Moment Tensor	:	-10289.087 44690.480 -40222.211
(Buckinghams)		44690.480 14364.789 26028.749 -40222.211 26028.749 -4075.702
Principal Axes Quadrupole	:	-76066.449 27198.352 48868.097
Radius of Gyration	:	28.595 Angstroms

#### Moments of Inertia and Principal Axes :

Moments	X-, Y- and Z-Components of Axes		
28217253.092	0.989955	-0.136413	0.037158
62877950.642	-0.009648	0.197021	0.980352
67347469.686	-0.141054	-0.970863	0.193725
Total Potential Energy	:	0.2536x10 <sup>13</sup> Kcal/mole	
Intermolecular Energy	:	4245449.5859 Kcal/mole	

<u>Energy Component Breakdown</u>	:	<u>Kcal/mole</u>	<u>Interactions</u>
Bond Stretching	:	7099.8889	13541
Angle Bending	:	8227.8642	24391
Urey-Bradley	:	934.5489	11183
Improper Dihedral	:	2068.4637	2483
Torsional Angle	:	5114.3545	35757
Van der Waals	:	0.2536E+13	89574646
Charge-Charge	:	-11976.0900	88029544

Van-Der-Walls –based calculation excluding H-atoms:

Total Area	:	73794.039 Square Angstroms
Total Volume	:	79389.400 Cubic Angstroms

Van-Der-Walls –based calculation including H-atoms:

Total Area	:	76157.482 Square Angstroms
Total Volume	:	82689.706 Cubic Angstroms

Accesible Area/Volume with a probe of 1.4Ang radius excluding H-atoms

Total Area	:	32892.110 Square Angstroms
Total Volume	:	150652.249 Cubic Angstroms

Accesible Area/Volume with a probe of 1.4Ang radius including H-atoms

Total Area	:	32327.968 Square Angstroms
Total Volume	:	152872.288 Cubic Angstroms

#### 4.2.2 $\alpha$ -Tubulin Monomer

Total Electric Charge	:	-5.0	
Electric Dipole Moment Magnitude	:	1193.709	Debyes
Electric Dipole Moment Direction	:	$\theta = 79.70.02^\circ$	$\phi(\text{azimuthal}) = 75.21^\circ$
Dipole X,Y,Z-Components	:	299.822, -1135.481, 213.844	
Quadrupole Moment Tensor	:	-15127.850, 9958.787, 1733.097	
(Buckingham's)		9958.787, 8499.271, 1200.796	
		1733.097, 1200.796, 6628.579	
Principal Axes Quadrupole	:	-18823.734 , 6188.978, 12634.756	
Radius of Gyration	:	20.601	Angstroms
Moments of Inertia and Principal Axes			
Moments	X-,	Y-	Z-Components of Axes
11431733.935	0.721451	-0.619738	0.308922
12582172.462	-0.106186	0.341830	0.933743

#### 4.2.3 $\beta$ -tubulin monomer

Total Electric Charge	:	-5.0	
Electric Dipole Moment Magnitude	:	1193.709	Debyes
Electric Dipole Moment Direction	:	$\theta^\circ = 79.7^\circ$	$\phi(\text{azimuthal}) = 75.21^\circ$
(I've aligned MT along y-axis)			
Dipole X,Y,Z-Components	:	299.822, -1135.481, 213.844	
Quadrupole Moment Tensor	:	-15127.850, 9958.787, 1733.097,	

(Buckingham's) 9958.787, 8499.271, 1200.796,  
1733.097, 1200.796, 6628.579,

Principal Axes Quadrupole : -18823.734, 6188.978, 12634.756,

Radius of Gyration : 20.6 Angstroms

#### Moments of Inertia and Principal Axes:

Moments	X-,	Y-	Z-Components of Axes
11431733.935	0.721451	-0.619738	0.308922
12582172.462	-0.106186	0.341830	0.933743
16740682.841	-0.684275	-0.706454	0.180806



### 4.3 Conclusions and Discussion

TINKER with CHARMM parameters has given close matches to experimental values for dipole moments of other proteins, [6] so we expect the above quoted  $|\mathbf{p}_{\alpha\beta}|=1740\text{D}$  to be reasonably close to the real value of the dipole for the crystallized tubulin unit cell in a flat sheet of antiparallel zinc-induced protofilaments, without C-termini, (as these were the experimental conditions for the pdb data). It was also found that the dipole moment of the individual  $\alpha$ - and  $\beta$ - monomers to be  $|\mathbf{p}_{\alpha}|=552\text{D}$  and  $|\mathbf{p}_{\beta}|=1193\text{D}$  respectively. Note that the  $\beta$ -monomer has approximately twice the dipole moment vector magnitude of the  $\alpha$ -monomer and both point in virtually the same direction, consistent with the fact that they have nearly identical sequence and tertiary structure. The minimum volume we calculated using pdb data was  $V\approx 78,000 \text{ \AA}^3$ . As expected, the Van der Waals attractive forces constitute the maximum contribution to the energy of the tubulin molecule.

## CHAPTER V

### REFRACTOMETRY, SURFACE PLASMON RESONANCE AND DIELECTRIC SPECTROSCOPY OF TUBULIN

#### 5.1 Theory of Dielectrics

##### 5.1.1 Dielectric Properties of Polar Molecules

The dipole moment  $\mathbf{p}$  is defined as a vector associated with a separation of two identical point charges. Its magnitude is defined as the (positive) charge times the displacement vector between the positive and the negative charge and its direction is from the negative to the positive

$$\mathbf{p} = q \cdot \mathbf{d} \quad (27)$$

where  $q$  is the charge (in Coulombs) and  $\mathbf{d}$  the displacement vector pointing from - to +. Units of 'Debyes' are customarily used where  $1\text{D} = 3.338 \times 10^{-30}$  Coulomb · meters. For  $N$  dipoles, in volume  $V$ , we define the total electric polarization vector  $\mathbf{P}$  as the total electric dipole moment per unit volume

$$\mathbf{P} = N\mathbf{p}/V \quad (28)$$

The (time invariant) displacement electric field  $\mathbf{D}$  in isotropic media is defined as

$$\mathbf{D} = \epsilon \mathbf{E} = \epsilon_0 \mathbf{E} + \mathbf{P} \quad (29)$$

where  $\epsilon_0$  and  $\epsilon$  are the permittivities of free space and sample respectively and  $\mathbf{E}$  is the external electric field and thus

$$\mathbf{P} = (\kappa - 1) \epsilon_0 \mathbf{E} \quad (30)$$

Where we have defined  $\kappa = \varepsilon / \varepsilon_o$  the optical frequency *dielectric constant* of the material which is related to the refractive index  $n$  via

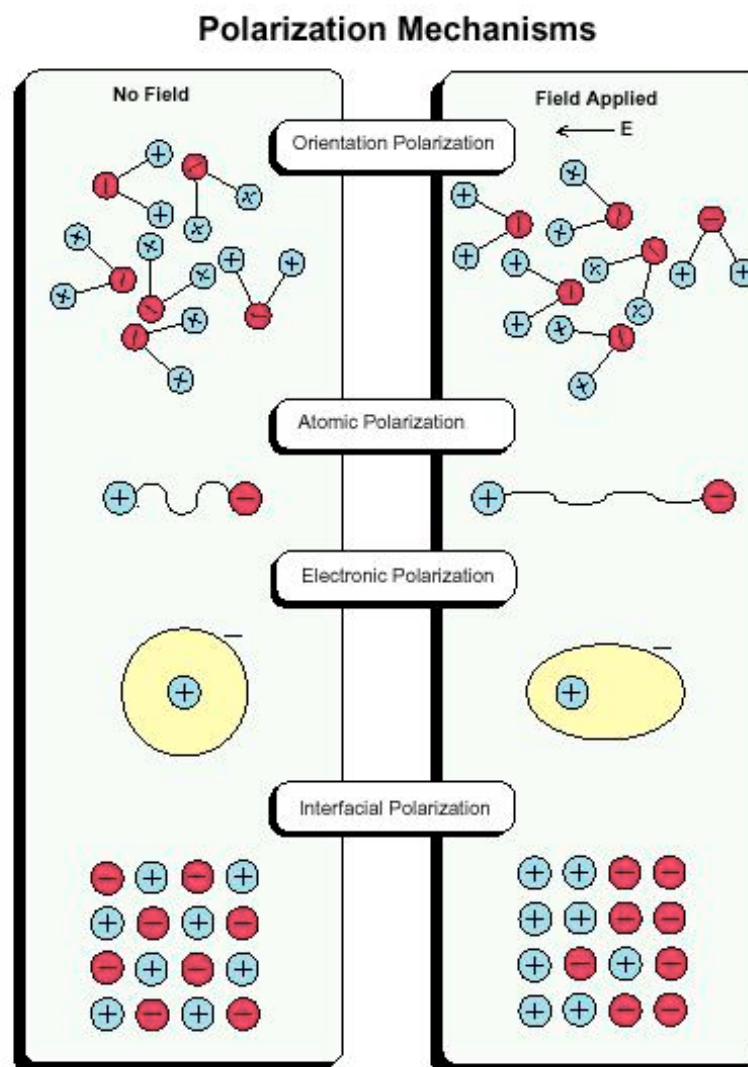
$$\kappa = n^2 \quad (31)$$

The dielectric permittivity  $\varepsilon$  of a substance is a measure of its ability to "neutralize" part of a static electric field by responding to it with a displacement of some of its localized charge. This charge displacement is referred to as polarization and is not dependent on a material having excess charge. Even for a static electric field but most importantly when the incident field is time-varying the dielectric permittivity will also depend on time. Because the capacitance (ability to store charge for a given potential difference)  $C$  of a medium is directly proportional to its  $\varepsilon$  (as in the elementary case of the parallel plate capacitor where  $C = \varepsilon A / d$  with  $A$  the area and  $d$  the separation of the plates in the limit  $d^2 \ll A$ ),  $\varepsilon$  can be measured by inserting the medium between the plates of a capacitor and noting the ratio of the capacitance with ( $C$ ) and without ( $C_o$ ) the medium so that  $\varepsilon = C / C_o$ . This general basic principle holds even for a fluctuating field but with certain modifications as will be illustrated later.

Molecular electric polarizability  $\alpha$  is a scalar of proportionality that quantifies the polarization of a sample as a result of application of an electric field which in general can have four components: electronic  $\alpha_e$  (sensitive even to high frequency fields), ionic or atomic  $\alpha_i$  (medium frequency), orientational or dipolar  $\alpha_d$  (low frequency) and interfacial  $\alpha_{dc}$  (very low to DC frequencies). For simplicity, we will assume that  $\alpha$  is an isotropic characteristic of a protein solution sample, which is justifiable at low concentrations. The total polarizability as a function of frequency  $\alpha(\omega) = \alpha_e(\omega) + \alpha_i(\omega) + \alpha_d(\omega) + \alpha_{dc}(\omega)$  is arguably a good parameter to use when describing a system such as a protein in solution since, unlike the total dipole moment it does not change as a result of solvation, changes in pH, or local electric field ( $E_{loc}$ ) amplitude or direction. We define the total dipole moment as the sum of the permanent dipole moment added to polarizability-dependent dipole moment.

$$\mathbf{p} = \mathbf{p}_{perm} + \alpha \mathbf{E}_{loc} \quad (32)$$

The various polarization mechanisms are illustrated in Fig. 11 and Fig. 12 below.



**Fig. 11. Polarization Mechanisms.** Polarization mechanisms depend on frequency and medium composition. Homogeneous samples cannot exhibit interfacial polarization.

It can be shown [105] that a molecule in a spherical cavity surrounded by a medium of volume polarization  $\mathbf{P}$  will experience a local electric field

$$\mathbf{E}_{loc} = \mathbf{E} + \mathbf{P}/3\epsilon_0 \quad (33)$$

The above is known as the Lorentz field approximation and is applicable in the case of simple dipolar rotor molecules. Combining equations (2), (4) and (6) one finds that the average electric dipole moment to be

$$\bar{p}_{av} = \frac{\alpha}{3\epsilon_o} \left( \frac{\kappa+2}{\kappa-1} \right) \bar{P} \quad (34)$$

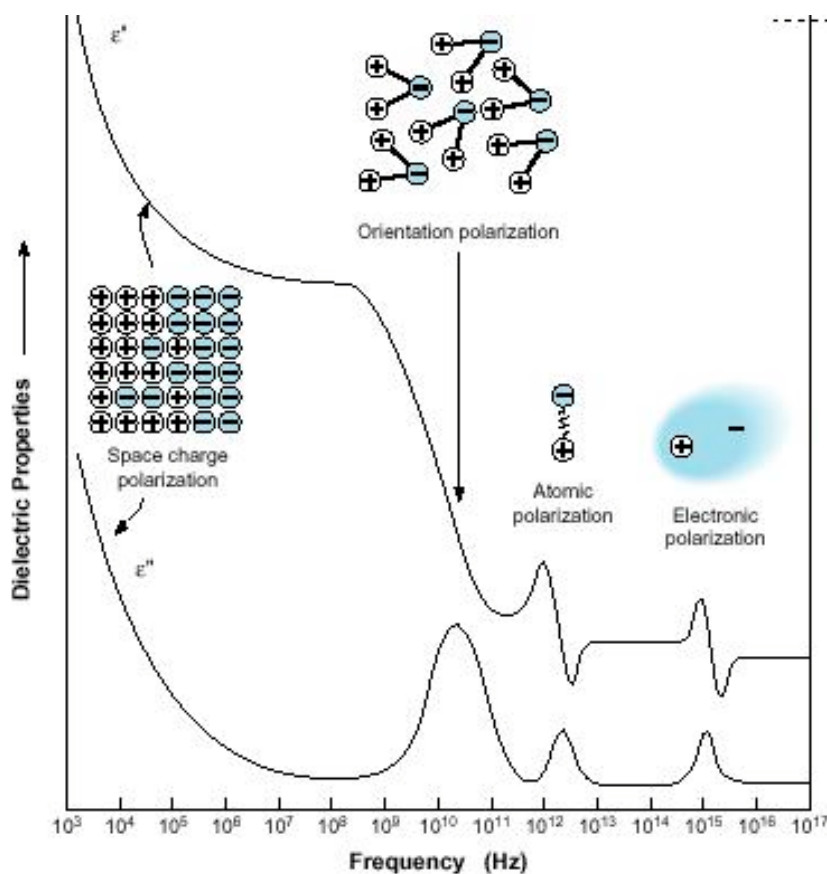
where  $\kappa=\epsilon$ =relative dielectric constant, and one arrives at the Clausius-Mossotti relation for electric polarizability

$$\alpha = \left( \frac{\kappa-1}{\kappa+2} \right) \left( \frac{3\epsilon_o V}{N} \right) \quad (35a)$$

and by extension,

$$\begin{aligned} \bar{P} &= \frac{\bar{p}N}{V} \\ \bar{P} &= (\kappa-1)\epsilon_o \bar{E} \\ \Rightarrow \bar{p} &= \frac{V}{N} (\kappa-1)\epsilon_o \bar{E} \end{aligned} \quad (35b)$$

Note that equations 9 and 9b can give  $\alpha$  and  $\mathbf{p}$  in terms of macroscopic, measurable parameters such as the dielectric constant  $\kappa$  and volume and number of molecules in the sample while equation (8) is not easily applicable to an experimental determination of  $\mathbf{p}$  as it contains the difficult-to-measure  $\mathbf{P}$ . However, (9) is not applicable to cases where the local field cannot be approximated by the simple field assumed by equation (7). These cases include water where if the measured permanent dipole moment ( $6.1 \times 10^{-30}$  C . m) is inserted into the Claussius-Mossoti equation one arrives at a negative value for  $\kappa$ .



**Fig. 12. Frequency Dependence of Polarization Mechanisms.**

### 5.1.2 Dielectric in a Non-Polar Solvent

Noting that anti-parallel orientations between the local field and the dipole moment of a molecule in a sample will have higher interaction energies  $U$  (where  $U = -\mathbf{p} \cdot \mathbf{E} = -|\mathbf{p}||\mathbf{E}|\cos\theta$ ) than parallel ones, we can find the contribution of the permanent electric dipole of a molecule to the volume electric dipole moment of a bulk sample as follows: consider an equilibrium situation where the thermal energy  $k_B T \gg U$  and we can expand the probability of each dipole's orientation (determined by Boltzmann statistics

$\propto \exp^{-U/k_B T}$ ) keeping only the zeroth and first-order terms. This gives the average dipole moment as

$$\mathbf{p}_{\text{ave}} = |\mathbf{p}|^2 \mathbf{E} / (3k_B T) \quad (36)$$

and the volume polarizability ignoring high frequencies can be written as

$$\alpha = \epsilon_0 + \alpha_i + \alpha_d = \alpha_i + |\mathbf{p}|^2 / (3k_B T) \quad (37)$$

so volume polarizability varies inversely with temperature as expected (at lower temperatures it is easier to re-orient dipoles as  $k_B T$  is closer to  $\mathbf{p} \cdot \mathbf{E}$ ). In the case of a dilute liquid, for instance when a protein is present at low concentration inside a non-polar buffer, and assuming the properties of the solution are the sum of the properties of the components, we can write the effective molar polarizations of each component in terms of their mole fractions. For instance, by replacing  $V/N$  in equation (9) by  $V_m$  the molar volume of the material, we can write the molar polarizability  $\alpha_m = 3\epsilon_0 \left( \frac{\kappa - 1}{\kappa + 2} \right) V_m$

and also the molar polarization  $P_m = \frac{a_m}{3\epsilon_0} = P_o + P_p$  where  $P_o$  and  $P_p$  are the induced and

permanent dipole moments respectively.  $P_o = \alpha_o / 3\epsilon_0$  and  $P_p = |\mathbf{p}|^2 / (9\epsilon_0 k_B T)$ . In this dilute approximation, the molar polarization for an N-component solution would be given by

$$P_m = \sum_i^N X_i P_{mi} \quad \text{where } X_i \text{ is the mole fraction of the } i\text{-th component and } P_{mi} \text{ is its}$$

polarization. By performing an experiment in a step-wise fashion where all the



ingredients are added one at a time (e.g. starting with the buffer base added to a non-polar solvent) one can determine all the  $P_{mi}$  's. In the case of a binary solution with non-polar solvent (i.e. one with only induced polarization) we can approximate the molar polarization of the solvent  $P_{m1}$  as that of pure solvent and using only the first term of

(11) arrive at:  $P_{m1} = \frac{(\kappa_1 - 1)M_1}{(\kappa_1 + 2)\rho_1}$  where  $M_1$  is the mass and  $\rho_1$  the density of the solvent.

Thus to determine the solute molar polarization at each concentration we can use:

$$P_{m2} = P_{m1} + (P_m - P_{m1})\left(\frac{1}{X_2}\right) \quad (38)$$

where  $P_m$  stands for the measured 'bulk' molar polarization of the binary solution. Note here that according to this simplistic formalism one would expect the result of (12) to be independent of concentration since it is supposed to be uniquely determined by the molecular structure. However, it is frequently observed that the polarization increases as the concentration decreases due to significant solvent-solute interactions. As a result, it is customary to report the molar polarization extrapolated to an infinite dilution i.e.  $P_{m2}$  as  $\lim(X_2 \rightarrow 0)$  (cf Homeopathy!!). We address further limitations of this approach below.

Hedestrand's procedure [106] for determining polarizabilities of solutions is based on the above approach plus assumptions that the dielectric constant and the density of the solution are linear in the solute mole fraction, i.e. in our case  $\kappa = \kappa_1 + aX_2$  and  $\rho = \rho_1 + bX_2$  where  $a$  and  $b$  are the derivatives of the dielectric constant and density with respect to mole fraction. Substituting these into (12) one obtains:

$$P_{m2} = \left( \frac{3M_1}{(\kappa_1 + 2)^2 \rho_1} \right) a - \left( \frac{(\kappa_1 - 1)M_1}{(\kappa_1 + 2)\rho_1^2} \right) b + \left( \frac{(\kappa_1 - 1)M_2}{(\kappa_1 + 2)\rho_1} \right) \quad (39)$$

where  $M_1$  and  $M_2$  are the molar masses of the solvent and solute and  $\rho_1$  is the density of the solvent. It can be seen then that we only need to know the limiting slopes of the  $\kappa$  and  $\rho$  versus mole fraction slopes to determine  $P_{m2}$  and these we can obtain by measuring a number of solutions of increasing dilution.

### 5.1.3 Dielectric in Polar Solvent and Generalized Case

When dealing with a protein it is important to realize that modeling it as a dipolar rigid rotator is only justified in very specific cases. In general, proteins have many rigid dipoles, polar substituents such as backbone amides, polar side chains and C-termini. Although constrained to be part of the protein, these have significant freedom and can rotate and translate at low incident field frequencies to give very large dielectric constant to proteins. The generalized Kirkwood-Frohlich theory gives a way to combine the high-frequency dielectric constant with the complicated dipolar contributions to obtain our desired static or DC dielectric constant of the protein in a polar solution. In this approach the sample of dielectric constant  $\epsilon$  is approximated to a collection of permanent rigid dipoles embedded in surroundings of dielectric constant  $\epsilon_\infty$  which represents the sample's high frequency dielectric constant (which can be easily determined from a measurement of the refractive index). Focusing on a spherical region of volume  $V$ , of the order of the size of a molecule of sample and using classical continuum theory the

effective alligning field is calculated ( $E_{eff}$ ) as a function of the average field in the medium  $E$  which results in the following relation [107,108]:

$$\frac{3V\epsilon_o(\epsilon - \epsilon_\infty)(2\epsilon + \epsilon_\infty)}{\epsilon(\epsilon_\infty + 2)^2} = \left( \frac{\partial}{\partial E_{eff}} \langle \vec{M} \cdot \hat{E}_{eff} \rangle \right)_0 \quad (40)$$

where  $\vec{M} = \sum_i \vec{p}_i$  is the total instantaneous dipole moment of the spherical volume  $V$ , the vector sum of the individual dipoles  $\vec{p}_i$ , and it is dotted into the unit vector pointing in the direction of  $E_{eff}$ . The angled brackets denote statistical thermodynamic average and the derivative is evaluated at zero field strength. Note that the  $\vec{p}_i$  have the magnitude of the dipole moments in a theoretical 'gas' phase. A relationship between the thermal fluctuation of  $M$  and in the M.E term can be derived from statistical mechanics and one finally arrives [109] at:

$$\frac{3V\epsilon_o(\epsilon - \epsilon_\infty)(2\epsilon + \epsilon_\infty)}{\epsilon(\epsilon_\infty + 2)^2} = \frac{\langle (\vec{M} \cdot \hat{E}_{eff})^2 \rangle_0 - \langle \vec{M} \cdot \hat{E}_{eff} \rangle_0^2}{k_B T} \quad (41)$$

by including the correction term  $g$  [107] in the right-hand side of the Kirkwood-Frohlich theory  $Ng \frac{p^2}{3k_B T}$  ( $N$  is the number density of dipole molecules,  $p$  as before the 'gas' phase moment of one molecule) one can account for the correlation between dipoles. If  $g = 1$  moments are entirely free from interaction with each other. For  $g > (<) 1$  we have positive (negative) correlation, both physical in the case of polar liquids. So  $g$  is in a sense the ratio of actual fluctuations to theoretical 'gas' uncorrelated fluctuations and it has been shown [109] to be  $g = \sum_{j=1}^{n_d} \langle \cos \theta_{ij} \rangle_0$  where  $\theta_{ij}$  is the angle between dipoles  $\mathbf{p}_i$

and  $\mathbf{p}_j$  and  $n_d$  is the number of dipoles in the sample. Gilson and Honig [109] generalized this to the case of proteins in polar or non-polar environments and *constrained* dipoles and arrived at:

$$g' = \frac{\langle (\vec{M} \cdot \hat{E}_{eff})^2 \rangle_0 - \langle \vec{M} \cdot \hat{E}_{eff} \rangle_0^2}{\sum_{i=1}^{n_d} \left[ \langle (\vec{p}_i \cdot \hat{E}_{eff})^2 \rangle_0 - \langle \vec{p}_i \cdot \hat{E}_{eff} \rangle_0^2 \right]} \quad (42)$$

and also invented a constraint factor  $C$  which accounts for the reduction of the freedom of individual dipoles

$$C = \frac{n_d p^2}{3 \sum_{i=1}^{n_d} \left[ \langle (\vec{p}_i \cdot \hat{E}_{eff})^2 \rangle_0 - \langle \vec{p}_i \cdot \hat{E}_{eff} \rangle_0^2 \right]} \quad (43)$$

And finally we have that:

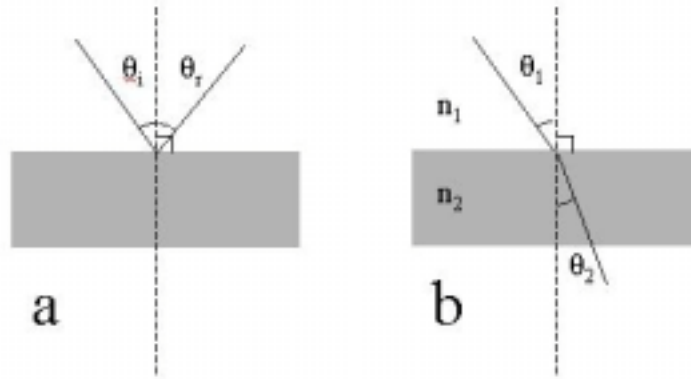
$$\frac{3\epsilon_o(\epsilon - \epsilon_\infty)(2\epsilon + \epsilon_\infty)}{\epsilon(\epsilon_\infty + 2)^2} = \frac{g'}{C} N \frac{p^2}{3k_B T} \quad (44)$$

As seen above, by measuring the dielectric constant of tubulin solution at various concentrations (and incident frequencies) one can experimentally deduce the dipole moment of the free tubulin dimer but it is not a straightforward task. By using a solution with above-critical concentration it is also possible to monitor the changes in the dipole moment as tubulin dimers polymerize into MTs. At high frequencies where only  $\alpha_e$  will contribute, one can use the Clausius-Mossotti equation with the substitution  $\kappa = n^2$  and by measuring the refractive index of the solution arrive at the value of  $|\mathbf{p}_{ave}|$ .

An ideal dielectric contains no free charge, yet parts of its constituent units (individual molecules, polymer filaments etc.) can suffer a localized separation of charge as a result of application of an external electric field

## 5.2 Optics

The two basic laws of optics are the law of reflection:  $\theta_i = \theta_r$  (the angle of incidence is equal to the angle of reflection) and the law of refraction, also known as Snell's law:  $n_1 \sin \theta_1 = n_2 \sin \theta_2$  where  $n_i$  refers to the refractive index of medium  $i$  and  $\theta_i$  is the angle between the normal and the incident and refracted beams see Fig 13. Both these laws refer to specular processes (i.e. the boundary between the media can be assumed smooth) and can be derived from Maxwell's equations for electromagnetic waves incident on a boundary [105].



**Fig. 13. Laws of Optics. a) Law of reflection b) Snell's law**

Using Snell's law for  $n_2 > n_1$  in Fig. 13(b) above, it can be easily shown that there will be a critical angle  $\theta_c = \sin^{-1}(n_1/n_2)$  for a beam incident from  $n_2$  such that the emergent beam will make an angle of  $\theta_1 = 90^\circ$  and will be just grazing the surface. By exceeding this critical angle the beam is reflected back into the material (total internal reflection) and this is of importance in many applications including light guidance by optical fibers,

sensing by surface plasmon resonance and refractometry. Note also that the refractive index is a slow function of temperature:  $n_{T=25^{\circ}C} = n_T - (25.0 - T)(0.00045)$

### 5.2.1 Refractometry

The easiest way to measure  $n$  would be to pass a laser beam at some angle (other than the normal) through a sample of known thickness and measure the beam's deviation from the original path. This presents obvious problems with liquid sample containment etc. so practical refractometers are instead based on the phenomenon of total internal reflection and utilize high-quality prisms that can be tilted to compensate for wavelength-dependent dispersion and thus ordinary sunlight or white light can be used as the source. The machine used for these experiments [Abbe Refractometer, Vista C10] was of exceptional accuracy and particularly elegant design requiring no electrical power. Briefly, light was allowed to enter and be reflected into a prism which was coated with the material of interest and covered. The prism's refractive index was known and the beam's incident angle was tilted until total internal reflection was reached (seen as a dark band in the eyepiece). The refractive index of the sample was then read on a pre-calibrated scale. This method depends on the prism having a higher refractive index than the material. Our machine was capable of measuring refractive indices between 1.3000 and 1.7000. After standard calibration and prior to measurement of tubulin solutions a number of different NaCl solutions of varying concentration were used as additional calibration. Determining the exact concentration was the main source of error in this measurement so high precision electronic scales and precision micro pipettes

were used. The prism was cleaned after each measurement with ethanol soaked cotton and left to dry before applying the next sample. It was found that 30 to 50  $\mu\text{L}$  of solution were adequate to deposit a thin film on the prism such that there was virtually no noise (indicated as colors). This small volume is comparable to the requirements of the sophisticated BIAcore 3000 machine for a single injection.

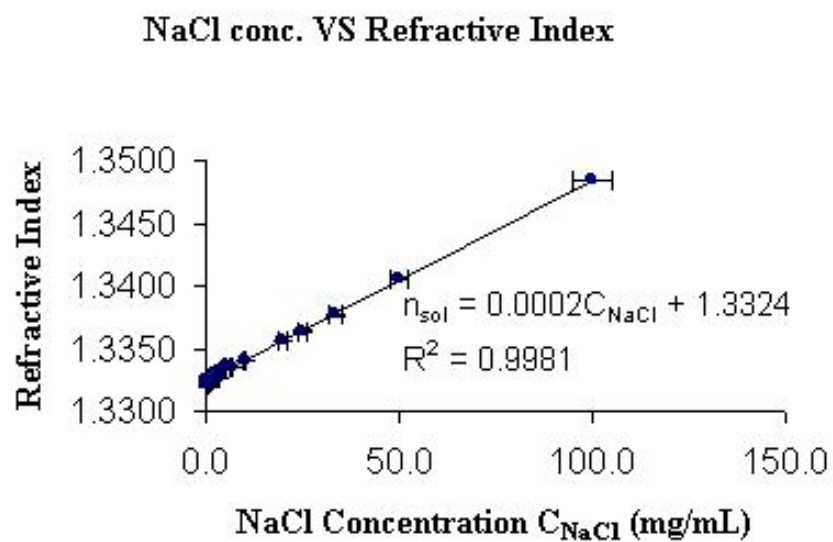
#### 5.2.1.1 Refractometry Results

The refractive index of a series of concentrations of NaCl (in 18.1M $\Omega$  H<sub>2</sub>O) and tubulin in buffer (0.1M 4-Morpholinoethane sulphonic acid (MES), 1mM EGTA, 0.1mM EDTA, 0.5mMMgCl<sub>2</sub>, 1mM GTP at pH 6.4) was measured. Three measurements were taken for each data point and the average is shown in Table 3. Errors are estimated at ~5% for concentration (shown). The refractometer was scale limited with an error of 0.00005 for  $n$  (not shown, represented as the size of the data points. In Figures 14, 15 a least-squares fit linear regression yields straight lines with R factors 0.9981 and 0.9928 respectively. The intercepts were manually set to the zero-point concentration averages. A limited second set of data points was taken ( $n_{\text{tub}2}$ ) at several times after the first but as it was practically impossible to keep the timing consistent it is only shown here for qualitative purposes. The results at different times did not deviate appreciably suggesting that at this wavelength range tubulin dimers and microtubules have similar refractive indices.

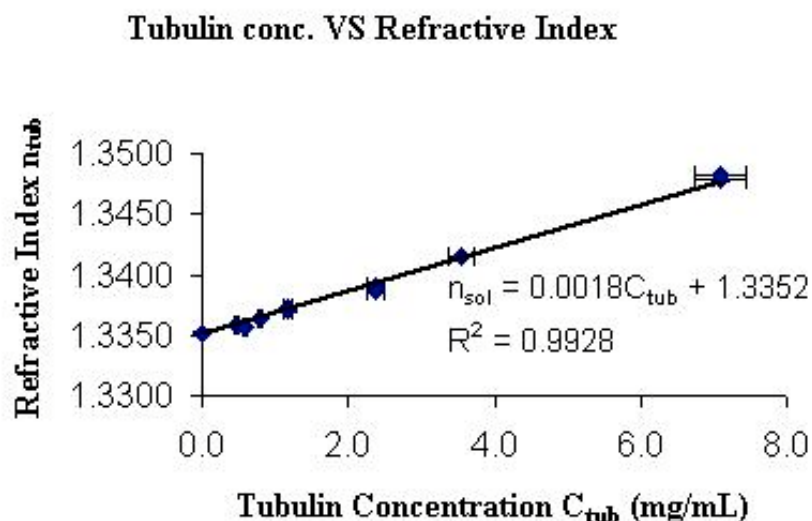


NaCl (mg/mL)	n <sub>NaCl</sub>	Tub (mg/mL)	n <sub>tub1</sub>	n <sub>tub2</sub>	time (min)
0.000	1.3324	0.00	1.3352	1.3352	40
0.084	1.3321	0.00	1.3351	1.3353	51
0.167	1.3324	3.55	1.3415		
0.208	1.3324	2.37	1.3386	1.3380	15
0.333	1.3325	1.18	1.3370	1.3371	17
0.416	1.3321	0.789	1.3364	1.3364	25
0.833	1.3323	0.592	1.3357	1.3360	25
1.67	1.3325	7.10	1.3478	1.3489	29
2.50	1.3329	7.10	1.3482		7
3.33	1.3327	0.592	1.3357	1.3360	42
5.00	1.3335	1.183	1.3372	1.3370	45
6.67	1.3335	2.37	1.3390	1.3390	47
10.0	1.3341	0.473	1.3358	1.3358	55
20.0	1.3356				
25.0	1.3364				
33.3	1.3377				
50.0	1.3406				
100.	1.3484				

Table 3. Refractometry Data.



**Fig. 14. NaCl Concentration vs Refractive Index.** Note the low value of the slope (compared to tubulin).



**Fig. 15. Tubulin Concentration vs Refractive Index.**

Note how a very small change in concentration of tubulin results in a large jump in the index of refraction (Fig. 15) giving a slope of  $\Delta n/\Delta C = 1.800 \pm 0.090 \times 10^{-3}$  (strongly corroborated by the SPR measurement of the same value which gave  $1.80 \pm 0.20 \times 10^{-3}$ ). Compare this to  $\Delta n/\Delta C \sim 0.0002$  for the NaCl solution.

A physiological concentration is assumed at  $15.0 \mu\text{M}$  (i.e.  $1.50 \times 10^{-5} \text{ mol/L}$ ) [110]. Since the molecular weight of a tubulin dimer is 110kD this gives a proportionality of  $1.00 \text{ mg/mL} \sim 9.10 \mu\text{M}$  so  $15.0 \mu\text{M}$  is equivalent to  $1.60 \text{ mg/mL}$  and this gives a molecular density of  $N = 9.03 \times 10^{18}$  tubulin molecules per liter or  $9.03 \times 10^{21}$  per  $\text{m}^3$ . Note that the concentration necessarily varies across cell types, intracellular position and cell condition. For instance, although a TAU-burdened cell has the same overall tubulin

density, it has much higher local axonal and dendritic density of tubulin when MTs have deteriorated into neurofibrillary tangles.

The partial contribution to the refractive index of the solution by tubulin can be found if the density dependence on concentration of the solution is known (see Fig. 15). Assuming that the contributions from the various components are additive linearly, we have for the total index of refraction of the solution  $n_{sol} = \sum_i C_i n_i$  where  $C_i$  and  $n_i$  are the fractional concentration of the  $i$ th component with refractive index  $n_i$  and  $i$  runs over all components. Lumping the contribution from all the buffer components we can write

$$n_{sol} = (1 - \chi_{tub})n_{buffer} + \chi_{tub}n_{tub} \Rightarrow n_{tub} = \frac{n_{sol} - (1 - \chi_{tub})n_{buffer}}{\chi_{tub}} \quad (45)$$

Where  $\chi_{tub} = C_{tub} / \rho$  the mass fraction and  $\rho$  is the density of the solution. It could be argued that using a volume fraction is more appropriate here but for our purposes a mass fraction is adequate and simpler. At  $C_{tub} = 1.60\text{mg/mL}$ ,  $n_{sol} = 1.8000 \times 10^{-3} C_{tub} + 1.3352$  (from Fig. 15) gives  $n_{sol} = 1.34 \pm 0.07$  and using the measured value for the solution density  $\rho =$  at  $C_{tub}=1.60\text{mg/mL}$  we arrive at the value for  $n_{tub}$

$$n_{tub} = 2.90 \pm 0.10 \quad (46)$$

which can be used in

$$\kappa = n^2 \quad (47)$$

to give the high frequency tubulin dielectric constant

$$\kappa = 8.41 \pm 0.20 \quad (48)$$

A thorough search of the bibliography suggests that this is likely the first time these two quantities have been experimentally determined for tubulin.

Both  $n$  and  $\kappa$  are at the very top range of what is usually assumed for proteins, as expected since tubulin seems to have such a high dipole moment in molecular dynamics simulations.

The refractive index  $n$  of an optically dense material is related to the high frequency polarizability  $\alpha$  via:

$$n^2 = 1 + \frac{N\alpha}{\epsilon_o} \frac{1}{\left(1 - \frac{N\alpha}{3\epsilon_o}\right)} \quad (49)$$

where  $N$  is the molecular concentration in which for our chosen concentration is  $9.03 \times 10^{21}$  molecules/m<sup>3</sup>. Solving the above equation for  $\alpha$  gives

$$\alpha = \frac{\epsilon_o}{N} \frac{3(n^2 - 1)}{(n^2 + 2)} \quad (50)$$

and therefore the high frequency tubulin polarizability is

$$\alpha = 2.1 \pm 0.1 \times 10^{-33} \text{ C m}^2/\text{V} \quad (51)$$

A very large number owing to the evidently large dipole moment of tubulin. Note that the generally accepted value of the density of proteins is 1.45gr/mL [111]

## 5.3 Surface Plasmon Resonance

### 5.3.1 SPR Basics

The technique of surface plasmon resonance (SPR) [112,113] allows measurement of changes in the optical properties of a medium adjacent to a thin metal film. Practical applications of the SPR method include chemical sensors [114,115] and biosensors [116]. Specifically, the SPR technique is by now a well-established method for the analysis of interactions among biomolecules [117]. SPR curves (sensograms) can be measured either by varying the angle or the wavelength of the incident light [118,119,120]. Here, we discuss our application of the SPR technique to measurement of the dielectric properties of the bovine cytoskeletal protein tubulin.

A surface plasmon (SP) is an electromagnetic wave that can propagate along the surface of a dielectric-metal interface [113]. Surface plasmons can be excited by shining light on a layered system consisting of a transparent medium on one side, a metal film (most often gold or silver) and a dielectric on the other. When the light is incident at an angle greater than the critical angle of total internal reflection, an evanescent wave is produced and penetrates into the adjacent medium to a depth of the order of one wavelength. The maximum coupling between the evanescent wave and the surface plasmon takes place when their phase velocities coincide at which point the surface plasmon is excited at resonance. Thus, the surface plasmon resonance (SPR) occurs at a characteristic angle of incidence. This angle depends on the thickness as well as the dielectric permittivities of the layers of the adjacent media. Since the effective

permittivities depend on the frequency of the exciting laser light, the resonance angle does too. The most convenient geometry for the development of a sensor is the Kretschmann-Raether configuration which consists of a glass prism, a metal film and the adjacent medium that is to be probed.

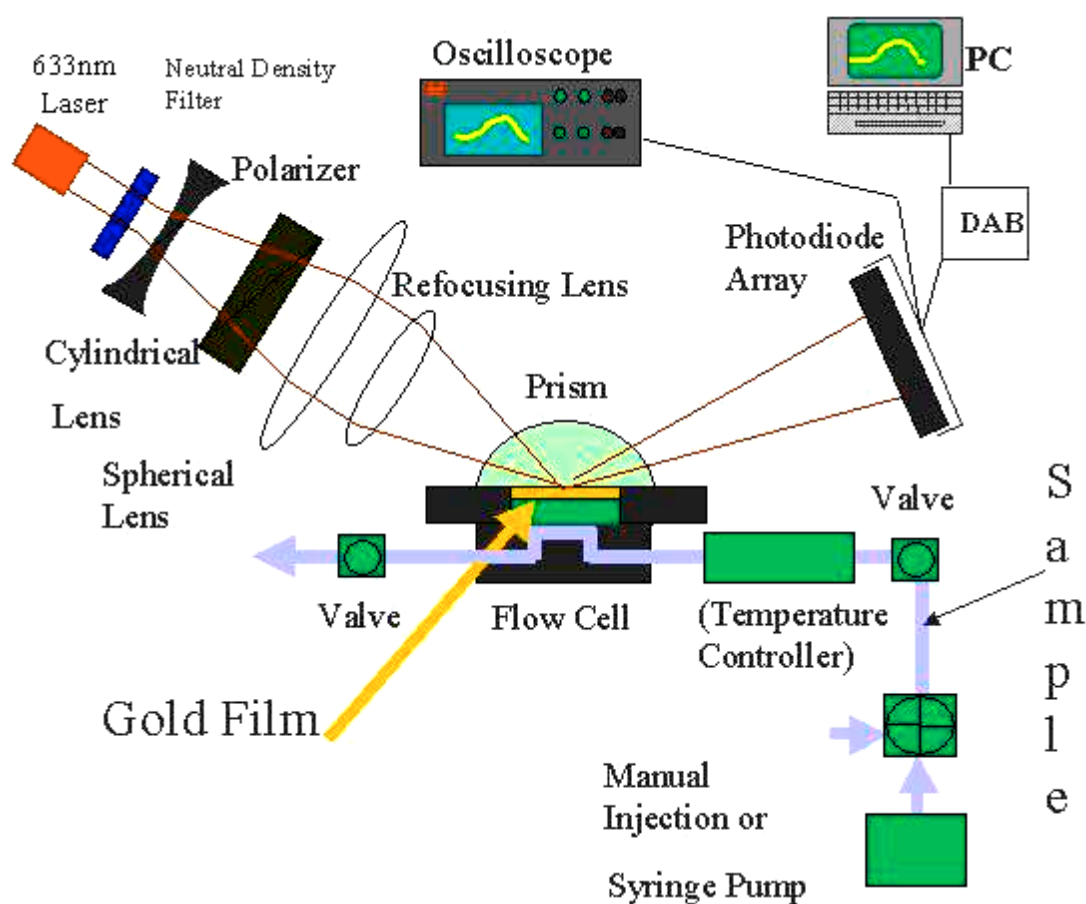
### **5.3.2 The SPR Sensor**

Fig. 16 shows the experimental arrangement of our custom-built SPR sensor. In addition to the experimental arrangement shown, we used the commercial SPR-based BIAcore 3000 and 1000 sensors, which furnished the additional convenience of automated injection of very small volumes of analyte solutions and allowed for cross-checking of results.

#### **5.3.2.1 Optics and Data Acquisition**

A helium-neon laser provided the incident illumination at 633 nm (or 760nm in the BIAcore). A p-polarized light beam convergent in an angular interval was produced with an arrangement of lenses and a polarizer. A prism provided the coupling of the laser beam to the SPs that were excited in the gold film, and a multiple-channel custom-build (see below) flow cell allowed solution access to the gold film. The angular distribution of the reflected light was measured with a photodiode array and its electrical output was read with a data acquisition (DAQ) board and transferred to a PC computer using software developed in-house by the author. The readout rate of the DAQ board set the time resolution to 67 milliseconds. The spatial resolution was determined by the

dimensions of the laser beam spot at the surface: 0.5 mm×0.3 mm. The angular resolution for the configuration used was  $\sim 1$  resonant unit (RU); this angular unit, commonly used in SPR measurements, corresponds to  $10^{-4}$  degrees. The change of the SPR angle by this quantity occurred when the change of the refractive index was only approximately  $10^{-6}$  [21].



**Fig. 16. Experimental Setup of the SPR Sensor.** Sample flow is indicated with light blue. DAB: data acquisition board. The prism provides the coupling of the excitation light to the surface plasmon. The polarizer P is used to produce the p-polarized light, since only this component interacts with the surface plasmon. The angular distribution of the reflected light intensity is detected by the photodiode array (PDA) which can be replaced by just two photodiodes with differential lock-in detection. The sample medium is injected into a small flow cell adjacent to the gold film. The fluidic cell presented a serious challenge and is described separately below.



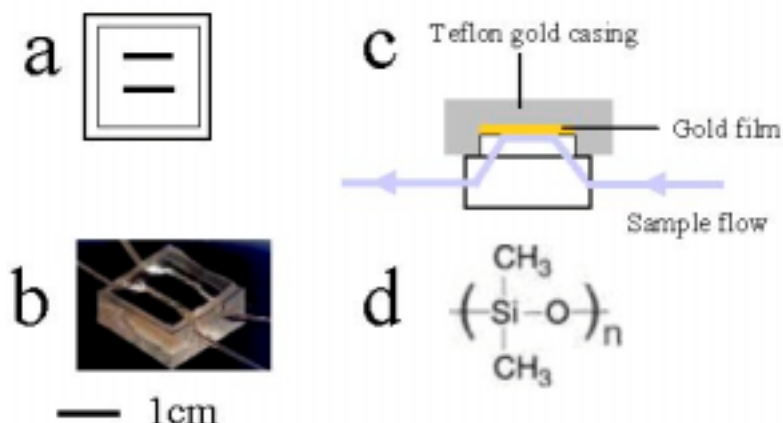
### 5.3.2.2 Fluidic Cell

One of the serious challenges in an SPR measurement is the management and routing of the samples. In commercial devices, such as the BIAcore 3000, proprietary microfluidic technology based on lithography casting is used and injections require robot arm handling and sophisticated electronics raising the cost of the device by several hundred thousand dollars. Previous methods used for in-house SPR measurements used hand-cut rubber and micro-machined plexiglass cells and manual injection using microsyringes. In both rubber and plexiglass cell designs, significant errors were introduced as a result of misalignment of the various cell parts, evaporation of sample and presence of air bubbles. In our apparatus, to bring a series of 30-100 $\mu$ L sample injections into close contact with a vertical gold film, avoiding air bubbles and mixing of samples, a casting technique was developed as follows. Using AutoCAD software, channels of precise dimensions (3mmx0.5mm and 3mmx0.3mm) were laser printed on thin plastic sheets (overhead transparencies). Those were then cut by hand under a dissecting stereoscope and pushed against modeling clay. The clay was pliable enough to follow the contours imposed by the plastic sheet positive and after oven curing became the negative mold.

Poly-Di-Methyl-Siliconate (PDMS) (was used as the material for a fluidic cell. PDMS was found to be ideal for this application because it is biologically inert and virtually indestructible. Unfortunately, the material is non-machineable as holes drilled

tend to self-seal but this was eventually advantageous for our purposes facilitating channel-syringe interfaces. None of the chemicals tried (ethanols, xylenes, acetone, hydrochloric acid) left any trace of abrasion, and freezing in liquid nitrogen and heating with an acetylene torch produced no effect. The material is transparent and we also found that this polymer is non-homogeneous in its fluorescence properties. Seemingly random parts of a large piece of PDMS would fluoresce strongly when exposed to UV laser illumination while others would be entirely transparent. This may be the result of domains of specially oriented polymer strands in the bulk of the material and would be interesting to investigate in a separate project. Stainless steel tubes (outer diameter 0.002, inner 0.001in) were used to interface with the channels and provided a way to inject and clear sample (see Fig. 16, 17). The mold and PDMS were de-gassed in a low-vacuum (200mTorr) custom-built chamber and left to dry for 24 hours. The elasticity of the final product was of importance as if too elastic it would deform under pressure during sample injection and if too stiff it would not form the close contact needed to avoid evaporation. Elasticity was controlled by addition of curing and viscosity agents (Sylgard 186/184 and D.C. 200 respectively) and finding the optimum ratio.

The technique described above allowed us to comfortably have up to four independently-addressable channels while previously only one or at most two were possible. The limiting factor for the number of channels is the accuracy of the human hand in cutting the positives under a stereoscope. Delegating this task to a metal-deposition circuit board machine such as the T-Tech 700 would make it possible to obtain up to 8 channels before encountering problems with self-sealing.



**Fig. 17. PDMS Fluidic Cell.** **a)** Top view **b)** photograph of a two-channel cell **c)** side view **d)** PDMS chemical composition formula. The parenthesis is repeated n times (polymer)

### 5.3.2.3 Theoretical Model

To obtain quantitative data, we use a five-layer model that is based on Maxwell's equations describing reflection of light from a layered system. This enabled us to calculate SPR curves, estimate SPR response from protein immobilization and estimate changes in dielectric permittivity. We consider a structure with five layers: layer 1 consists of a prism with dielectric permittivity  $\epsilon_1=2.30$ , layer 2 consists of a gold film of thickness  $d_2=47$  nm with complex permittivity  $\epsilon_2 = -13.2 + i1.25$ , layer 3 consists of a dextran layer filled with high relaxation (HR) solution of thickness  $d_3=140$  nm [122] and  $\epsilon_3=1.78$  in the case of the sarcomeres, and with buffer in the case of tubulin, layer 4 consists of our sample medium (tubulin) with thickness  $d_4$  and layer 5 consists of only solution. The fifth layer is assumed to be semi-infinite with respect to surface plasmon penetration depth. One can obtain the intensity reflection coefficient  $R$  for this system

with the following recursive formula [123] by calculating each input impedance  $Z_{in,m}$  and each layer impedance  $Z_m$ .

$$R = \left| \frac{Z_{in,2} - Z_1}{Z_{in,2} + Z_1} \right|^2 \quad (52)$$

The input impedance at layer  $m$  ( $Z_{in,m}$ ) and layer impedance ( $Z_m$ ) are obtained from,

$$Z_{in,m} = Z_m \left[ \frac{Z_{in,m+1} - iZ_m \tan(k_{z,m} d_m)}{Z_m - iZ_{in,m+1} \tan(k_{z,m} d_m)} \right], \quad m=2,3,4 \quad (53)$$

where,

$$Z_{in,5} = Z_5, \quad Z_m = \frac{k_{z,m}}{\epsilon_m k_0}, \quad k_{z,m} = \sqrt{\epsilon_m k_0^2 - k^2}, \quad k = k_0 \sqrt{\epsilon_1} \sin(\theta), \quad k_0 = \frac{2\pi}{\lambda} \quad (54)$$

The wavelength of laser in vacuum is  $\lambda$ . The incidence angle  $\theta$  of light onto the prism-gold interface determines the component of the wave vector  $k$  that is parallel to the interface. A change in dielectric permittivity of sarcomeres or tubulin solution ( $\epsilon_4$ ) will alter the reflection coefficient  $R$ . Once the change in the SPR angle  $\Delta\theta_{SPR}$  for different media is experimentally determined, the corresponding change in the dielectric constant ( $\Delta\epsilon_4$ ) can be calculated from equations (2) and (3) and the change in the refractive index  $n$  inferred from  $\epsilon = n^2$ .

The decrease of the SPR sensitivity to changes in the dielectric permittivity with depth  $z$  starting from the boundary between 3<sup>rd</sup> and 4<sup>th</sup> layers into the protein sample was calculated. This decrease can be approximated as  $\sim e^{-(z/d_p)}$  and the characteristic penetration depth  $d_p$  can be calculated to be 110 nm [123]. For BIAcore, and  $\lambda=760\text{nm}$   $d_p \geq 110\text{nm}$  and therefore we do not expect to see saturation of the signal due to

sensitivity degradation. This can also be seen if one considers that each free tubulin dimer occupies one binding site on the dextran surface thus saturation is achieved when the total mass of immobilized protein reaches that of a monomolecular layer (with thickness of  $\leq 10\text{nm}$ ).

#### 5.3.2.4 Tubulin and Immobilization

Following established protocols [124], tubulin was purified from bovine cerebra (provided courtesy of R.F. Luduena). Our SPR measurements took place at  $24^{\circ}\text{C}$  and the time between injection and measurement was of the order of 10 s. Measurements were taken for times up to 5 minutes. Tubulin does not polymerize at  $0^{\circ}\text{C}$  and although 10sec is adequate time for our sample of  $50\text{ }\mu\text{L}$  to reach room temperature and start polymerizing, we are confident that in our measurements mainly free tubulin dimers were present and not MTs since (using spectrophotometry and monitoring the absorption curve) we had previously determined that the characteristic time for our tubulin to polymerize into MTs was of the order of 45 minutes at room temperature (data not shown) agreeing with literature [125].

Gold film chips (CM5) coated with carboxymethylated dextran were obtained from BIAcore (Biacore AB, Sweden). Using standard chemical activation/deactivation protocols [126], we introduced N-hydroxysuccinimide esters into the surface matrix of the chip by modifying the carboxymethyl groups with a mixture of N-hydroxysuccinimide (NHS) and N-ethyl-N'-(dimethyl-aminopropyl)-carbodiimide

(EDC). These esters then form covalent bonds with the amine groups present in the ligand molecules thus immobilizing them on the surface.

Effective immobilization requires that the pH be lower than the isoelectric point of the protein; however, lowering pH below 4.9 eliminates tubulin function and was avoided.

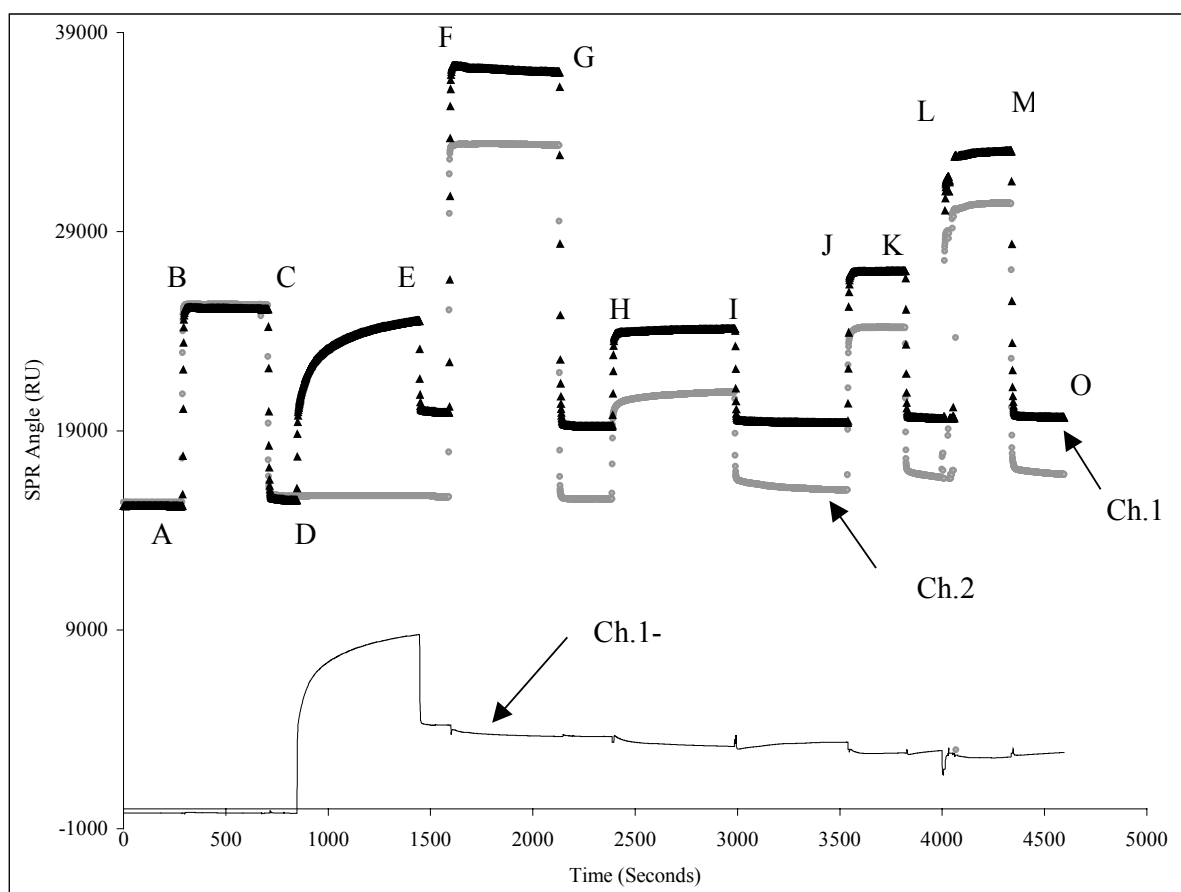
The temperature controller raised and maintained the temperature of the inflow at 26°C..

### 5.3.3 Surface Plasmon Resonance Results

In this setup, a 1ng/mm<sup>2</sup> surface immobilization yields a signal of 1kRU and the laser spot size on the gold chip is 1.2 mm<sup>2</sup>. As shown in Fig. 18, after tubulin immobilization and application of a high flow rate (20 nL/min) of running buffer to wash away any weakly-bound protein, the average response was ~4 kRU which means 4.8 ng of protein (i.e.  $2.6 \times 10^{10}$  individual tubulin dimers) were captured by the dextran. A reference cell on the same chip without any immobilized tubulin was used as control and any non-immobilization relevant signals (such as due to refractive index changes) were automatically subtracted.

Electron crystallography measurements on zinc-induced tubulin protofilament sheets have shown that the tubulin heterodimer has dimensions 46 X 80 X 65 Å [4,5,6] so the footprint of the molecule on the surface can be between 30 nm<sup>2</sup> minimum and 52 nm<sup>2</sup> maximum depending on orientation. Using the average of these two values, it can be seen that a monomolecular layer covering the 1.2 mm<sup>2</sup> spot would require  $3.0 \times 10^{10}$  individual tubulin molecules, leading us to believe that we have achieved 87% coverage,

an observation corroborated by the immobilization part of the sensogram where a tendency towards saturation can be clearly seen (Fig. 18 D→E).



**Figure 18. BIAcore3000 sensogram for tubulin.** Tubulin was immobilized on Channel 1. Channel 2 was treated identically to Channel 1 but had no tubulin. Ch.1 - Ch.2 shows tubulin signal - background. A→B: running buffer. B→C: EDC/NHS dextran-activating complex injected, note identical response of both channels. C→D: running buffer. D→E: Ch.1 shows tubulin immobilization with a clear tendency towards saturation, Ch.2 remains at running buffer baseline level. E→F: high flow rate running buffer. Difference between Ch1. and Ch.2 shows amount of immobilized tubulin ~4000RU. F→G: ethanolamine blocking (dextran-deactivation). G→H: running buffer. H→I: 0.51mg/ml tubulin in Ch.1. Since both channels exhibit same signal, all signal is due to refractive index change, not tubulin-tubulin binding (there is slight non-specific binding to Ch.2). I→J: running buffer. J→K: 1.70mg/ml tubulin in Ch.1, all signal is due to refractive index change. K→L: running buffer, L→M: 5.1mg/ml tubulin in Ch.1, all signal is due to refractive index change. Slight noise in the forms of bumps in Ch1-Ch.2 is due to 0.5 sec delay between measurement of Ch.1 and Ch. 2 and subsequent subtraction. Bump at around 4000sec is due to the temporary presence of a bubble in the 5.1mg/ml tubulin sample.

*In vitro* polymerization happens spontaneously at room temperature (also at 37°C only faster) if the protein concentration is above critical and the buffer contains adequate GTP. The critical concentration varies for different tubulin preparations. By using spectrophotometry, we determined that our tubulin started polymerizing at room temperature when concentration exceeded 1.0mg/ml (data not shown). In order to determine the dielectric constant of tubulin we first had to be sure that the shift in SPR angle was due to the change in the refractive index of the solution floating over the gold chip and not due to further immobilization of protein or perhaps tubulin-tubulin binding (polymerization).

To address the first concern, we performed the experiment in parallel, utilizing a reference channel on the same chip but without any tubulin in it. The reference signal was automatically subtracted from the tubulin signal thus also addressing concerns related to non-specific binding to deactivated dextran. To eliminate the possibility that our signal was due to further tubulin-tubulin interactions on the surface (polymerization) we tried both below critical (0.51mg/ml) and above critical (1.7mg/ml and 5.1mg/ml) concentrations and saw return to baseline in all cases showing that in this environment tubulin was incapable of polymerization, a fact that may be due to dextran binding and/or insufficient nucleation sites. Using the sensogram of Fig. 18 we calculated the changes of the refractive index and dielectric constant with tubulin concentration:

$$\frac{\Delta n}{\Delta c} = (1.85 \pm 0.20) \times 10^{-3} (mg / ml)^{-1} \Rightarrow \frac{\Delta \epsilon}{\Delta c} = (5.0 \pm 0.5) \times 10^{-3} (mg / ml)^{-1} \quad (55)$$



where  $\Delta n$  and  $\Delta \epsilon$  are the changes in the refractive index  $n$  and dielectric constant  $\epsilon$ ;  $\Delta c$  is the change in concentration  $c$ .

Since saturation occurs at only  $\sim 4\text{kRU}$  (nearly a monomolecular layer of tubulin), our assertion that we are dealing with free tubulin dimers is supported as each dimer must occupy one dextran binding site and there is no tubulin-tubulin binding or aggregation/polymerization into MTs.

As the dielectric constant and refractive index of a solution are intimately connected to the polarizability and consequently to the dipole moment of its constituents, these measurements show that SPR can be used to further elucidate the dielectric properties of 'live' proteins in solution.

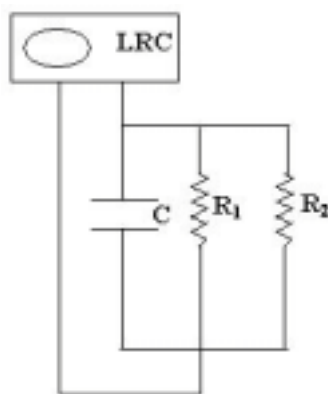
#### **5.3.4 Refractometry-SPR Comparison**

Both refractometry and SPR, two methods based on the same underlying physical principles yet very far apart in implementation, gave a  $\Delta n/\Delta c$  of  $1.8 \times 10^{-3}$ , a strong indication that these methods are consistent, our apparatus properly calibrated and our analysis correct. In summary, refractometry and SPR gave consistent results for the dielectric constant and polarizability of tubulin. These methods alone cannot provide the permanent dipole moment of the molecule since they address only the high frequency region where the permanent dipole is 'frozen out'..

## 5.4 Dielectric Spectroscopy

### 5.4.1 Simplified Case

To illustrate the main principles behind the method used, consider the simplest way to measure the low-frequency dielectric constant of a solution: a capacitor-resistor (RC) circuit.



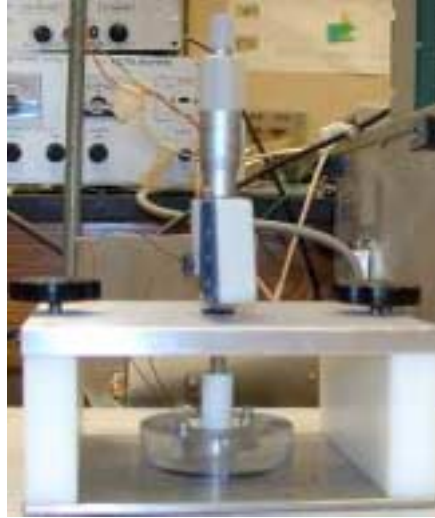
**Fig. 19. LRC Bridge.**

The capacitance  $C$  of a flow cell with conducting parallel-plate walls can be measured first filled with air and then filled with the tubulin-buffer solution for various tubulin concentrations.  $R_1$  is assumed to be infinite in the case of air and some finite but very large value (of the order of  $10\text{M}\Omega$ ) in the case of solution.  $R_2$  is set to a known value (e.g.  $5\text{k}\Omega$ ) and is needed to overwhelm any small conductance due to the presence of liquid between the plates so that the equivalent resistance in the circuit is identical for all the measurements. The inductance-resistance-capacitance (LRC) bridge performs the measurement at several low to medium frequencies (e.g.  $100\text{Hz}$  to  $1\text{kHz}$ ) by measuring the RC time constant and displaying the total equivalent resistance and capacitance for

the circuit. The ratio  $C'/C$  for the tubulin/air capacitances then gives  $\kappa$  and from equation (9) the dipole moment can be inferred. Unfortunately, a simple RC circuit with low inductance connected to a bridge such as the one described above and shown in Fig. 19 is not ideal because aqueous solutions tend to have high conductivity through the solution and form double layers at the electrodes giving extremely high values for  $\kappa$  at low frequencies. A further complication arises from the requirement that the sample volumes be as small as possible as purified proteins and especially tubulin are expensive.

#### 5.4.2 Capacitor and Signal Analyzer

A more sophisticated approach was followed involving the measurement of the transfer function through a sample contained in a custom-build small volume capacitor. A signal analyzer (SR 780 Stanford Research Systems, Inc.) was used that sampled the real and imaginary parts of the transfer function in the 1kHz-100kHz frequency range. The device was calibrated with water, alcohol and methanol and by employing the distance variation polarization-removal technique it was possible to extract information about the lower limit of the frequency range even though individual scans were swamped by the electrode polarization effects below about 10kHz. The experimental set-up is shown in Fig. 20. A custom built capacitor probe was used with stainless steel parallel plates of 27mm diameter and a micrometer-control distance. The distance control was reproducible down to the 3 $\mu$ m level.



**Fig. 20. Custom Built Capacitor.** The capacitor had stainless steel plates of variable diameter (27mm was used), a precision digital micrometer controlling the plate separation (to 3 $\mu$ m precision) , a plexiglass sample holder (sample ~1mL)

The signal analyzer provides a sinusoidal voltage to the capacitor. The ratio of the output of channel 1 to that of channel 2 is recorded as a function of frequency.

The real and imaginary parts of the ratio are stored separately for additional processing by software. Amplifier  $A_2$  is used to hold the electrode at ground potential. As a result, alternating current  $I$  exists in the sample and produces a voltage drop  $V_1$  where  $V_1 = IZ$ . The voltage  $V_2$  is equal to the product of current  $I$  and the resistor  $R_2$ . Thus the transfer function is related to impedance of the sample through

$$\frac{V_2}{V_1} = \frac{R_2}{Z} \quad (56)$$

$R_1$  provides an upper limit for the current when the impedance is smaller. The Amplifier (AD797, 9729, G 21701 ) has unit gain and also provides buffering to channel 1.

The main source of error in measuring biological impedance is due to electrode polarization. This effect becomes very strong when measurements are carried out at low frequencies. We minimized this effect as follows. The measured impedance  $Z^O$  is the sum of the sample impedance and the polarization impedance  $Z^P$ . We took two measurements of each sample at slightly different plate separations yielding  $Z^O_1$  and  $Z^O_2$  where,

$$\begin{aligned} Z^S_1 + Z^P &= Z^O_1 \\ Z^S_2 + Z^P &= Z^O_2 \end{aligned} \tag{57}$$

Since the polarization effect is assumed to be the same in both cases, subtracting the two measurements gives

$$Z^S_1 - Z^S_2 = Z^O_1 - Z^O_2 \tag{58}$$

Our parallel plate capacitor had capacitance  $C = \frac{\epsilon A}{d}$ , where  $\epsilon$  is the dielectric permittivity of the suspension and  $A$  is the plate area and  $d$  is of the electrode separation and since the capacitor impedance is given by  $Z =$

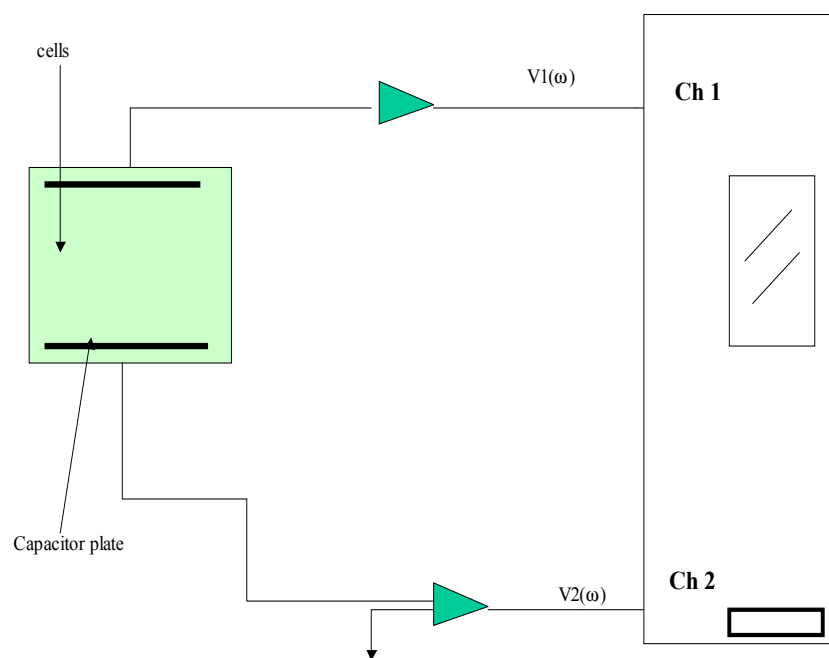
$$Z^O_1 - Z^O_2 = \frac{d_1 - d_2}{(\sigma + i\omega\epsilon)A} \tag{59}$$

This leads to the two dispersion curves:

$$\sigma(\omega) = \text{Re}(Z_1^0 - Z_2^0) = \text{Re} \frac{d_1 - d_2}{A(Z_1 - Z_2)} \quad (60)$$

$$\varepsilon(\omega) = \text{Im}(Z_1^0 - Z_2^0) = \text{Im} \frac{d_1 - d_2}{\omega A(Z_1 - Z_2)} \quad (61)$$

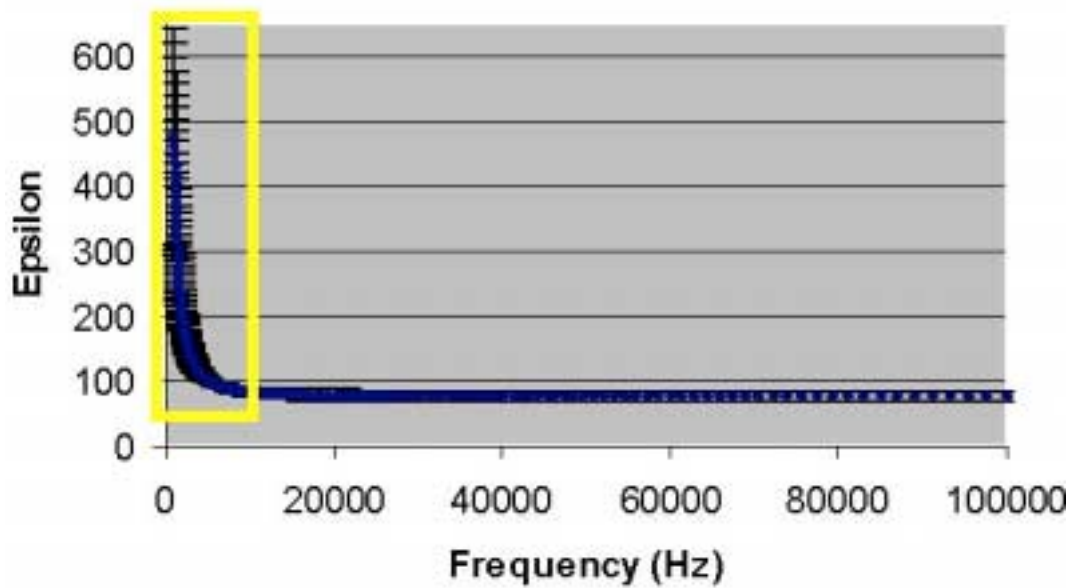
where  $\sigma(\omega)$  and  $\varepsilon(\omega)$  are the frequency dependent conductivity and permittivity of the sample respectively. It is thus seen that by obtaining the imaginary part of the transfer function, one can deduce  $\varepsilon(\omega)$ .



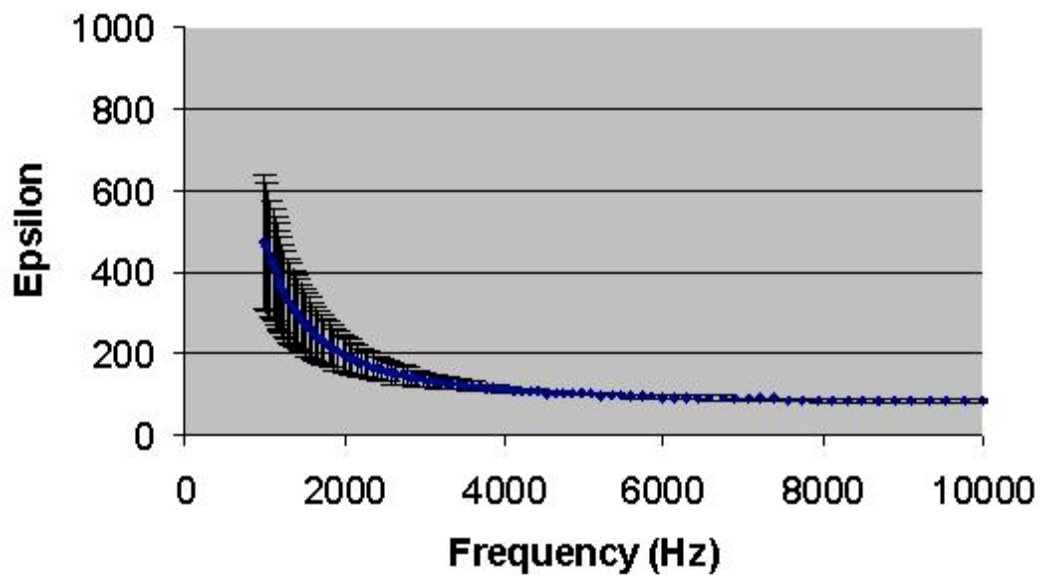
**Figure 21. Circuit Diagram of Signal Analyzer and Capacitor**

### 5.4.3 Calibration and Errors

Data was taken with the network (signal) analyzer shown in Fig. 21 above. For each run, 198 data points were obtained in a logarithmic spread covering the range of 1kHz-100kHz. Each run was repeated at least 3 times. Because of the large number of data points, tabulating the results is impractical so only plots of the average values will be shown.



**Fig. 22. Water Calibration.** Pure, deionized water (18.0mOhm) tends to an relative permittivity of 75 at high frequency. The sharp rise near DC frequencies (highlighted in yellow box) was used to illustrate the polarization effect contribution to experimental error (see next figure for close-up of error bars).

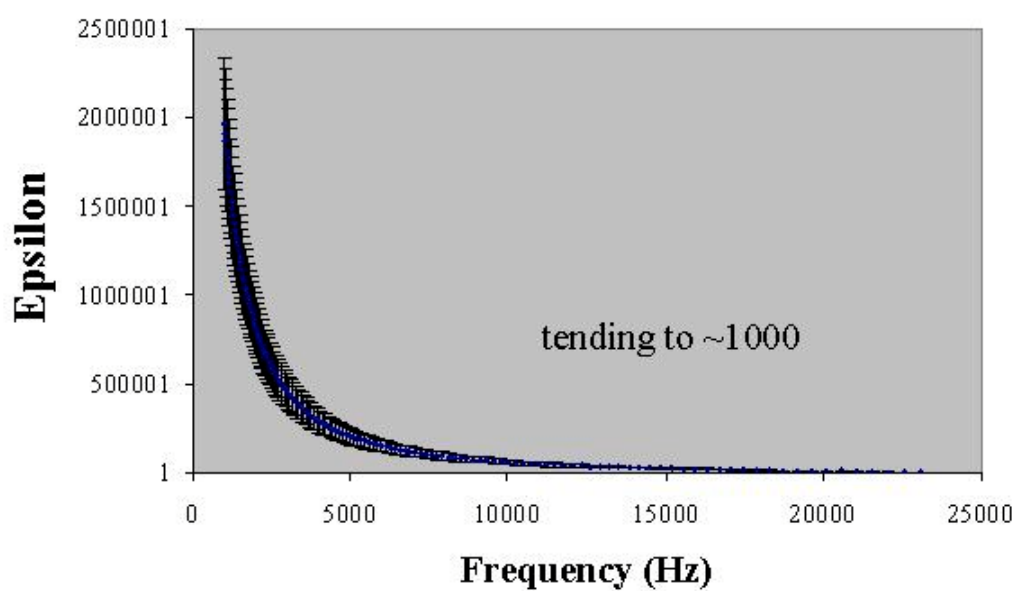


**Fig. 23. Calibration Close-up.** A close-up of the water calibration data is shown, note the exponential increase of the error bars (derived by calculating the standard deviation of 10 measurements) indicating that tubulin data near DC frequencies will be unreliable.

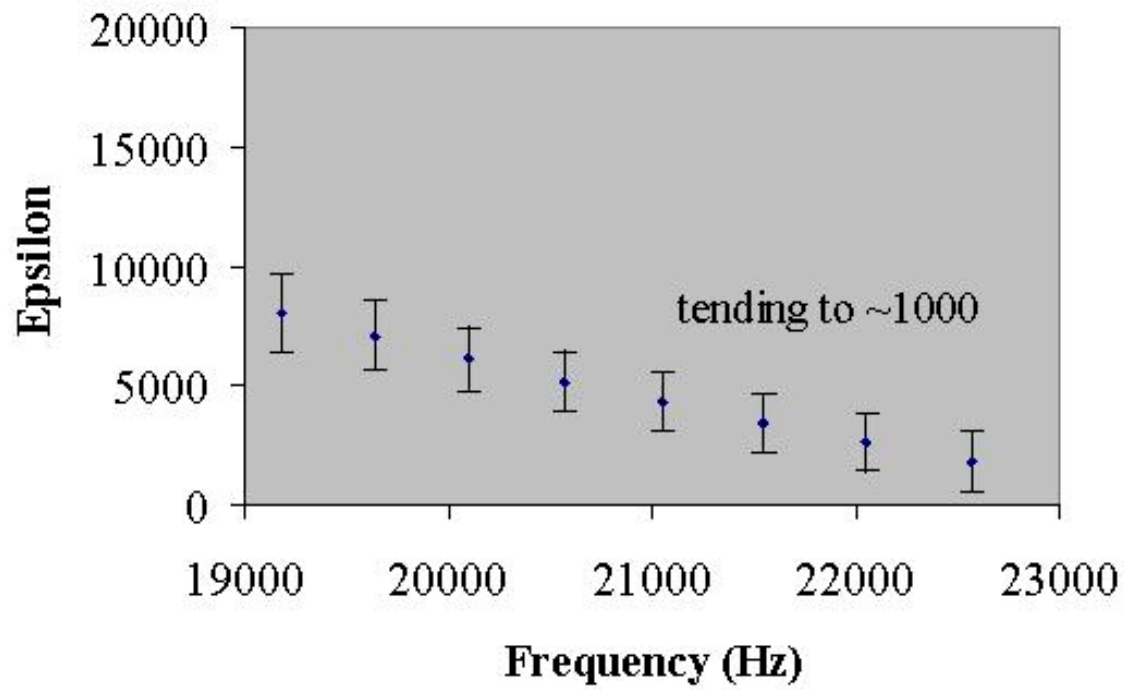


#### 5.4.4 Dielectric Spectroscopy Results

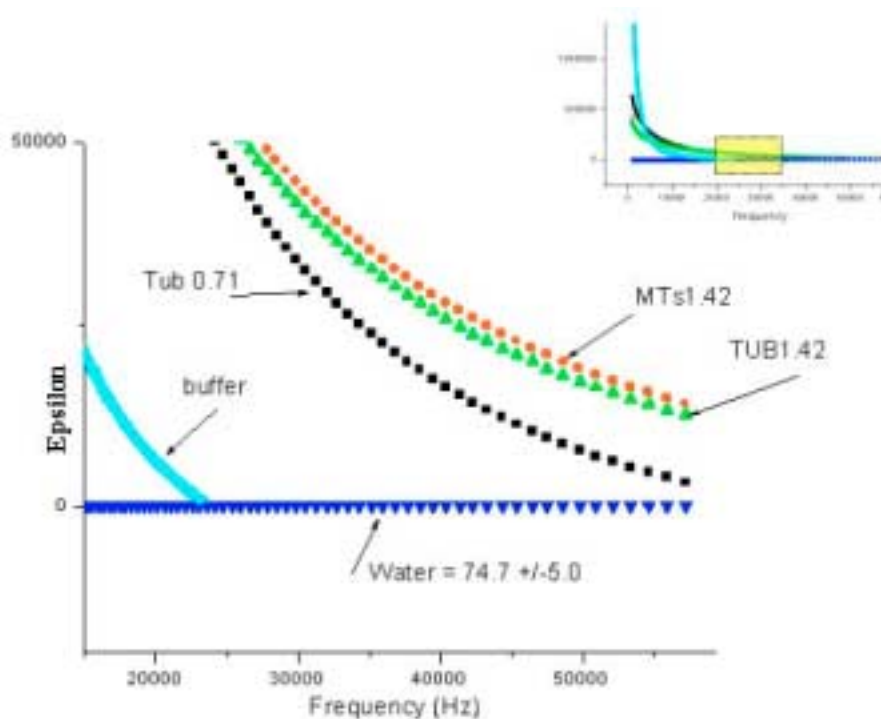
The results of dielectric spectroscopy on tubulin at various concentrations are summarized in Fig. 24,25 and 26 below.



**Fig. 24. Dielectric Spectroscopy of Tubulin Buffer at Relatively Low Frequency.**



**Fig. 25 Buffer Close-up.** A close-up of the tail of the buffer background data. Error bars here show that even at 20kHz there is considerable noise.



**Fig. 26. Combination Graph.** Composite graph of three indicative tubulin concentrations. The inset shows the entire frequency range behavior and the main graph is the close-up. The MTs 1.42 (microtubules at 1.42 mg/mL) and TUB 1.42 (tubulin at 1.42 mg/mL) plots are within each other's error bars (not shown for clarity). To arrive at  $|\mathbf{p}| \sim 10^3 \text{ D}$  (a strictly order-of-magnitude estimate at this point) the 50 kHz data was taken.

#### 5.4.5 Discussion of Dielectric Spectroscopy Results

It is stressed that at this point the dielectric spectroscopy results are shown only as a proof of principle. In other words, it is possible, by taking data at a range of concentrations to obtain the characteristic curves of concentration VS dielectric permittivity and by adding the components of the sample one by one it is in principle possible to extract an accurate value for the dipole moment of a large protein molecule

(and the rest of the components) at around 50kHz. Below this frequency a sophisticated error-reduction technique is required which is currently lacking. From the preliminary data shown here, an order of magnitude calculation for the dipole moment of tubulin can be performed from equation (9) of this Chapter to yield  $|\mathbf{p}| \sim 10^3$  using the 7.1mg/mL concentration data and assuming no interaction of buffer and tubulin dipole moments. This value is purely qualitative at this point but can be refined with further experimentation.

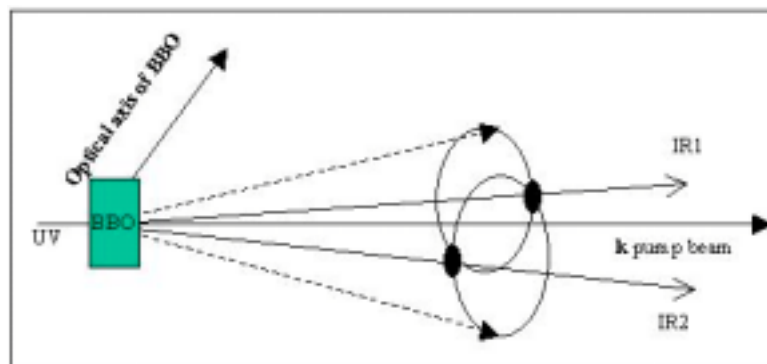
## CHAPTER VI

### FUTURE DIRECTIONS

#### 6.1 Entanglement

Since 1935 when Erwin Shroedinger coined the word "entanglement" to refer to a state where the wavefunction describing a system is unfactorizable, much has been learned about this peculiar phenomenon and it has turned out to be very useful in quantum information science, quantum cryptography and quantum teleportation. Entanglement has been experimentally realized in light [127,128], in matter [129] and in combinations of those [44,130]. One way to produce entangled states in light is via type II phase-matching parametric downconversion which is a process occurring when ultraviolet (UV) laser light is incident on a non-linear beta-barium borate (BBO) crystal at specific angles. A UV photon incident on a BBO crystal can sometimes spontaneously split into two correlated infrared (IR) photons (each of half the energy of the incident photon). The infrared photons are then emitted on opposite sides of the UV pump beam, along two cones, one of which is horizontally polarized and the other vertically. The photon pairs that are emitted along the intersections of the two cones have their polarization states entangled. This means that each photon is individually unpolarized, but the photons necessarily have perpendicular polarizations to each other. The state  $\Psi$  of the outgoing entangled photons can be written as:  $|\Psi\rangle = (\leftrightarrow, \uparrow) + e^{i\alpha}(\uparrow, \leftrightarrow)$  where the arrows indicate polarizations for the (first,second) IR photon and can be controlled by inserting appropriate half wave plates, while the phase factor  $e^{i\alpha}$  can be controlled by

tilting the crystal or using an additional BBO in a setup similar to the one depicted in Fig. 27, modified from [131]



**Fig. 27. Type II Phase Matching Parametric Downconversion.** For certain orientations, a UV photon is absorbed by the BBO crystal and re-emitted as two entangled IR photons (IR1, IR2)

Measuring the state of one of the outgoing photons -say IR1, immediately determines the state of the other (IR2) regardless of their separation in space. This counterintuitive phenomenon is referred to as the Einstein Podolsky Rosen (EPR)-paradox and such pairs are called EPR pairs.

## 6.2 Molecular Electronics

Today's conventional devices are of order 180nm in size while future molecular devices promise a further order of magnitude reduction to this minimum. As a result, there have been considerable efforts concentrated on identifying various chemical substances with appropriate characteristics to act as binary switches and logic gates. For instance, rotaxanes have been considered as switches/fuses [21] and carbon nanotubes as active channels in field effect transistors [22]. Many of these substances are

unsuitable for placement on traditional chips [23] or for forming networks, while virtually all of these efforts attempt to hybridize some kind of electrical wires to chemical substrates in order to obtain current flows. This complicates the task because of the need for appropriately nanomanufactured wires and connections.

This proposed approach is different as the role of the binary states is not played by the presence or bulk movement of electrons, but by naturally occurring conformational states of tubulin molecules and their self-assembled polymers - microtubules (MTs). Moreover, the external interaction with these states is to be performed by coupling laser light to specific spots of a microtubular network. Signal propagation is via travelling electric dipole moment flip waves along MTs while modulation is achieved by microtubule-associated-protein (MAP) binding that creates “nodes” in the MT network. In our proposed scheme for information manipulation, there is no bulk transfer of (charged) mass involved. Tubulin polymerization can be controlled by temperature and application of chemicals and MAPs to yield closely or widely spaced MTs, centers, sheets, rings and other structures [24,25], thus facilitating fabrication of *nanowires, nodes and networks* and even structures capable of long-term information storage (*biomolecular computer memory*). MT-based “quantum brain” models and hypotheses offer a plethora of predictions such as long-lived quantum superposed and quantum entangled states among tubulin dimers and long-range non-neurotransmitter-based fast communication among neurons. Further, predictions of ferroelectricity along MT protofilaments, emission of coherent photons, intracellular quantum teleportation of dipole quanta states [28] and other controversial yet fascinating features have been

proposed, all based on the reasonable *assumption* that tubulin has the electric (and quantum) properties suggested by computer simulations. Currently, no experimental determination of these properties exists.

## **6.3 Proposed Further Research**

### **6.3.1 On-Demand Entangled Photon Source**

An on-demand entangled photon source (ODEPS) can be built and utilized to do spectroscopic analysis of proteins and other biomolecules. Such a device would greatly facilitate studies of the fundamental quantum properties of entangled objects, possible quantum properties of living matter, quantum information science and more. It would also provide an opportunity to test and identify the problems associated with the construction of a portable entanglement source to be taken "into the field" if and when entangled photons become indispensable to secure communications. For instance, tolerances to of entangled photon generation to vibration and temperature changes will be studied. A minimally modified design of the SPR apparatus developed for this project, coupled to a source of entangled photons would be capable of detecting the often conjectured mesoscopic bulk coherence and partial quantum entanglement of electric dipole moment states, existence of which will cast biomolecules as appropriate candidates for the implementation of *qubits*. We will follow a protocol similar to one developed by Oberparleiter et. al. [132] , capable of producing brightnesses in excess of 360,000 entangled photon pairs per second, coupled to a setup similar to the one developed by Altewischer et. al. [133] where entangled photons are transduced into



(entangled) surface plasmons and re-radiated back as entangled photons. The essential difference would be that the insides of the perforations in the gold film of Altewischer et. al. would be covered with dextran to which a monolayer of tubulin dimers or microtubules would be immobilized by amine coupling (this is standard procedure in our laboratory). The evanescent wave of the (entangled) surface plasmon generated at resonance will interact with the electric dipole moment of the immobilized protein complexes and presumably transfer the entanglement to a dipole state in a manner similar to the transfer of the photon polarization entanglement to surface plasmons. At the end of the tunnel, the surface plasmons would be reradiated having undergone the interaction with the protein electric dipole moment. If partial entanglement with the partner photon (that underwent none of these transductions) is found, then this would suggest that the protein is capable of "storing" the entanglement in its electric dipole moment state and characteristic decoherence times could be derived. The obvious objection to suggestions of long decoherence times for quantum properties of large molecules at room temperature comes from the application of equilibrium principles to the quantum mechanical aspects of the constituent atoms. We hope to investigate deeper, as although -for instance- the tubulin molecule consists of some 17,000 atoms which are subject to considerable thermal noise, the electric dipole moment state depends crucially on only a few electrons that can be in two sets of orbitals. In addition, tubulin is not an equilibrium system, rather it is a dynamic dissipative system where energy is being pumped in and out constantly. Our theoretical work has suggested that for a certain set of parameters (such as the value of the dipole moment, the pH etc.) tubulin could indeed

sustain a quantum mechanically coherent state for times of the order of microseconds [8].

### 6.3.2 Ways to Detect Quantum Coherence in Microtubules

In Chapter II and [8] comprehensive model conjecture treating certain regions inside MTs as isolated high-Q(uality) QED cavities was put forth as well as a scenario according to which the presence of ordered water in the interior of MTs results in the appearance of electric dipole quantum coherent modes, which couple to the unpaired electrons of the MT dimers via Rabi vacuum field couplings. The situation is analogous to the physics of Rydberg atoms in electromagnetic cavities [32]. In quantum optics, such couplings may be considered as experimental proof of the quantized nature of the electromagnetic radiation. In our case, therefore, if experimentally detected, such couplings would indicate the existence of coherent quantum modes of electric dipole quanta in the ordered water environment of MT, as conjectured in [42,43], and used here.

To experimentally verify such a situation, one must first try to detect the emergent ferroelectric properties of MTs, which are predicted by this model and are potentially observable. Measurement of the dipole moment of the tubulin dimers is also an important step (see Chapter V). A suggestion along these lines has been put forward in [39]. In addition, one should verify the aforementioned vacuum field Rabi coupling (VFRS),  $\lambda_{\text{MT}}$ , between the MT dimers and the ordered water quantum coherent modes. The existence of this coupling could be tested experimentally by the same methods used

to measure VFRS in atomic physics [33], i.e. by using the MTs themselves as cavity environments, in the way described above, and considering tunable probes to excite the coupled dimer-water system. Such probes could be pulses of (monochromatic) light coupling to MTs. This would be the analogue of an external field in the atomic experiments mentioned above. The field would then resonate, not at the bare frequencies of the coherent dipole quanta or dimers, but at the Rabi splitted ones, leading to a double peak in the absorption spectra of the dimers [33]. By using MTs of different sizes one could thus check on the characteristic  $\sqrt{N}$ -enhancement of the (resonant) Rabi coupling as described by equation 10 of Chapter II for MT systems with N dimers.

### 6.3.3 Other Ways to Measure Dipole Moments

Although the most direct approach to determine this quantity would be to measure the acceleration of evaporated single molecules with dipole moment in the gradient of an electric field in vacuum this may prove a difficult task. Even though it is possible to keep tubulin from polymerizing in solution (e.g. by lowering the temperature or raising the salinity), evaporating individual tubulin molecules may be very difficult due tubulin's affinity towards polymerization and aggregation. In other words the protein is naturally 'sticky' and will be hard to corpusculize. In addition, any spraying of this large molecule is bound to break it into its constituent peptides. Furthermore, tubulin's electric dipole moment in vacuum is not directly relevant to its physiological value (although such a measurement would facilitate cross-check of theoretical molecular dynamics simulation calculations). In addition to the techniques described in detail

above, the dipole moment can also be experimentally determined in a manner similar to the one used in “optical tweezers”. A thin gold chip is bathed in a solution of purified depolymerized tubulin. A small spot ( $1\text{mm}^2$ ) is illuminated with a continuous-wave laser beam of known wavelength and power. The laser beam’s diameter can be modulated creating a gradient in the intensity of the beam. The dielectric moment of tubulin will interact with this gradient and the molecule will feel a ponderomotive electric force towards higher beam intensity. This, over a period of time, will concentrate the tubulin molecules at the center of the laser spot. The concentration of tubulin along the chip will be monitored in real time using a second laser beam exciting the SPR. Thus, by measuring the redistribution of molecules in response to the interaction with the intensity gradient and accounting for Brownian motion, one can evaluate the force exerted on tubulin and therefore the electric dipole moment.

## CHAPTER VII

### UNIFICATION OF CONCEPTS AND CONCLUSION

#### 7.1 Putting It All Together

Tubulin was studied with a variety of experimental, theoretical and computational techniques with a focus on establishing the first steps towards using cytoskeletal proteins in novel biomolecular based electronic and/or quantum information processing devices. To this end and to aid in further theoretical study of tubulin and microtubules, work concentrated on investigating the electric properties of this molecule. Supercomputer based molecular dynamics simulations were performed to study geometrical, energetic and electric properties of tubulin *in silico*. The electric dipole moment was determined agreeing closely with similar simulations performed by others and for the first time the dipole moments of the alpha and beta tubulin monomers were individually determined. In order to provide an experimental value to check the simulation results, precision *in vitro* refractometry with two independent methods (direct refractometry and surface-plasmon resonance sensing) was performed yielding the optical frequency polarizability and refractive index of tubulin for the first time. Furthermore, a custom-built dielectric spectroscopy apparatus was developed to demonstrate a method of obtaining the low (~50kHz) dielectric constant and as proof of principle a preliminary run was performed. This paves the way for more precise measurements of tubulin and other proteins and it is shown that the low frequency dielectric response of proteins can be used as an additional handle in proteomics as it

depends strongly on the dipole moment of the protein. The latest theoretical approaches were described yet currently there is not an adequate theory to analytically and accurately describe the dipole-dipole interactions of a protein molecule in a polar solvent so only order-of-magnitude values for the dipole moment of tubulin were obtained based on simplifying assumptions.

In order to establish a connection between the microtubular cytoskeleton and information processing *in vivo*, the effects of overexpression of microtubule associated protein TAU in the associative olfactory memory neurons of *Drosophila* were determined.

Future directions of research concentrating on establishing the possible quantum nature of tubulin were developed theoretically.

Putting all of the above together makes for a wide scope study that impinged upon many aspects of tubulin. This work aims to show the way for focussing future efforts in a number of directions that will hopefully lead to a deeper understanding of proteins and the role that the dielectric and possibly quantum properties of biomolecules play in their function.

## 7.2. Conclusion

It has become increasingly evident that fabrication of novel biomaterials through molecular self-assembly (e.g. microtubules) is going to play a significant role in material science [134] and possibly the information technology of the future [127]. My efforts described in this dissertation strongly suggest that tubulin is near the 'front lines' of intracellular information manipulation and storage. I established that relatively straightforward spectroscopic techniques such as refractometry, surface plasmon resonance sensing and dielectric spectroscopy, coupled with molecular dynamic simulations and (quantum) electrodynamic analytical theory are a fruitful field of study and the first steps in those directions have been illustrated in this manuscript.

Tubulin, microtubules and the dynamic cytoskeleton are fascinating systems and in their structure and function contain the clues on how to imitate nature in artificially fabricated biomolecular information processing devices.

## REFERENCES

1. Nanopoulos, D.V., hep-ph/9505374, from the "XV Brazilian National Meeting on Particles and Fields", Angra dos Reis, Brazil, October 4-8, 1994, and on an invited talk at the "Physics Without Frontiers Four Seas Conference", Trieste, Italy, June 25-July 1, 1995.
2. Penrose, R. (1989) *The Emperor's New Mind*, Oxford University Press, Oxford.
3. Penrose, R. (1994) *Shadows of the Mind* Oxford University Press, Oxford
4. Nogales, E., Whittaker, M., Milligan, R.A. & Downing, K.H (1999)*Cell* **96**, 79-88.
5. Nogales E., Wolf S.G. & Downing K.H. (1998) *Nature* **291**, 199-203.
6. Brown, J. A. (1999) *Ph.D. Thesis*, University of Alberta, Edmonton Canada.
7. Mitchison, J. (1997) *Annu. Rev. Cell Dev. Biol.* **13**, 83-117, 99-100.
8. Mavromatos N.E. & Nanopoulos D.V. (1998) *Inter. J. of Mod. Physics B* **B12** 517-527.
9. Jobs, E., Wolf, D.E., & Flyvbjerg, H. (1997) *Phys. Rev. Lett.* **29 No.3**, 519-522.
10. Flyvbjerg, H., Holy, T.E., & Leibler, S. (1994) *Phys. Rev. Lett.* **73(17)**, 2372 – 2375.
11. Hameroff, S. (1998) *Toxicology Letters* **100-101**, 31-39.



12. Melki, R., Carlier, M.F. Pantaloni, D., & Timasheff, S.N. (1989) *Biochemistry* **28**, 9143-9152.
13. Stebbins, H. & Hunt, C. (1982) *Cell. Tissue Res.* **227**, 609-617.
14. Sackett, D.L., (1995) in *Subcellular Biochemistry*, Volume 24, *Proteins: Structure, Function and Engineering*, Biswas B.B. & Roy, S. Eds., Plenum Press, New York.
15. Pokorny, J., Jelinek, F. & Trkal V. (1998) *Bioelectrochemistry and Bioenergetics* **45**, 239-245.
16. Jelinek, F, Pokorny, J., Saroch, J., Trkal, V., Hasek J. & Palan, B. (1999) *Bioelectrochemistry and Bioenergetics* **48**, 261-266.
17. Pokorny, J. (1999) *Bioelectrochemistry and Bioenergetics* **48**. 267-271
18. Nanopoulos, D.V. Mavromatos, N.E. & Zioutas, K. (1998) *Advances in Structural Biology* **5**, 127-137.
19. Mershin, A., Nanopoulos D.V. & Skoulakis E.M.C. (1999) *Proceedings of the Academy of Athens* **74**, 123-173 <http://xxx.lanl.gov/abs/quant-ph/0007088>. ACT-08/00, CTP-TAMU-18/00.
20. Sataric, M.V., Tuszyński, J.A. & Zakula, R.B. (1993) *Physical Review E* **48** (1) 589-597
21. Collier, C. P., Wong, E. W., Belohradský, M., Raymo, F. M., Stoddart, J. F., Kuekes, P. J., Williams, R. S. & Heath, J. R. (1999) *Science* **285**, 391-394.
22. Gates V., Derycke, R. Martel, J. Appenzeller, P. & Avouris, P. (2001) *NanoLetters* (10.1021/nl015606f S1530-6984(01)05606-5) **Vol. 0, No.0**, 3.3

23. Kohzuma, T., Dennison, C., McFarlane, W., Nakashima, S., Kitagawa, T., Inoue, T., Kai, Y., Nishio, N., Shidara, S., Suzuki, S. & Sykes, A.G. (1999) *J. Biol. Chem.* **270**, 25733-25738.
24. Diaz, J.F. Pantos, E. Bordas, J. & Andreu, M.J. (1994) *J. Mol. Biol* **238**, 214-225.
25. Hirokawa, N., Shiomura, Y. & Okabe, S. (1988) *The Journal of Cell Biology* **107**, 1449-1459.
26. Weinkauff, R. Schanen, P., Yang, D., Soukara, S. & Schlag, E.W. (1995) *J. Phys. Chem.* **99**, 11255-11265.
27. Schlag, E.W., Sheu, S-Y., Yang, D-Y., Selzle, H.L. & Lin, S.H. (2000) *PNAS (USA)* **97**, 1068-1072.
28. Mavromatos, N.E., Mershin, A. & Nanopoulos D.V. (2002) *Int. J. Mod. Phys. B* **16(24)**, 3623-3642.
29. Dustin, P. (1992) *Microtubules* Springer-Verlag, Berlin.
30. Agarwal, G.S. (1984) *Phys. Rev. Lett.* **53**, 1732-1742.
31. Haroche S. & Raimond, J.M. (1994) *Cavity Quantum Electrodynamics* Ed. Berman P., Academic Press New York.
32. Sanchez-Mondragon, J.J. Narozhny N.B. & Eberly, J.H. (1983) *Phys. Rev. Lett.* **51**, 550-560.
33. Bernardot F. (1992) *Europhysics Lett.* **17**, 34-44.
34. Julsgaard, B. , Kozhekin A. & Polzik, E. (2001) *Nature* **413**, 400-412.

35. Fröhlich, H. (1986) *Bioelectrochemistry*, Ed. Guttman, F. & Keyzer, H. Plenum Press, New York.
36. Lal, P. (1985) *Phys. Lett.* **111A**, 389-400.
37. Satarić, M.V. , Tuszyński, J.A. & Zakula, R.B. (1993) *Phys. Rev.* **E48**, 589-599.
38. Zurek, W.H. (1991) *Phys. Today* **44(10)**, 36-56.
39. Mavromatos, N.E., Nanopoulos, D.V., Samaras, I. & Zioutas, K. (1998) *Advances in Structural Biology* **5**, 127-137.
40. Sackett, D.L. (1995) *Subcellular Biochemistry* Plenum Press, New York.
41. Hameroff, S.R. (1974) *Am. J. Clin. Med.* **2**, 163-173.
42. Del Giudice, E., Doglia, S., Milani M. & Vitiello, G., (1986) *Nucl. Phys. B* **275**, 185-195.
43. Del Giudice, E., Preparata, G., & Vitiello, G. (1988) *Phys. Rev. Lett.* **61**, 1085-1185.
44. Julsgaard B., Kozhekin, A. & Polzig, E. (2001) *Nature* **413** 400-403.
45. Scully M. & Zubairy, S. (2001) *PNAS (USA)* **98 No. 17**, 9490-9493.
46. Song, K-H. & Zhang, W-J. (2001) *Physics Letters A* **290**, 214-218.
47. Samal S. & Geckeler, K.L. (2001) *Chemical Communications*, 2224 [www.rsc.org/chemcomm](http://www.rsc.org/chemcomm).
48. Stebbins H. & Hunt, C. (1982) *Cell. Tissue Res.* **227**, 609-619.
49. Tegmark, M. (2000) *Phys. Rev. E* **61**, 4194-4200.

50. Otwinowski, M, Paul, R. & Laidlaw, W.G. (1988) *Phys. Lett. A* **128**, 483-493.
51. Tsue Y. & Fujiwara Y. (1991) *Progr. Theor. Phys.* **86**, 469-479.
52. Satarić, M.V., Zeković, S., Tuszyński J.A. & Pokorny, J. (1998) *Phys. Rev. E* **58**, 6333-6340.
53. Wouternsen H. & Bakker, H.J. (1999) *Nature* **402**, 507-510.
54. Jibu, M., Hagan, S., Hameroff, S., Pribram, K. & Yasue, K. (1994) *Biosystems* **32**, 195-214.
55. Kielpinski, D., Meyer, V., Rowe, M.A., Sackett, C.A., Itano, W.M., Monroe, C. & Wineland, W.M. (2001) *Science* **291**, 1013-1033.
56. Gisin N. & Percival, I. (1993) *J. Phys. A* **26**, 2233-2239.
57. Koruga, D.L. (1985) *Ann. NY Acad. Sci.* **466**, 953-957.
58. Peterlinz, K.A., (1996) *Optics Communications* **130**, 260-270.
59. Mavromatos, N., (1999) *Bioelectrochemistry and Bioenergetics* **48**, 100-123.
60. Vogel, G. (1998) *Science*, **280**, 123-133.
61. Mori, H. (1989) *Biochemical and Biophysical Research Communications* **159(3)**, 1221-1226.
62. Novak, M. (1999) *Proc. Natcl. Acad. Sci. USA*, **88**, 5837-5841.
63. Hutton, M., Lewis, J., Dickson, D., Yen, S-H. & McGowan, E. (2001) *Trends in Mol. Medicine* **7**, 467-470.
64. Lewis, J., McGowan, E., Rockwood, J., Melrose, H., Nacharaju, P., Van Slegtenhorst, M., Gwinn-Hardy, K., Paul-Murphy, M., Baker, M., Yu, X., Duff, K.,

Hardy, J., Corral, A., Lin, W.L., Yen, S.H., Dickson, D.W., Davies, P. & Hutton M (2000) *Nat Genet* **1**, 127-158.

65. Wittman, C.W., Wszolek, M.F., Shulman, J.M., Salvaterra, P.M., Lewis, J. Hutton, M. & Feany, M.B. (2001) *Science* **293**, 711-714.

66. Jackson, G.R., Wiedau-Pazos, M., Wagle, N., Brown, C.A., Massachi, S. & Geschwind, D.H. (2002) *Neuron* **34**, 509-519.

67. Brion, J.P., Tremp, G. & Octave, N.J. (1999) *Am J Pathol* **154**, 255-270.

68. Woolf, N.J., Zinnerman, M.D. & Johnson, G.V. (1999) *Brain Res.* **821(1)**, 241-249.

69. Armstrong, J.D., deBelle, J.S., Wang, Z. & Kaiser, K. (1998) *Learning and Memory* **5**, 102-114.

70. Brand, A.H. & Perrimon, N. (1993) *Development* **118**, 401-415.

71. Skoulakis, E.M.C. & Davis, R.L. (1996) *Neuron* **17**, 931-944.

72. Skoulakis, E.M.C., Kalderon, D., & Davis, R. L. (1993) *Neuron* **11**, 197-208.

73. Dubnau, J., Grady, L., Kitamoto, T. & Tully, T. (2001) *Nature* **411**, 476-480.

74. McGuire, S.E. & Le, P.T. (2001) *Science* **293**, 1330-1333.

75. Heidary, G. & Fortini, M. (2001) *Mech. of Development* **108**, 171-178.

76. Himmler, A. (1989) *Mol. Cell. Biol.* **9**, 1389-1396.

77. Himmler, A., Drechsel, D., Kirschner, M.W. & Martin, J.D.W. (1989) *Mol. Cell. Biol.* **9**, 1381-1388.

78. Tully, T. & Quinn, W. (1985) *J. Comp. Physiol.* **157**, 263-277.

79. Philip, N., Acevedo, S., & Skoulakis, E.M.C. (2001) *J Neuroscience* **21**, 8417-8425.
80. Beck, C.D.O., Schroeder, B. & Davis, R.L. (2000) *J. Neuroscience* **20**, 2944-2953.
81. Preat, T. (1998) *J. Neuroscience* **18**, 8534-8538.
82. Joynes, R.L. & Grau, J.W. (1996) *Behavioral Neuroscience* **110**, 1375-1387.
83. DeBelle, S.J. & Heisenberg, M. (1994) *Science* **263**, 692-695.
84. Wittman, C.W., Wszolek, M.F., Shulman, J.M., Salvaterra, P.M., Lewis, J., Hutton, M. & Feany, M.B. (2001) *Science* **293**, 711-714.
85. Buchanan, R.L. & Benzer, S. (1993) *Neuron* **10**, 839-850.
86. Crittenden, J.R., Skoulakis, E.M.C., Han, K-A., Kalderon, D. & Davis, R.L. (1998) *Learning and Memory* **5**, 38-51.
87. Merishin, A., Pavlopoulos, E., Fitch, O., Braden, B.C., Nanopoulos, D.V., & Skoulakis, E.M.C. (*accepted to J. Learning and Memory Oct. 2003*).
89. Cheng, Y., Endo, K., Wu, K., Rodan, A.R., Heberlein, U. & Davis, R.L. (2001) *Cell* **105**, 757-768.
90. Bancher, C., Brunner, C., Lassmann, H., Budka, H., Jellinger, K., Wiche, G., Seitelberger, F., Grundke-Iqbal, I. & Wisniewski, H.M. (1989) *Brain Res.* **477**, 90-99.
91. Garcia, M.L. & Cleveland, D.W. (2001) *Curr. Opin. Cell Biology* **13**, 41-48.
92. Lee, V.,M-Y, Goedert, M. & Trojanowski, J.Q. (2001) *Ann. Rev. Neurosci.* **24**, 1121-1159.
93. Mitchison, T. & Kirschner, M.W., (1984) *Nature* **312**, 237-242.

94. Torroja, L., Hsin, C., Kotovsky, I. & White, K. (1999) *Current Biology* **9**, 489-492.
95. Lewis, J., McGowan, E., Rockwood, J., Melrose, H., Nacharaju, P., Van Slegtenhorst, M., Gwinn-Hardy, K., Paul-Murphy, M., Baker, M., Yu, X., Duff, K., Hardy, J., Corral, A., Lin, W.L., Yen, S.H., Dickson, D.W., Davies, P. & Hutton, M. (2000) *Nat Genet* **1**, 127-148.
96. Connoly, J.B., Roberts, I.J.H., Armstrong, J.D., Kaise, K., Forte, M., Tully, T. & O’Kane, C.J. (1996) *Science* **274**, 2104-2107.
97. Ebner, A., Godemann, R., Stamer, K., Illenberger, S., Trinczeck, B., Mandelkow, E-M. & Mandelkow, E. (1998) *J. Cell Biol.* **143**, 777-794.
98. Martin, M., Iyadurai, S.J., Gassman, A., Gindhart, J.G.J., Hays, T.S. & Saxton, W.M. (1999) *Molec Biol Cell* **10**, 3717-3728.
99. Panda, D., Miller, H.P. & Wilson, L. (1999) *PNAS (USA)* **96**, 12459-12464.
100. Woolf, N.J., Young, S.L., Johnson, G.V.W. & Fanselow, M.S. (1994) *NeuroReport* **5**, 1045-1048.
101. Duffy J.B. (2002) *Genesis* **34**, 1-15.
102. Ponder J.W. & Richards F.M. (1987) *J. Comput. Chem.* **8**, 1016-1024.
103. Pappu, R.V., Hart, R.K., Ponder, J.W., (1998) *J. Phys. Chem. B*, **102**, 9725-9742.
104. MacKerrel, A.D., Banavali, N. & Foloppe, N. (2000) *Biopolymers* **56(4)** 257-265.

105. Jackson, J.D. (1999) *Classical Electrodynamics, third edition* John Wiley & Sons, Inc. New York.
106. Hedestrand, G., (1929) *J.Phys.Chem.* **B2**, 428-438.
107. Kirkwood, J.G. (1939) *J. Chem Phys* **7**, 911-919.
108. Kirkwood J.G., (1939) *J. Chem. Phys*, **7**, 919-924.
109. Gilson, M.K. & Honig, B.H. (1986) *Biopolymers*, **25**, 2097-2119.
110. Vater, W., Bohm, K.J., & Unger E., (1997) *Cell Mobility and the Cytoskeleton* **36**, 76-83.
111. Quillin, M.L. & Matthews, B.W. (2000) *Acta Crystallogr D Biol Crystallogr.* **56 ( Pt 7)**, 791-794.
112. Kretschmann, E., (1971) *Z. Physik* **241**, 313-324.
113. Raether, H., (1988) *Surface Plasmons on Smooth and Rough Surfaces and on Gratings*, Springer Tracts in Modern Physics, Volume 111 Springer-Verlag New York.
114. Matsubara, K. Kawata, S. & Minami, S. (1988), *Applied Optics* **27**, 1160-1163.
115. Van Gent, J., Lambeck, P.V., Kreuvel, H.J.M., Gerritsma, G.J., Sudhoelter, E.J.R., Reunhoudt, D.N. & Popma, T.J.A. (1990), *Applied Optics* **29**, 2843-2849.
116. Earp R.L. & Dessy, R.E. (1998) *Surface Plasmon Resonance in Commercial Biosensors: Applications to Clinical Bioprocesses and Environmental Samples*. Ed. by G. Ramsay, John Wiley & Sons New York.



117. BIAcore, Inc. "BIAcore AB": <http://www.biacore.com/scientific/reflist.html> (accessed on 06/01/2002).
118. Melendez, J., Carr, R., Bartholomew, D.U., Kukanskis, K., Elkind, J., Yee, S., Furlong, C. & Woodbury, R., (1996), *Sensors and Actuators B* **35**, 1-5.
119. Jorgenson, R.C., Jung, C., Yee, S.S. & Burgess, L.W. (1993), *Sensors and Actuators B* **13-14**, 721-722.
120. Tong, C., Kolomenskii, A.A., Lioubimov, V.A., Muthuchamy, M., Schuessler, H.A., Trache, A. & Granger, H., (2001) *Biochemistry* **40**, 13915-13924.
121. Kolomenskii, A.A., Gershon, P.D., & Schuessler, H.A. (1997) *Applied Optics* **36**, 6539-6547.
122. Stenberg, E., Persson, B., Roos, H. & Urbaniczky, C. (1991). *Journal of Colloid and Interface Science* **143**, 513-526.
123. Brekhovskikh, L.M., (1980). *Waves in Layered Media* Academic Press, New York.
124. Chaudhur, A.R., Tomita, I., Mizuhashi, F., Murata, K., Potenziano, J.L., & Luduena, R.F. (1998), *Biochemistry* **37(49)**, 17157-17162.
125. Liliom, K., Wagner, G., Pacz, A., Cascante, M., Kovacs, J. & Ovadi, J. (2000) *Eur. J. Biochem.* **267**, 4731-4739.
126. Lofas, S., Johnsson, B., Edstrom, Al, Hansson, A., Lindquist, G., Muller Hillgren & R., Stigh, L., (1995). *Biosensors and Bioelectronics*, **10**, 813-822.
127. Pereira, A., Kimble, A. & Peng A., (1992) *Phys. Rev. Lett.* **68**, 3663-3666.

128. Togerson, T., Branning, S., Monken, M. & Mandel A., (1995) *Phys. Lett. A* **204**, 323-328.
129. Sackett, L. (2000) *Nature* **404**, 256-259.
130. Rauschenbeutel E., (2000) *Science* **288**, 2024-2028.
131. Kwiat, P., Matle, P., Weifurter, P., & Zeilinger K., (1995) *Phys. Rev. Lett.* **75**, 4337-4343.
132. Oberparleiter, B. & Weinfurter, P., (2001) *Phys. Rev. A.* **64**, 23-28.
133. Altewischer, E.T., (2002) *Nature* **418**, 304-306
134. Zhang. S., (2003) *Nature Biotechnology* **21**, 10-18.

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